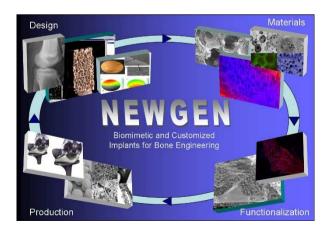






Ceramics and glasses for biomedical applications

S. Hocquet, F. Cambier CRIBC – Mons, BELGIUM



2nd Training School NEWGEN – MP1301 Patras (Greece) 9-12 May, 2017



- What are ceramics?
- Main characteristics
- Classification

Manufacturing

- Batch preparation of powdery materials
- Shaping
- Densification

Structural ceramics materials

- Area of applications
- Properties comparison of some particular ceramics
- Coatings/Porous ceramics

Bioceramics

- Bio-inert
- Bio-active

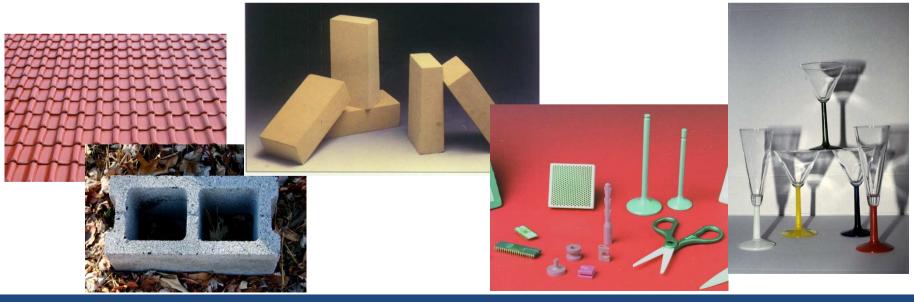
Bioglasses

INTRODUCTION

What are ceramics?

- → Inorganic and non-metallic materials, having high melting points and therefore requires high temperatures for their processing
- \rightarrow Ionic/covalent bond between metallic and non metallic elements (O, N, C, B)
 - ➢ Al₂O₃, ZrO₂, MgO
 - ➢ SiC, Si₃N₄, WC, ZrB₂

→ This includes : tiles, bricks, cements, concretes, refractories, advanced ceramics, ... and glasses



Main characteristics

- Brittle (poor ductility, poor tensile strength)
- > Chemically inert, stable
- > Hard
- Wear-resistant
- > A variety of electrical and thermal properties
- > Refractory
- > Non-magnetic

Some exceptions

- ➤ « YBaCuO » → Superconductor
- \succ (Ba, Sr)O.6Fe₂O₃ \rightarrow Hard magnet
- \succ Partially Stabilized Zirconia \rightarrow High toughness

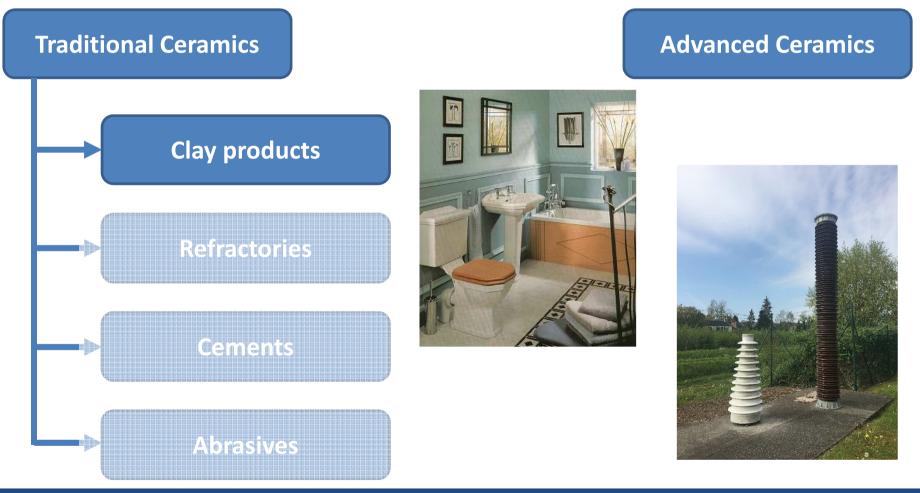
Classification?

 \succ Variety of materials, variety of properties... \rightarrow how to classify them?

Traditional Ceramics

Advanced Ceramics

Classification?



Classification?



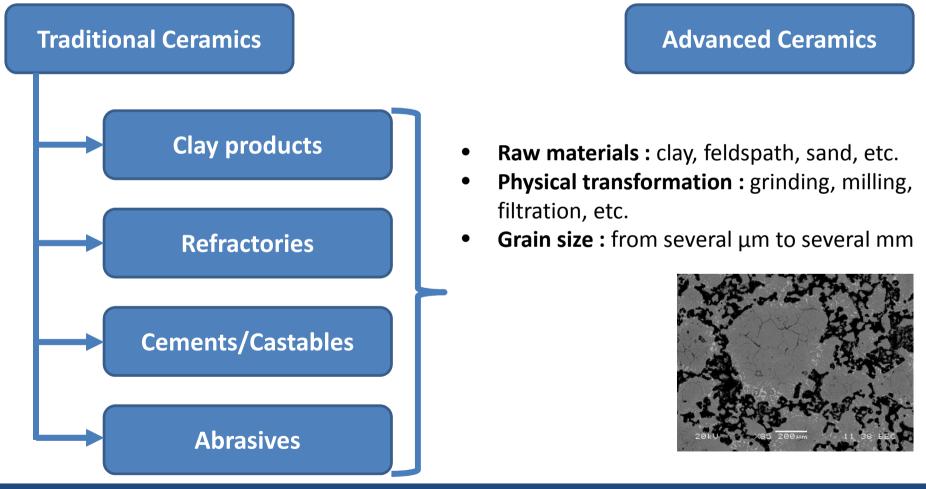
Classification?



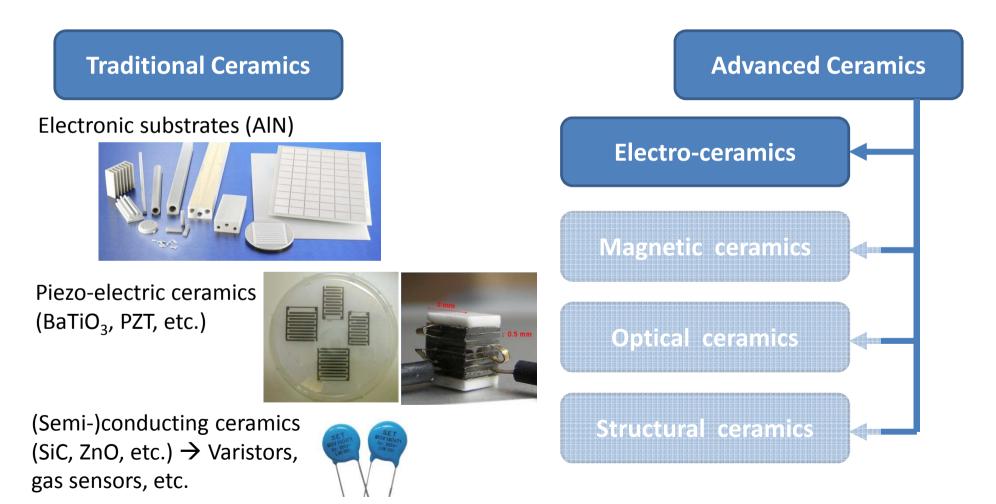
Classification?



Classification?



Classification?



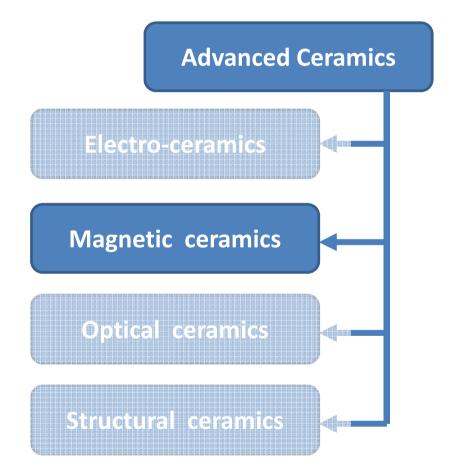
Classification?

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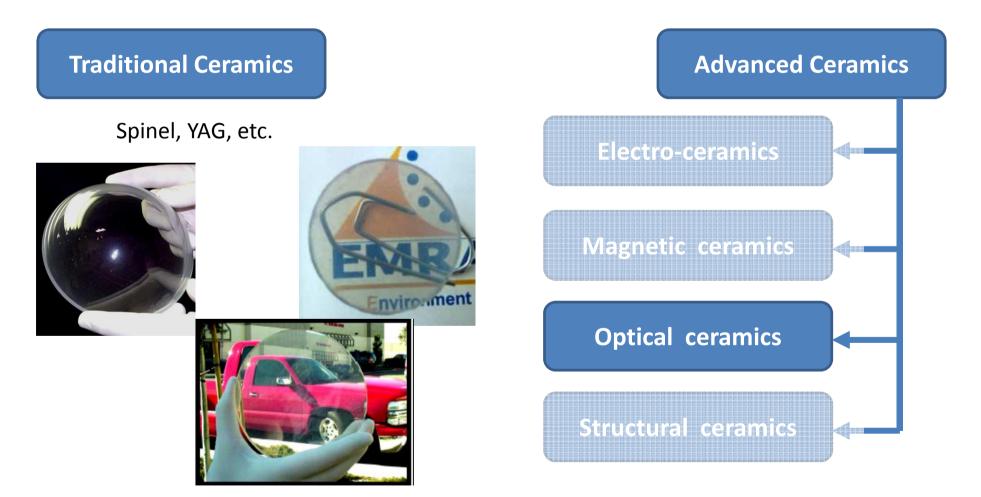
Traditional Ceramics

Ferrite with Fe_2O_3 as major constituent (MnO.Fe₂O₃, SrO.6Fe₂O₃, etc.)

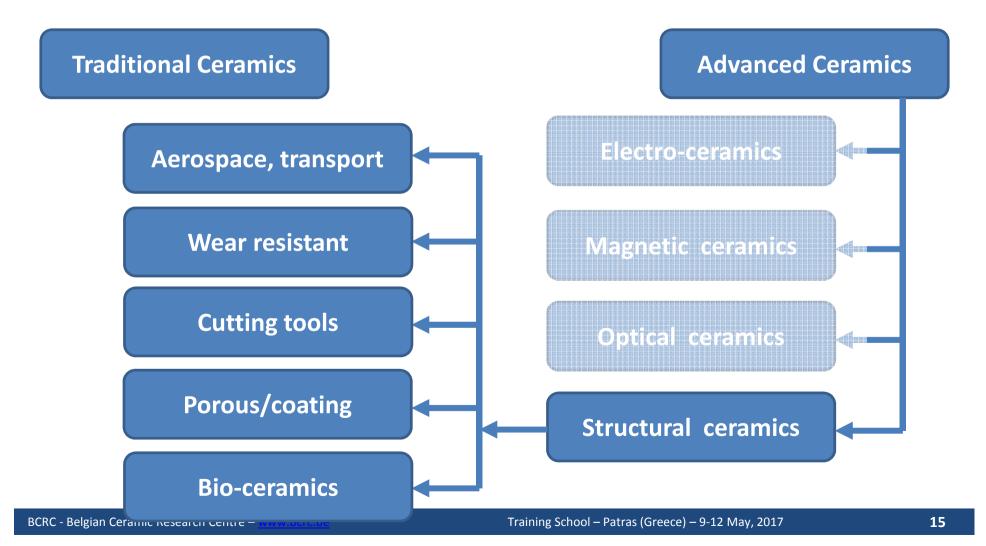
- \rightarrow Miniature transformers
- \rightarrow Microwave absorbing paints (defence)
- ightarrow Isolators and band pass filters
- \rightarrow NMR and drug delivery
- \rightarrow Magnetic sensors
- \rightarrow Robotics, data storage, energy storage, etc.



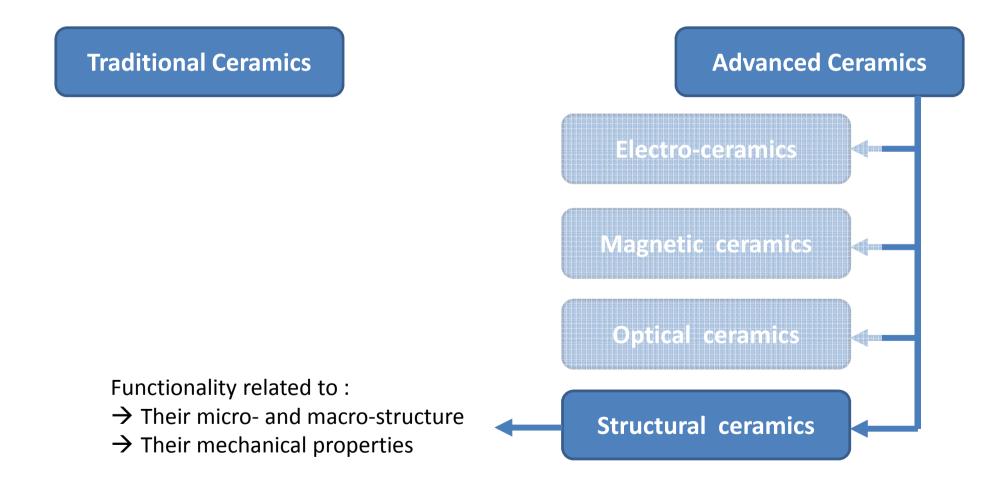
Classification?



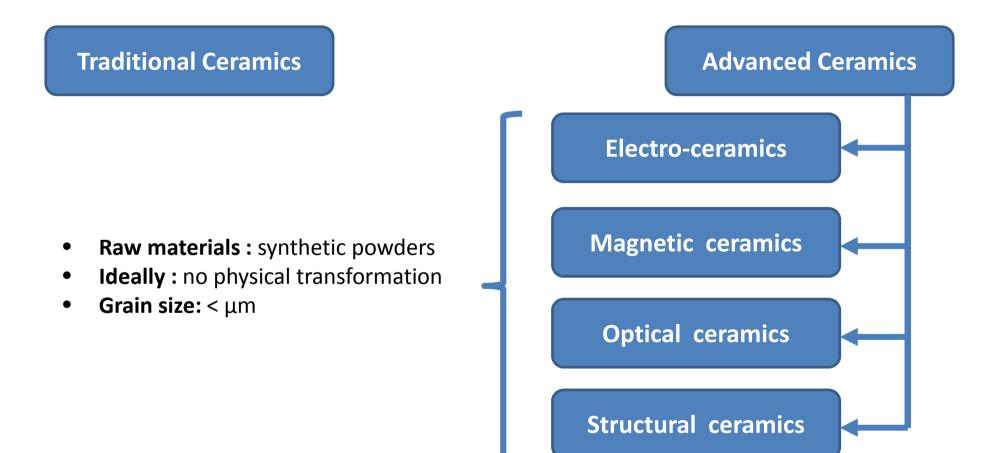
Classification?



Classification?



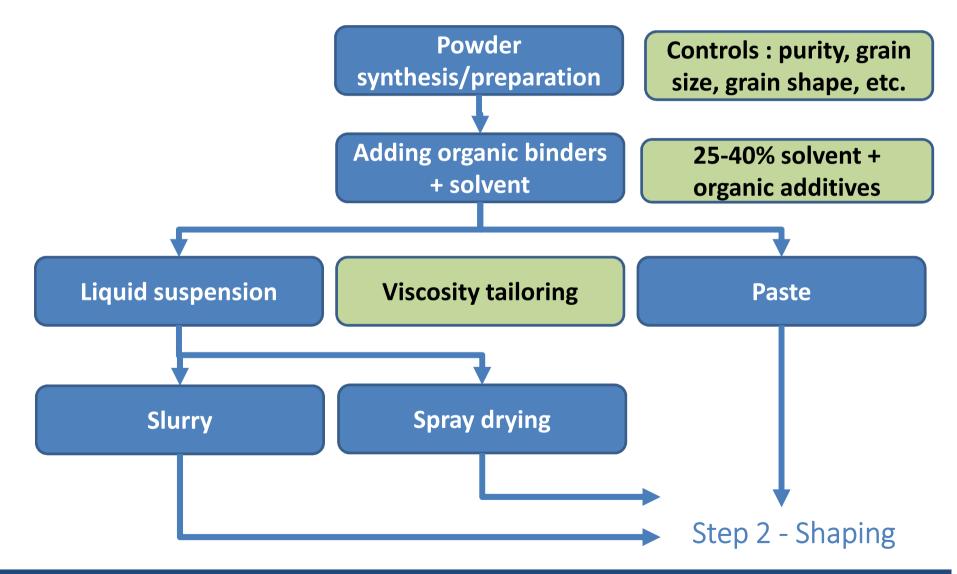
Classification?

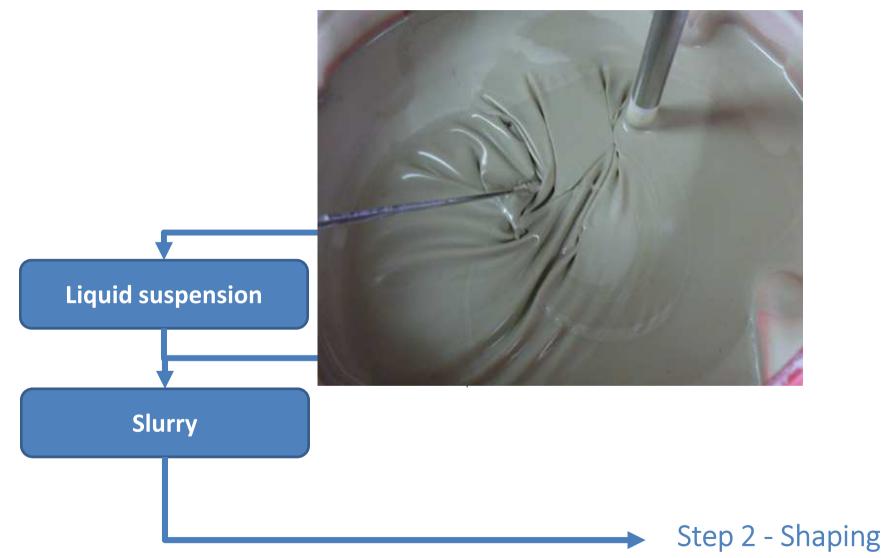


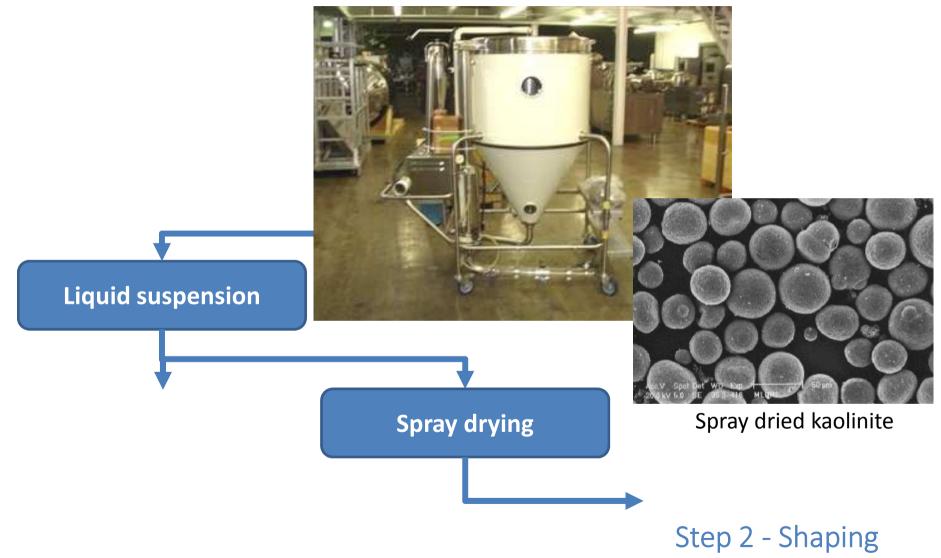
MANUFACTURING

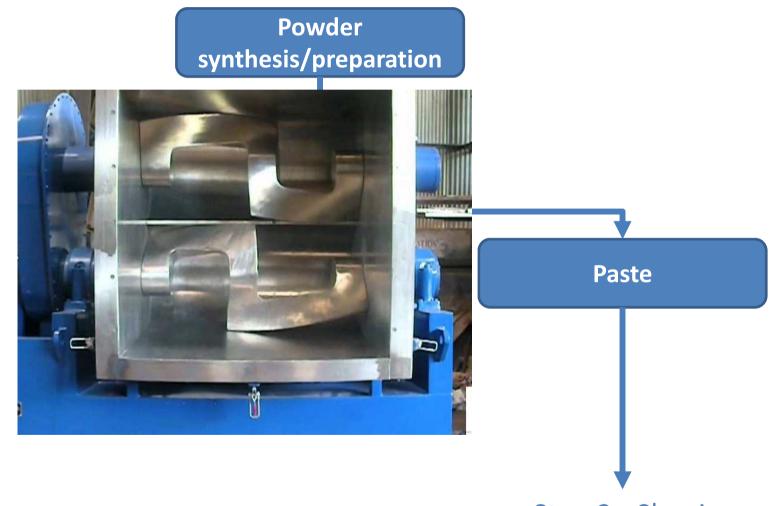
Ceramic manufacturing = sequential process :

- Powder Shaping Thermal treatment Machining
- → Importance of each step!
 - \rightarrow Need to control raw material preparation
 - → The powder synthesis will impact the final material properties
 - Grain size (<µm)
 - Grain size distribution
 - Grain shapes
 - Non agglomerate state
 - Chemical purity
 - Crystal phase
 - →Synthesis methods are classified according to state of the reaction material
 - •solid-solid
 - including a liquid (aquous or organic)including a gas

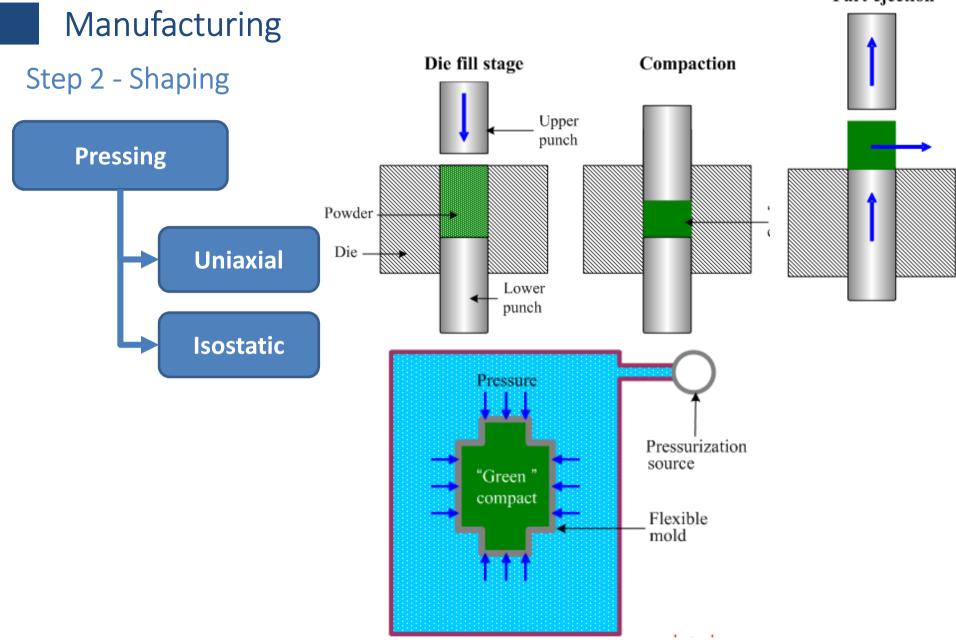


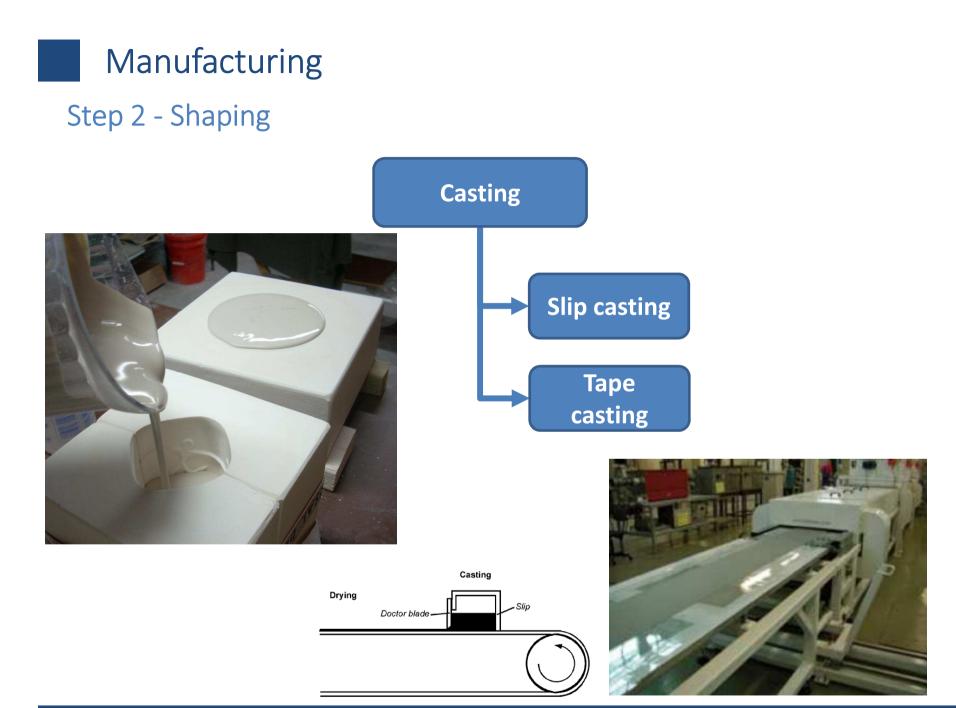




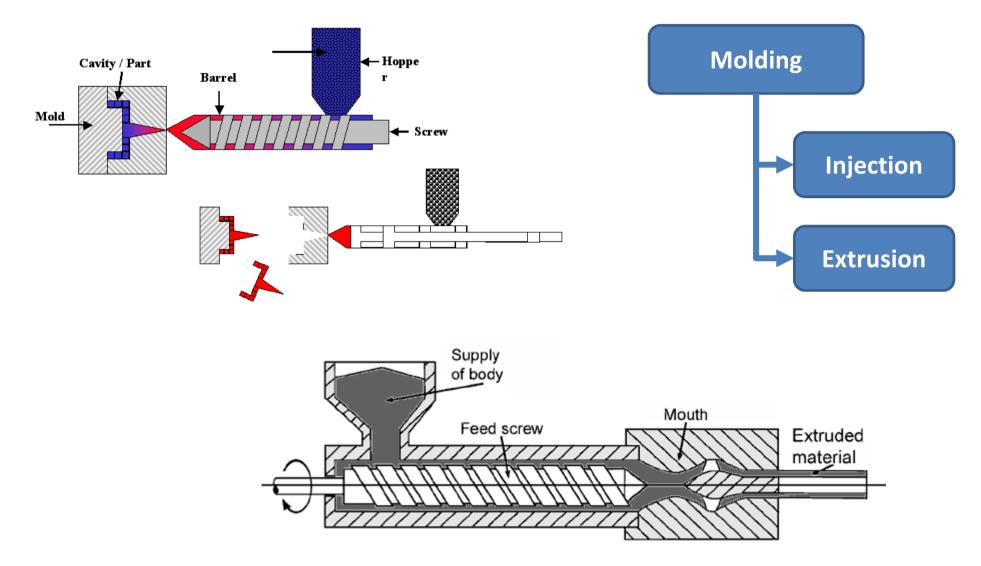


Part ejection



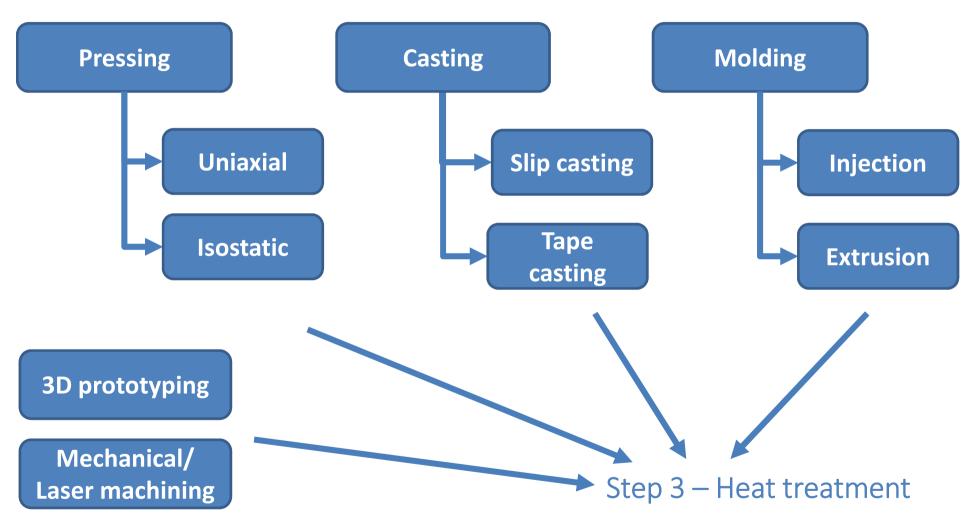


Step 2 - Shaping

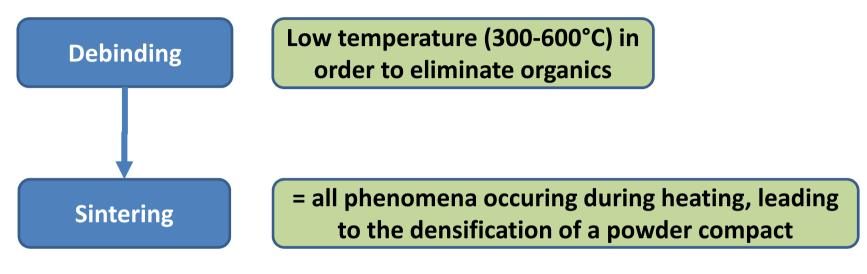




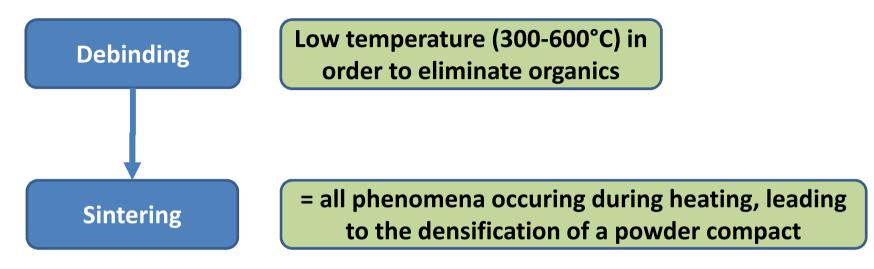
Step 2 - Shaping

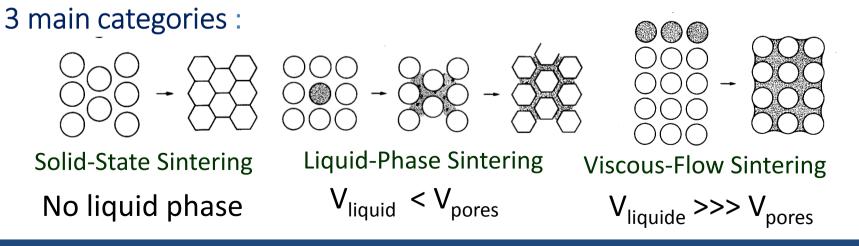


Step 3 – Heat treatment



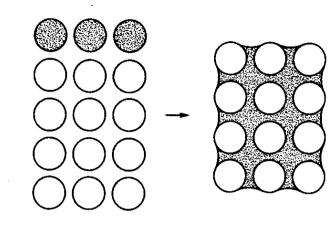
Step 3 – Heat treatment





Step 3 – Heat treatment

Viscous flow sintering





20% of initial solid particles are converted into liquid. Consolidation of materials through a liquid flux, under the action of capillary forces, and formation of a crystalline or vitrous phase during cooling.

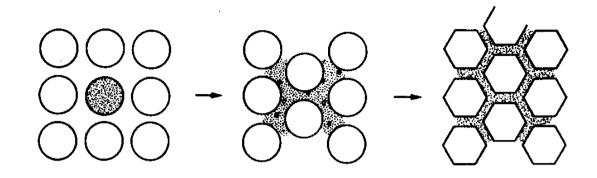
Traditional ceramics obtained from natural raw materials





Step 3 – Heat treatment

Liquid phase sintering



Selection of constituents and sintering temperature such as a small quantity of liquid is formed, allowing an easier diffusion of matter (soluble in the liquid phase) within this liquid phase

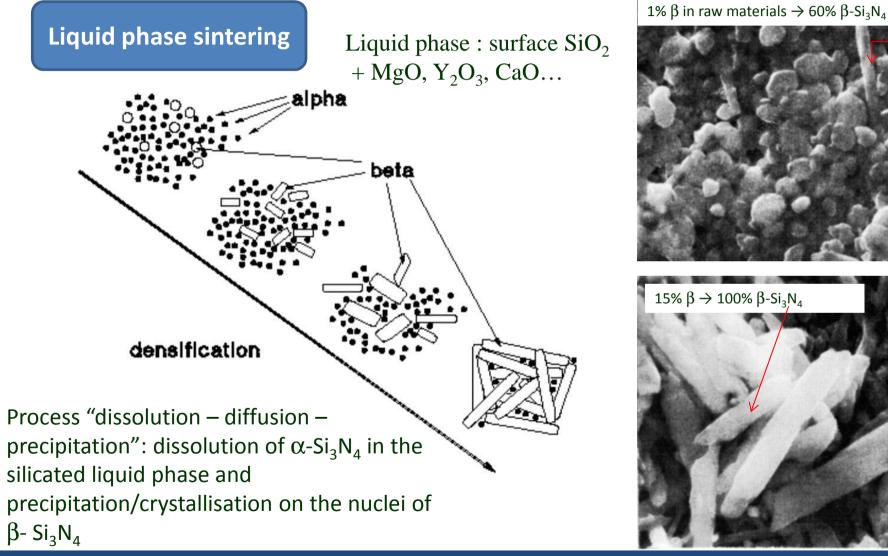
Refractories, alumina isolators, silicon nitride parts, etc.







Step 3 – Heat treatment



BCRC - Belgian Ceramic Research Centre -

Step 3 – Heat treatment

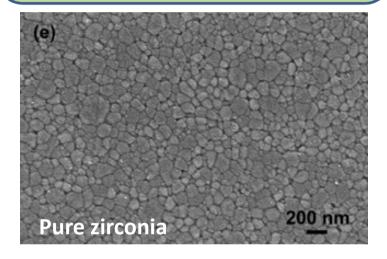
Solid-state sintering

For the manufacturing of high-tech ceramics

Need for high temperature and fine grains

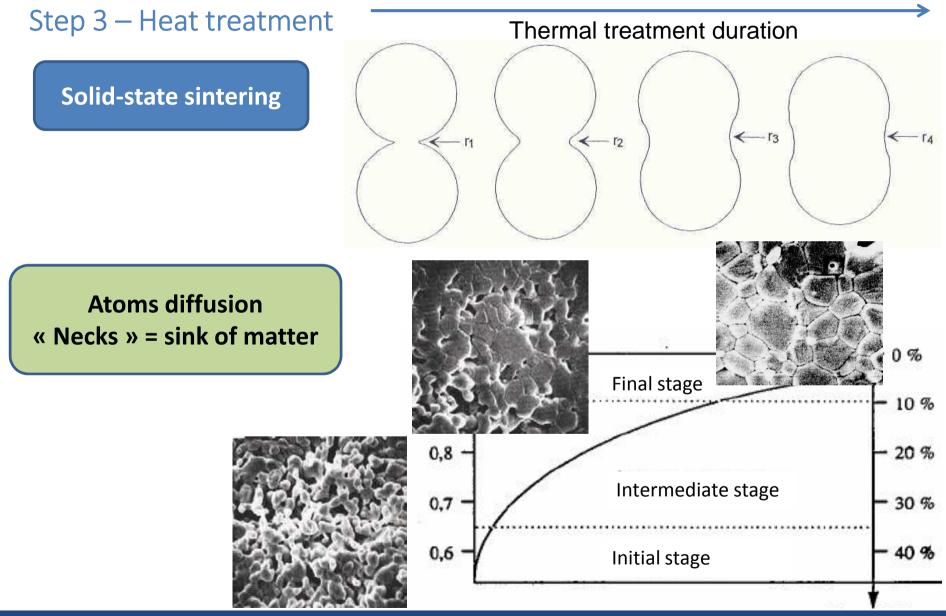
Typical/ideal microstructure :

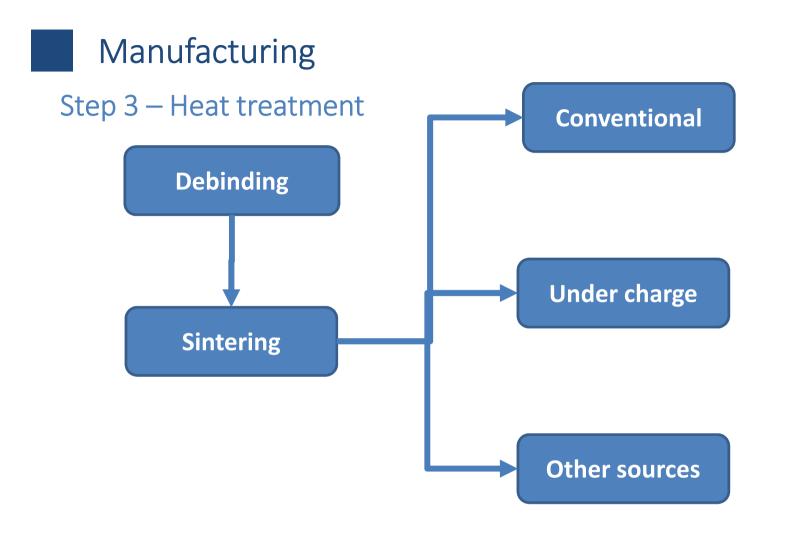
Equiaxial grains, with few residual porosities and no glassy phase at grain boundaries

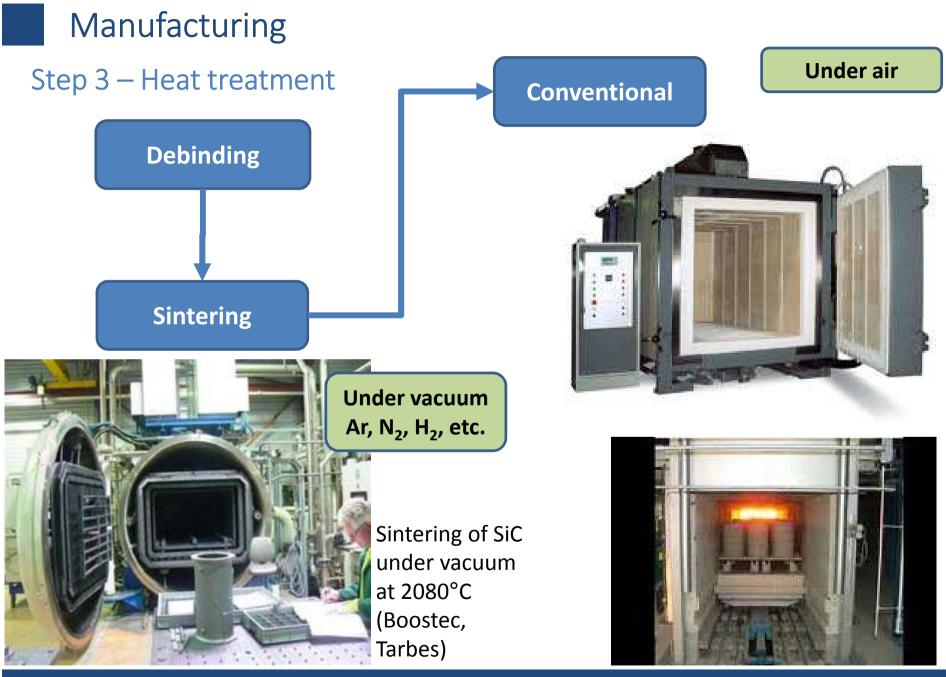


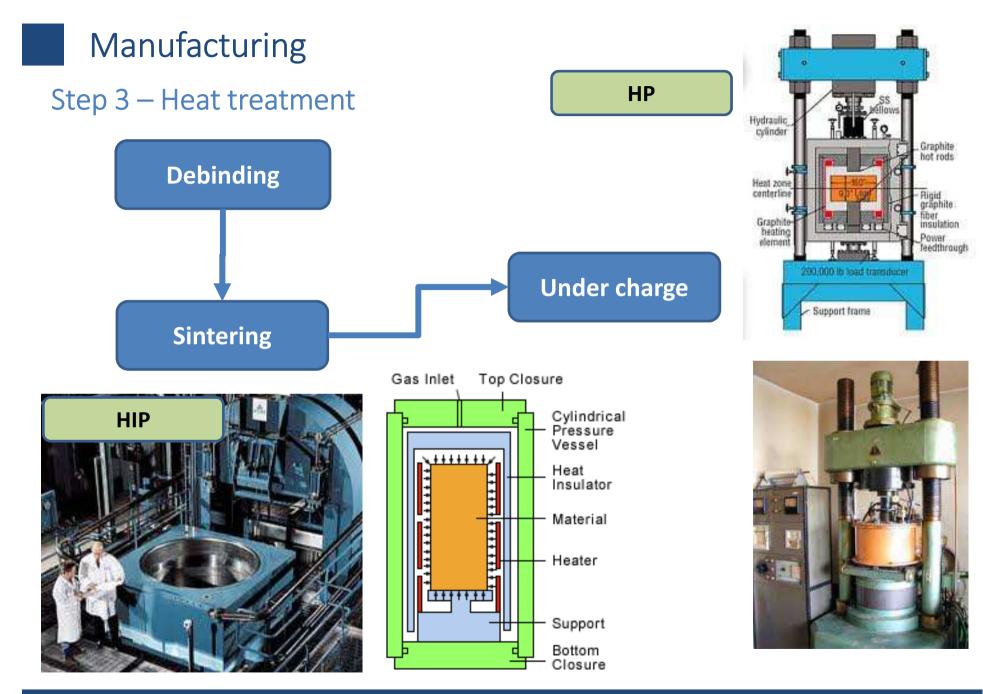


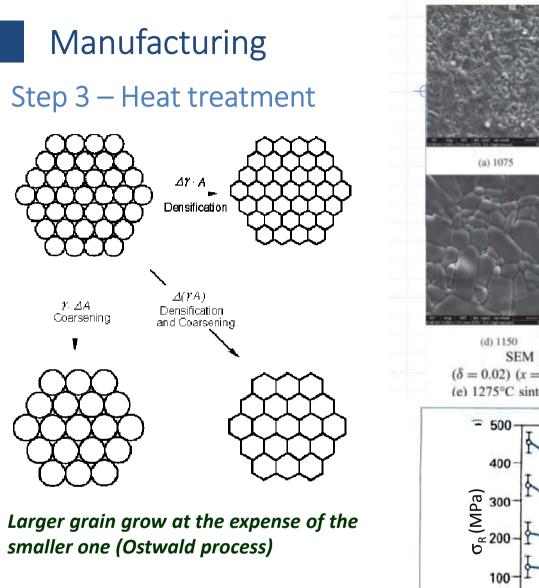


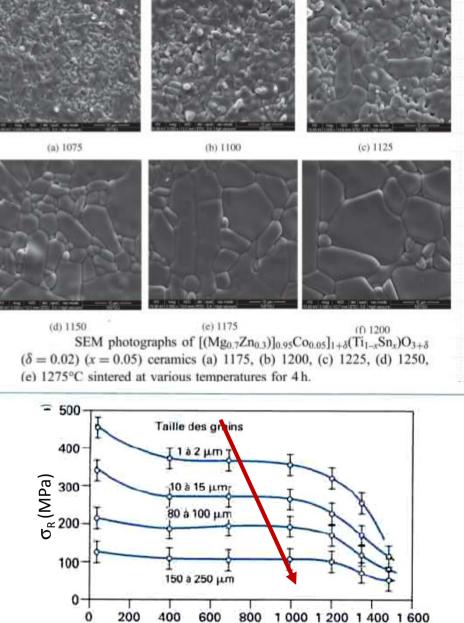




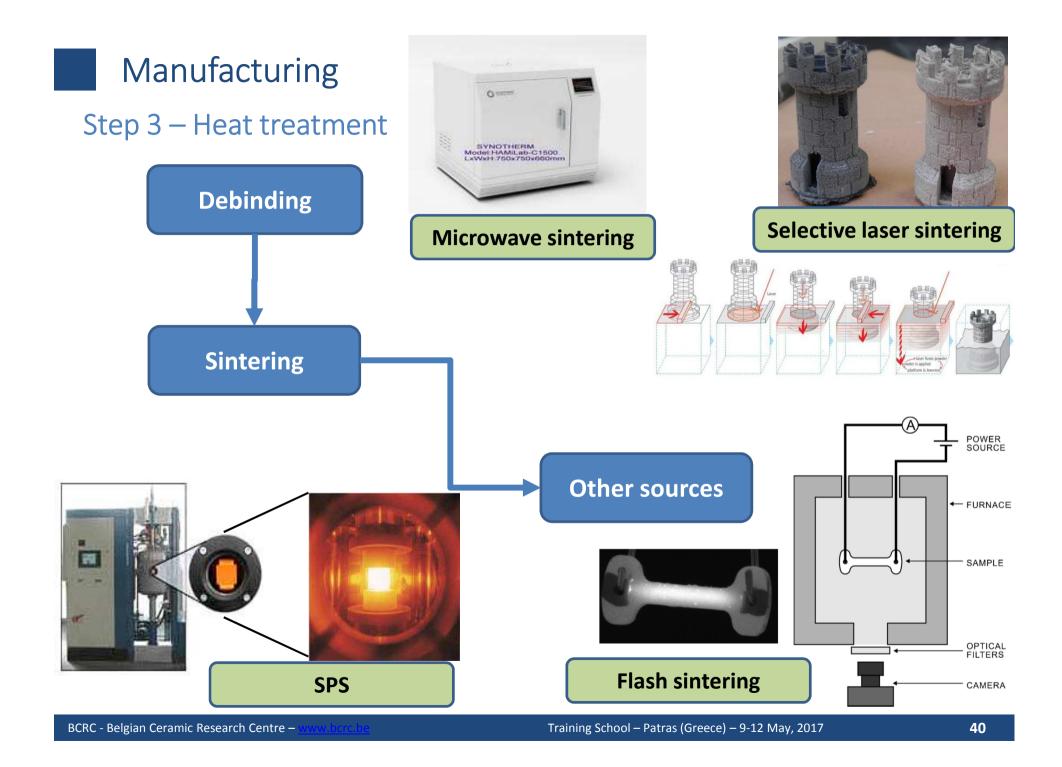








Température (°C)



STRUCTURAL CERAMICS

Categories of structural ceramics



Alumina, zirconia, and their derivatives

Non-oxide

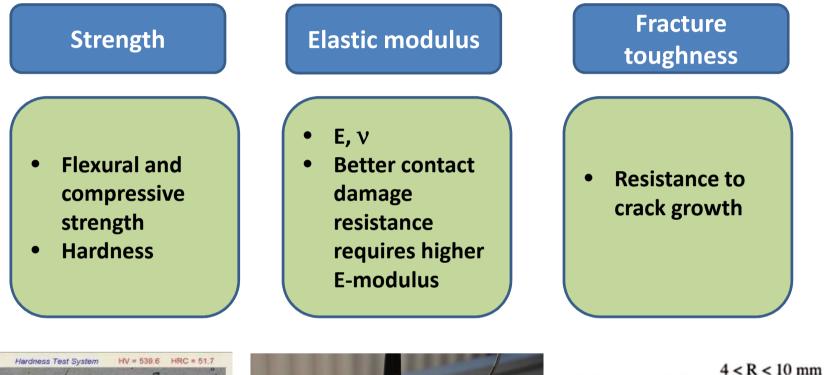
Carbides, borides, nitrides, silicides, etc.

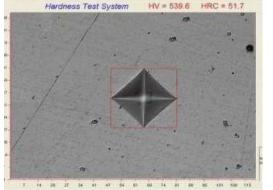
Composites

Particulate and fibre reinforced, combinations of oxides and non-oxides

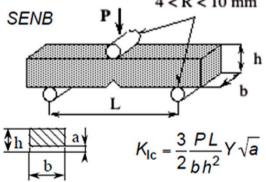
- Oxidation resistant
- Thermally stable
- Chemically inert
- Electrically insulating
- Low thermal conductivity
- Low oxidation resistance
- Extreme hardness
- Chemically inert
- High thermal and electrical conductivities
- Expensive manufacturing process
- High toughness
- Variable thermal and electrical conductivities
- Variable oxidation resistance
- High cost due to complex process

Mechanical properties









Important aera of applications

Application aera	Required properties	Materials used
Wear partsPump sealsBearingsNozzles	High harndess Low frictional resistance Moderate strength	Alumina Silicon carbide
Cutting tools	High strength High hardness Thermal conductivity	Alumina Silicon nitride SiAlON ZTA Alumina-TiC
Engine componentsTurbine rotorValvesCylinder lining	High temperature strength High temperature toughness Thermal insulation	Zirconia Silicon nitride Silicon carbide
Bioceramics	High strength High toughness Inert/Bioactive/biodegradable Controlled porosity	Alumina Zirconia CaP ceramics
PCPC – Polgian Coramic Poscarch Contro		

Properties of typical structural ceramics

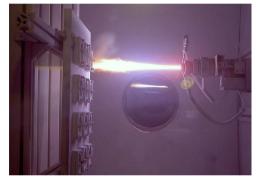
Properties	Alumina	Y-TZP	SiC	Si ₃ N ₄	Other
Compressive strength	3000 MPa	2500 MPa	2500 MPa	2800 MPa	Steel 300 MPa
Flexural strength	<600 MPa	<1200 MPa	350 MPa	1000 MPa	
κ _{1C}	<5MPa.m ^{1/2}	<12MPa.m ^{1/2}	4-5MPa.m ^{1/2}	6MPa.m ^{1/2}	Steel 200MPa.m ^{1/2}
Elastic modulus	390 GPa	250 GPa	400 GPa	300 GPa	Steel 200 GPa
Hardness	18 GPa	12 GPa	35 GPa	25 Gpa	Diamond 90 GPa

Coatings

- Ceramic materials are often used as surface coating on metallic components, in order to take advantage of
 - High hardness
 - Abrasion resistance
 - Thermal insulation
 - ...
- Coating of TiC, TiN, alumina on WC and high speed steel cutting tools improves their life by a factor of 2 – 5
- Zirconia coating are used as thermal barrier for engine components and for improvement of resistance to corrosion (aeronautics, aerospace, etc.)
- Hydroxyapatite coatings are also used to enhance the biocompatibility of surgical tools and medical devices

Coatings – processes used for ceramic coatings

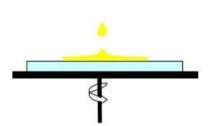
- Sol-gel method
 - dip-coating, spin coating
 - ~10-50µm
- RF Plasma spraying
 - ~10-50µm



> CVD

- ~ 10µm
- Spray pyrolysis
- Electro-phoretic deposition
 - 1-1000µm
- Laser Cladding
 - 0,2 1 mm





Porous ceramics

- \succ Broad range of characteristics \rightarrow wide variety of applications
 - Insulation



• Membrane, filtration, catalysis

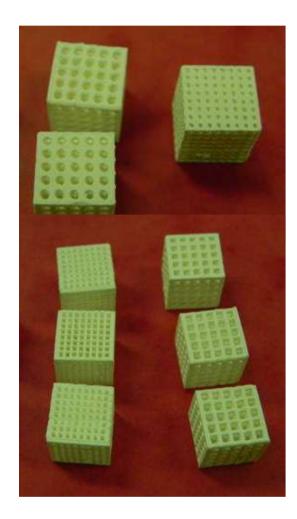




Biomedical applications

Porous ceramics – processing methods

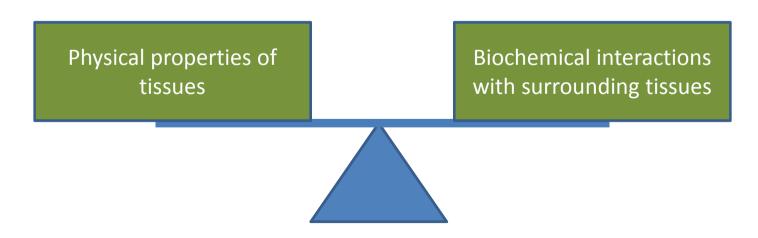
- Sacrificial template pore-forming agents
- ➢ Extrusion
- > Partial sintering process
- Casting of scaffolds
- > 3D prototyping
- ≻ ...
- \rightarrow Fine tuning of pore size distribution and pore shape



BIOCERAMICS

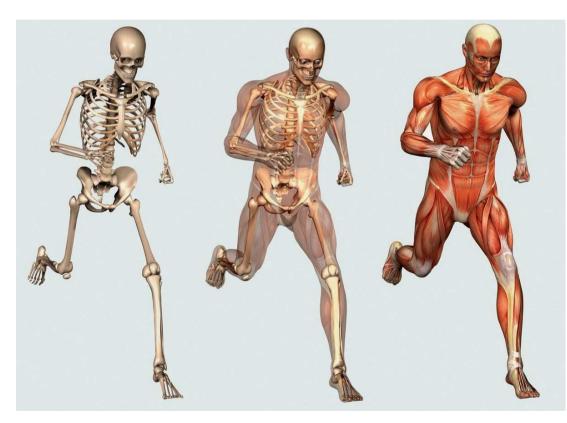
Introduction

- Biomaterials : Natural or synthetic materials compatible with their introduction into contact with living tissues, within the framework of a medical device, without damaging themselves or the environment
- Biomaterials : One of the most active areas of research of Materials Science in recent years
- Human body contains several types of tissues, which are possible to be replaced by man-made synthetic materials, either ceramics, metals, polymers or their composites



Introduction – human hard tissue

 \succ Bioceramics \rightarrow dedicated to replace hard tissue (bones, teeth)



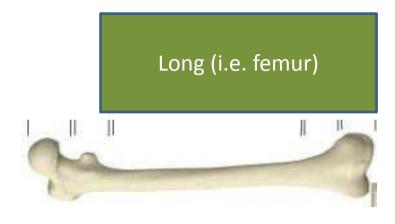
See M. Alini (16:00-17:30)

206 bones (adult)

- = frame of human body
- Protection of organs
 - Brain
 - Thoracic organs
- Supported by muscles, tendons, ligaments, fascias, cartilage
- Involved in blood cells formation
- Sink of minerals (Ca, Mg, ...)
- 4-6 kg for men
 3-4 kg for women

Introduction – human hard tissue

> Several types of bones :



Short (i.e. rotule)





Plane (i.e. clavicule)

Introduction – human hard tissue

- > Composed with :
 - > Water (10-20%)

Inorganic phase – calcium phosphate (60%)

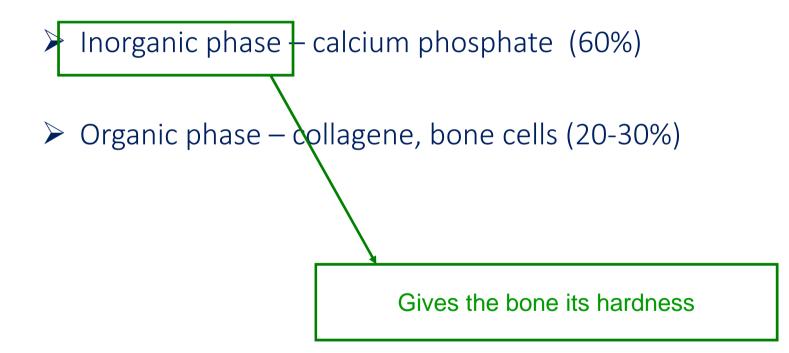
Organic phase – collagene, bone cells (20-30%)

Depends on the location in the body!

Introduction – human hard tissue

> Composed with :

> Water (10-20%)



Introduction – human hard tissue

- > Composed with :
 - > Water (10-20%)

Inorganic phase – calcium phosphate (60%)

Organic phase – collagene, bone cells (20-30%)

Gives the bone its flexibility and flexural/tensile strength

Introduction – human hard tissue

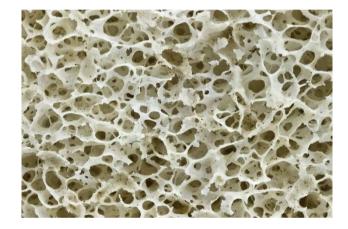
- > Composed with :
 - > Water (10-20%)
 - Inorganic phase calcium phosphate (60%)
 - > Organic phase collagene, bone cells (20-30%)

Bones = natural nano-composites in which collagens act as a bundle of fibers with dispersion on nano-particles of calcium phosphate, and proteins, polysaccharides, etc. acting as « cements »

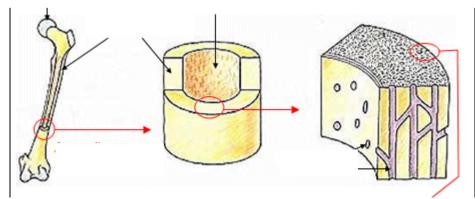
Depends on the location in the body!

Introduction – human hard tissue – 3D structure

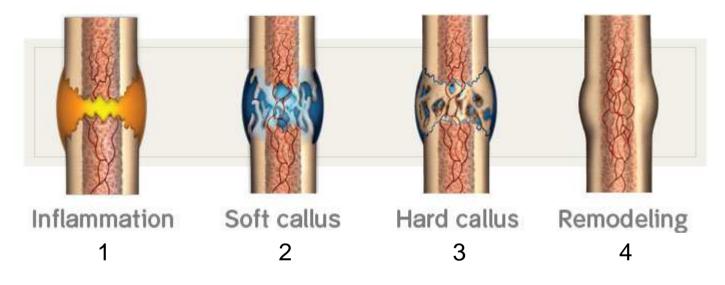
Cancellous or trabecular or spongy bones -> characterized by porous structure (tendons, ligaments attachment, vascularization, etc.)



➤ Cortical bones → characterized by a dense structure, with much higher strength in the loading direction (best combination of strength and modulus)

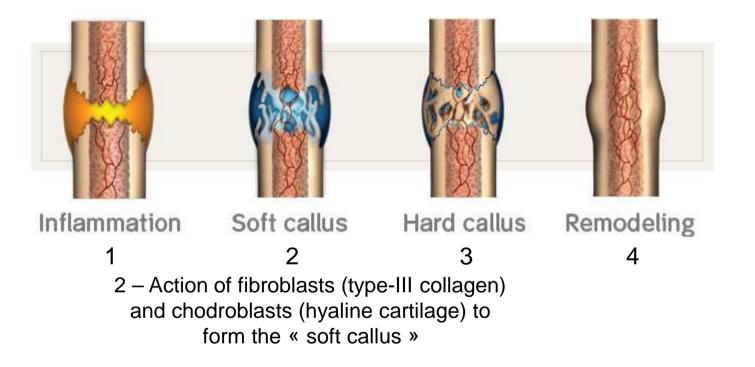


Introduction – Natural healing of hard tissues

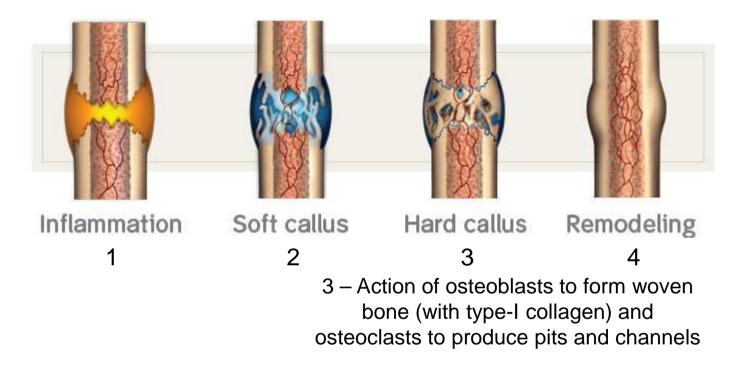


1 - Hematoma and inflammation around the broken bone ends

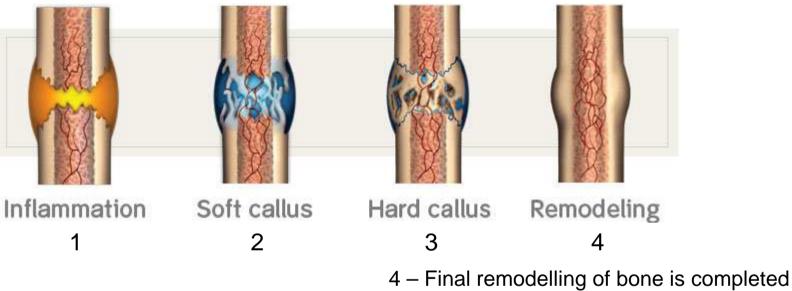
Introduction – Natural healing of hard tissues



Introduction – Natural healing of hard tissues



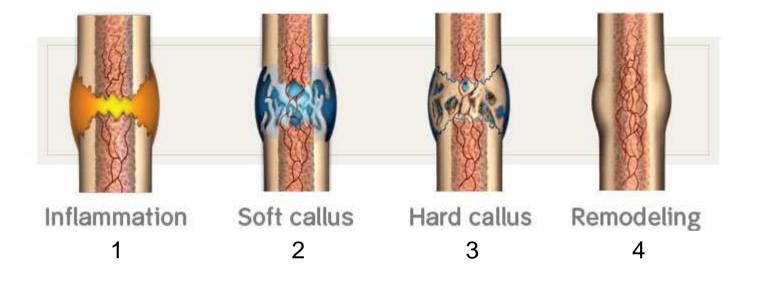
Introduction – Natural healing of hard tissues



by deposition of compact bone by osteoblasts in resorption pits prepared by osteoclasts



Introduction – Natural healing of hard tissues



- Limits : Direct healing occurs when the gap between bone ends is < 2mm
- For larger areas of bone loss, surgeons need to intervene to bridge the skeletal defects

Introduction – Biocompatiblity

- > See : R. Luginbuehl, May 12, 14:15
- Ability of a material to function satisfactory without any detrimental effect on the tissues surrounding it or any deterioration of the material itself

Three important aspects :

- Biochemically compatible, non-toxic, non-irratitive, non-allergenic and noncarcinogenic
- Mechanically compatible with surrounding tissues
- There must be bio-adhesiveness between the material and the surrounding tissues



Type of biomaterials

	BIOINERT	BIOACTIVE
Natural		Autograft, allograft, xenograft
Ceramic	Alumina, Zirconia	Calcium phosphates ceramics, bioglasses
Polymer(*)	PE, PEEK	Polycaprolactone, Polylactide, Polyglycolide
Metal(**)	Au, Ti, 316L	Mg alloys
(*) See E. De Barra – 14:45 (**) See M. Attalah – 11:30		



Type of biomateria	s	
	Advantages	Disadvantages
Natural	Biocompatible, osteoinductive, osteoconductive, non-toxic, no immunological problems	Additional surgical operation, time consuming, risk of disease transmission, availability
Ceramic	Biocompatible, osteoconductive, bond to bone (HA and TCP)	Poor mechanical properties
Polymer	Biodegradable, adjustable degradation rate, easy to process	Degradation products → inflammatory reactions, higher mechanical strength needed
Metal	Bioinert, high mechanical strength	Poorer biological properties

Type of bioceramics

- Since 1965-1970, ceramics are intensively used as bone substitutes, orthopaedic prosthesis (knee, hip) and dental tissues replacement (implants and prosthesis).
- No ceramic is able to associate both adapted mechanical properties and biological interface with bone
 - Alumina and zirconia lead to the formation of fibrous tissue at the interface with bone
 - Calcium phosphate ceramics have poor mechanical properties

Two categories of BIOCERAMICS

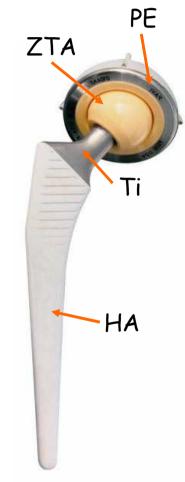
- □ Bio-inert (alumina, zirconia) \rightarrow for dense parts (cortical bones, teeth, etc.)
- \Box Bio-active (calcium phosphate) \rightarrow bone filling, porous parts (trabecular bone)



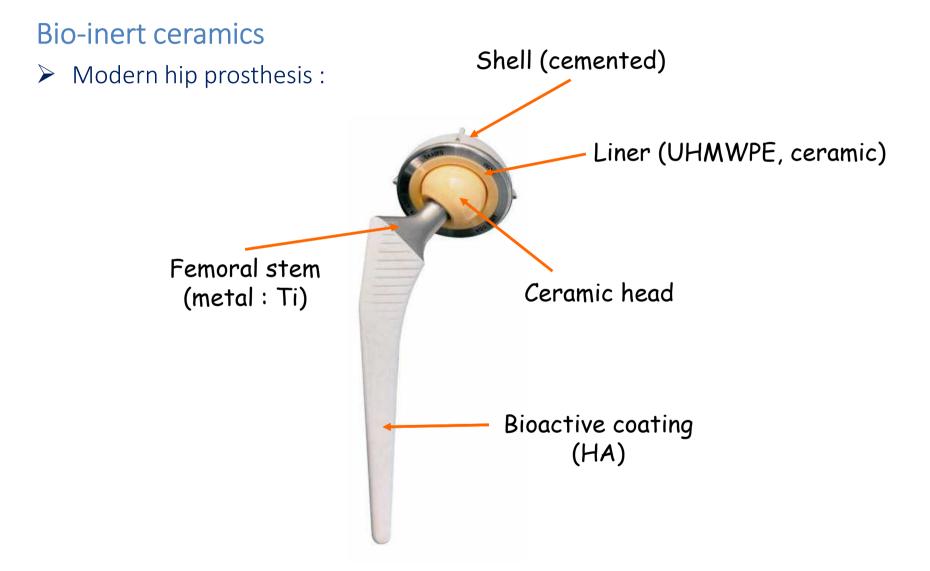
- Mainly : alumina, zirconia + composites ZTA
- > Applications : hip, knee, prosthesis, dental crown, etc.



~ 1.500.000/year

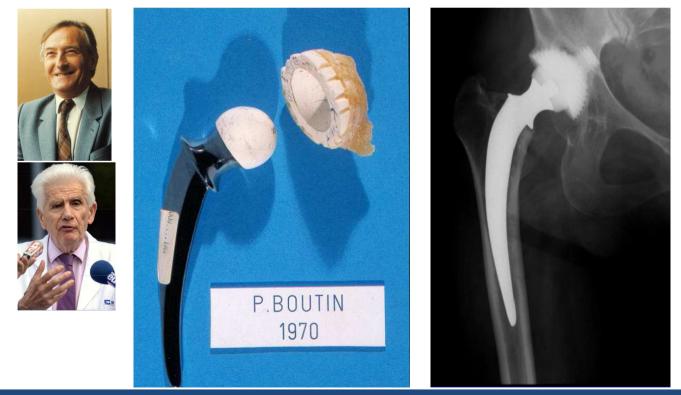






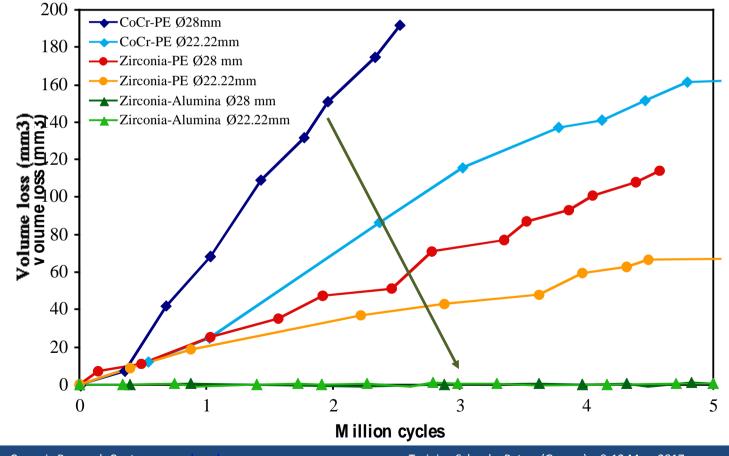


Alumina was first introduced for orthopedic applications in 1970's (Boutin, FR/Daniel Blancquaet, FR), with mixed success (rate of rupture >10%...)





➤ One of the most important advantage with ceramics → high hardness → roughness ~ nm → limitation of the PE wear debris → no inflammation → no disassembly





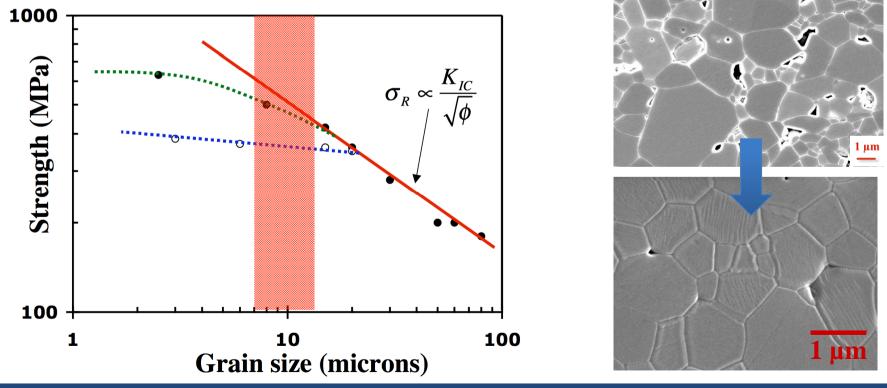
➢ How to increase the strength of ceramics ?

$$\sigma_{R} = \frac{K_{IC}}{\sqrt{\pi \, k \, a}}$$

- 1. Reduce the size of defects
- 2. Increase the fracture toughness

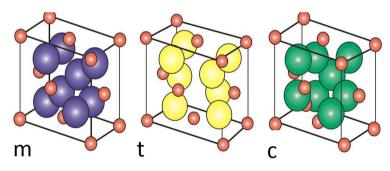


- The reduction of the rate of rupture (0,1%) was related to an improve of the process of elaboration, with a control of the grain size and density.
- Since 1977, alumina parts are post-hipped and even with a mean fracture toughness of around 4 MPa.m^{1/2}, the flexural strength was increased up to 600MPa





- But due to the poor fracture toughness of alumina (K_{1C} = 4MPa.m^{1/2}), it is limited to femoral head of at least 28mm diameter, and certainly not for knee prosthesis.
- > Yttrium Stabilized Zirconia was then considered, for its interesting mechanical properties ($K_{1C} > 6-12$ MPa.m^{1/2}) and flexural strength > 1000MPa!



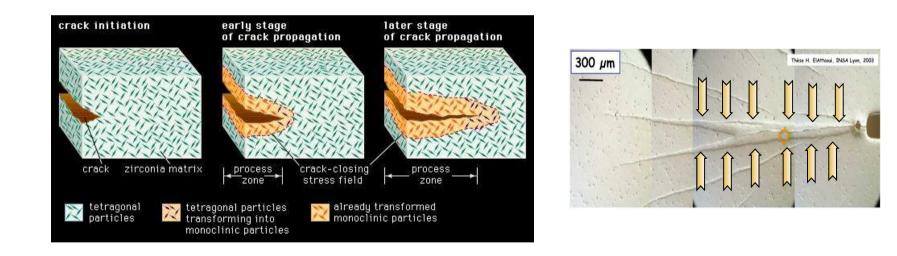
	11	70°C	0°C 2370°C		D°C 26		
-	Monoclinic	Tetrag	gonal	Cubic	Me	Iting	-

 Zirconia : mechanism of reinforcement : transformation toughening (t -> m) (Garvie, 1975)



 Zirconia : mechanism of reinforcement : transformation toughening (t -> m) (Garvie, 1975)

 $t \rightarrow m$: volume change (3-5%)



Before 2001 : rate of rupture < 0,1%, manufacturing of femoral head with a small diameter</p>

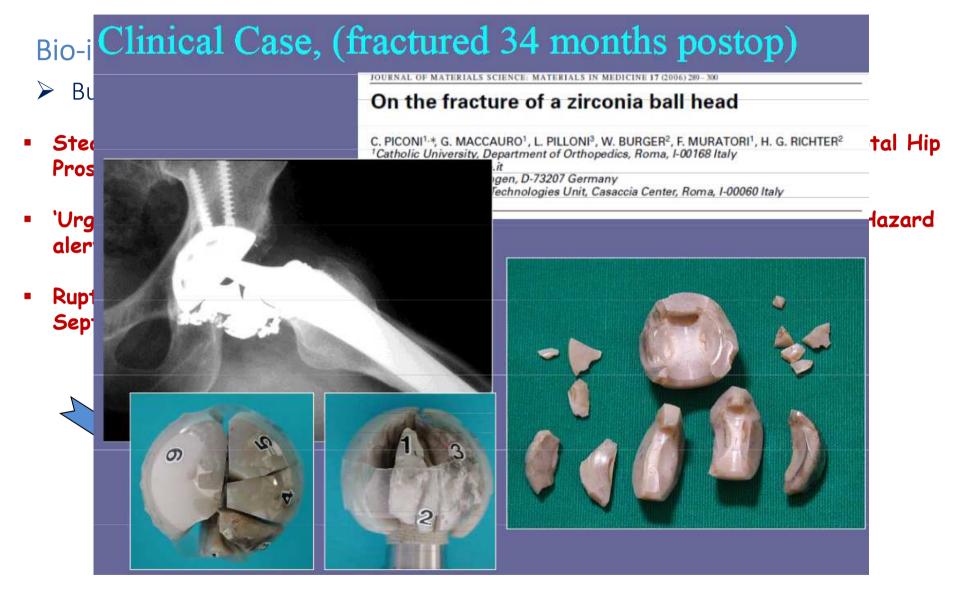


But : controversial success after more than 20 years of clinical test!

- Steam Re-Sterilization Causes Deterioration of Zirconia Ceramic Heads of Total Hip Prostheses, May 21, 1997, FDA (USA)
- 'Urgent information on spontaneous disintegration of zirconia femoral heads: Hazard alert', 23 August 2001, Therapeutic Goods Administration (Australia)
- Ruptures de têtes des prothèses de hanche en céramique de zircone lots TH, Septembre 2001, AFSSAPS (France)

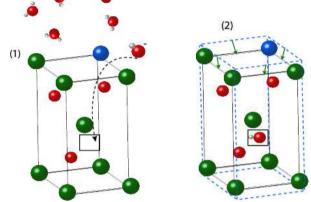
Change of sintering process (tube furnace) Modification of the microstructure Aging (very fast, unwaited) also in vivo! Subcritical crack growth → Ruptures (up to 37%)



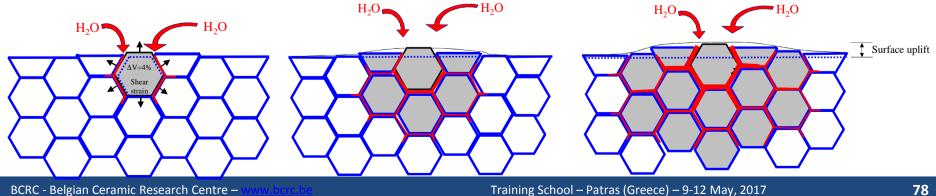




> Diffusion of OH⁻ ions in the tetragonal network, accelerated with Y-TZP due to lack of oxygen (Y³⁺)



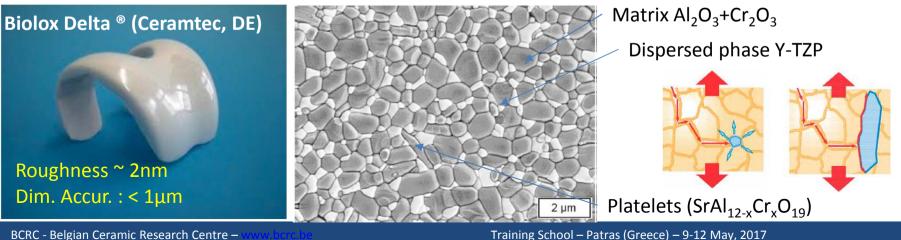
 \succ Destabilization of grains in surface to monoclinic phase \rightarrow increase of volume \rightarrow increase of roughness \rightarrow microcracks \rightarrow rupture!





- \succ Ce-TZP or Mg-TZP can solve the problem, with an increase of K_{1C}
- But although this degradation has been demonstrated and indirectly associated with a number of flaws in femoral head ceramic prostheses, nowadays, zirconia was completely abandoned for orthopedic applications

Development of composites composed	Material	K _{1C} (MPa.m ^{1/2})	Strength (MPa)	Hardness (Vickers, MPa)
with zirconia	Alumina	4-5	400-600	1800-2000
toughened alumina	3Y-TZP	6-12	800-1200	1200-1300
Biolox Delta		8,5	1150	2000



79



- HIP prosthesis : cemented (PMMA, for instance) in order to anchor the metal part with the bone
- Since 1986 : coating of HA $(Ca_{10}(PO_4)_6(OH)_2)$ (main constituent of bone)



- Plasma sputtering



- ➢ For dental prosthesis and crowns : strength of material > 600MPa.
- > More than only mechanical considerations, the esthetic aspect is critical
- White to Ivory color of bio-inert ceramics (alumina, zirconia) have encouraged their selection to replace metallic implants and prosthesis.





Micromilling



Laser machining



- Due to ageing of population, bone filling and bone regeneration are a major and daily clinical aspect (more than 700.000 surgical operations / year in Europe!)
- The use of <u>synthetic bone substitutes</u> has greatly developed since 1980 as <u>alternative to autograft</u>
- Most of the commercial products on the market are bi-phasic calcium phosphate porous part, composed with :
 - Hydroxyapatite (HA) (Ca/P ratio = 1,67) Ca₁₀(PO₄)₆(OH)₂
 - β -tricalcium phosphate (β -TCP) (Ca/P ratio = 1,5) Ca₃(PO₄)₂



- For load-bearing applications, surgeons will obviously select inert materials (Ti, Stainless Steel, Co-Cr alloys, alumina, ZTA, composites with polymers...)
- > Calcium phosphate ceramics have poor mechanical properties :

Compressive Flexural strength (MPa) strength (MPa) r		Young modulus (GPa)	Fracture toughness (MPa.m ^{1/2})
600	150-200	140	< 1
600	150-200	100	< 1
3000	400-600	400	4-5
80-200	150-200	15	2-12
	trength (MPa) 600 600 3000	trength (MPa) strength (MPa) 600 150-200 600 150-200 3000 400-600	trength (MPa) strength (MPa) modulus (GPa) 600 150-200 140 600 150-200 100 3000 400-600 400

(*) with 5 to 10% of porosity!

But HA/TCP have good biological properties!



HA/TCP integrate perfectly with bone tissue (BIO-INTEGRATION) without fibrous tissue formation! Indeed, they are chemically similar to the mineral phase of hard tissues in human body!

	Enamel	Dentine	compact bone	ТСР	HAP
Ca	36,1	35	35,5	38,8	45,2
Р	17,3	17,1	17,1	20,0	21,0
CO ₂	3	4	4,4	-	-
Ca/P (molaire)	1,61	1,58	1,60	1,50	1,667



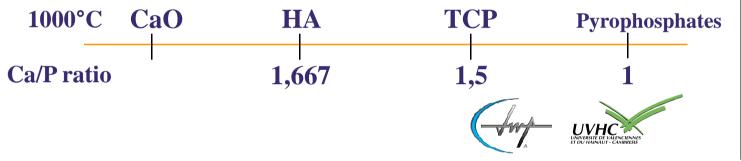
- HA/TCP integrate perfectly with bone tissue (BIO-INTEGRATION) without fibrous tissue formation! Indeed, they are chemically similar to the mineral phase of bones!
- HA/TCP are osteoinductive and osteoconductive : they guide bone cells and promote bone tissue development
- > HA/TCP can be used as **permanent** substitutes either as **bioresorbable** material
- > HA/TCP regulate the operation of bone cells (osteoblasts, osteoclasts)

Bioceramics

Bio-active ceramics : manufacturing

Powder synthesis: mixture of aqueous solution of calcium and phosphate salts, precipitation, calcination
Ca(NO) + (NH) HPO 2 Ca. (PO) (HPO) (OH)

 $Ca(NO_3)_2 + (NH_4)_2HPO_4 \rightarrow Ca_{10-x}(PO_4)_{6-x}(HPO_4)_x(OH)_{2-x}$



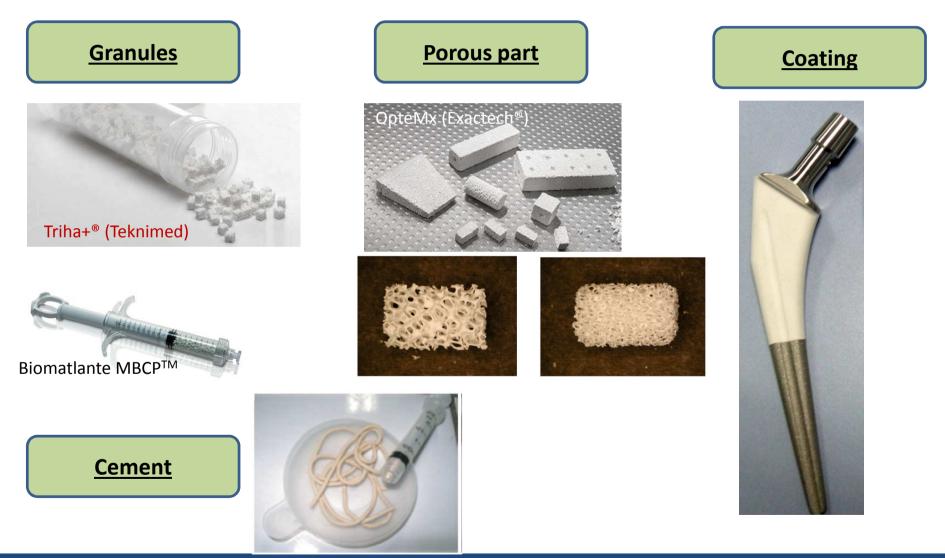


> <u>Sintering</u>

- HA ~ 1230-1260°C
- β -TCP ~ up to 1125°C (to avoid α -TCP formation)
- To get dense bi-phasic parts → need for non-conventional sintering process (microwave, post-HIP, SPS)



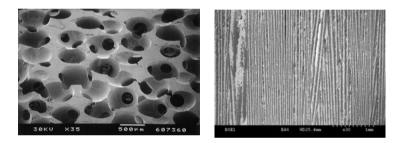
Bio-active ceramics : actual "shapes"



Bioceramics

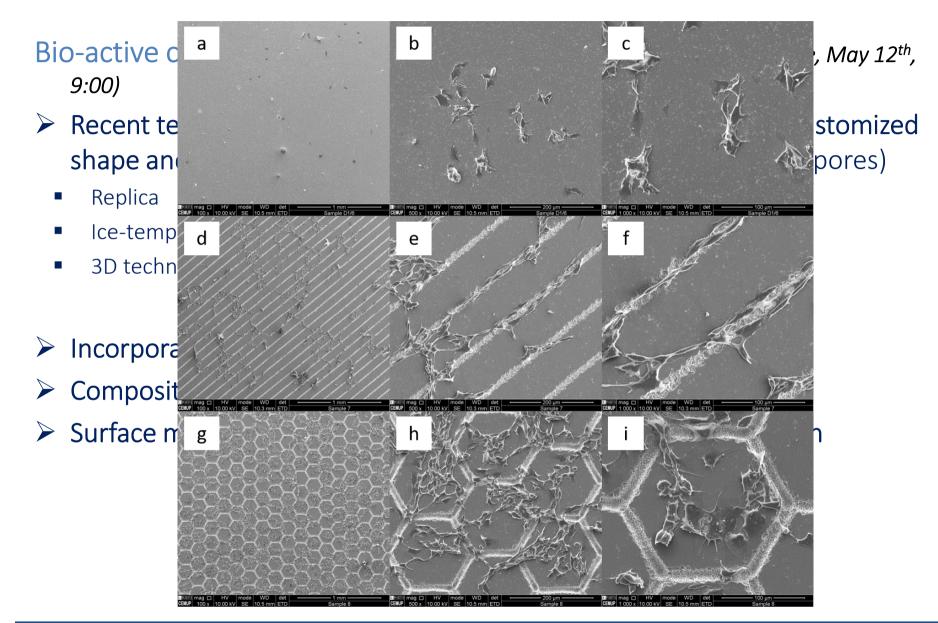
Bio-active ceramics : new trends/ fields of R&D (see Prof. A. Leriche, May 12th, 9:00)

- Recent technologies to design porous scaffolds, with complex/customized shape and controlled porosities (size, shape, interconnection of pores)
 - Replica
 - Ice-templating
 - 3D technologies



- Incorporation of stem cells, growth factors, antibacterial agents
- Composites polymer (PCL, PLA-PGA, PEKK)/ Bioceramics
- Surface modifications to enhance cells adhesion and proliferation

Bioceramics



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GLASS & BIOGLASS



What means « glass »?

Definition

Either a material or an object (to drink, a part of spectacles, ...)

- Internet: non-crystalline amorphous solid
- <u>Dictionary</u>: a hard, brittle, non crystalline, more or less transparent substance produced by fusion

In general: obtained by supercooling of a liquid: the solid material keeps some properties of the liquid

non crystalline mineral = amorphous

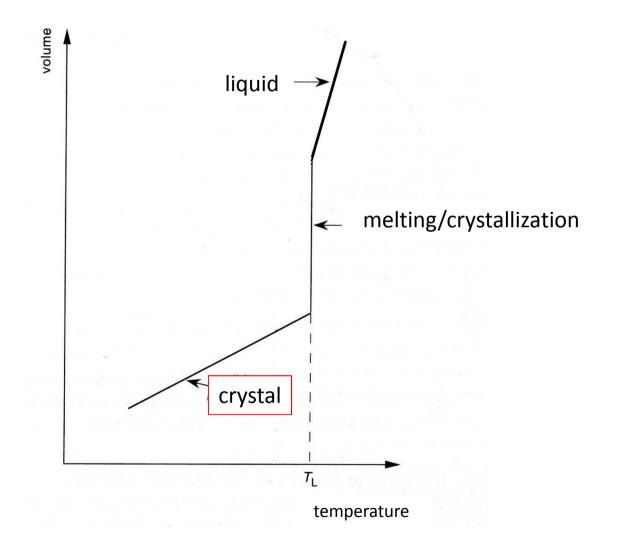
processing:

powder mixture \rightarrow high temperature \rightarrow liquid \rightarrow shaping \rightarrow cooling

Homogeneity and Isotropy

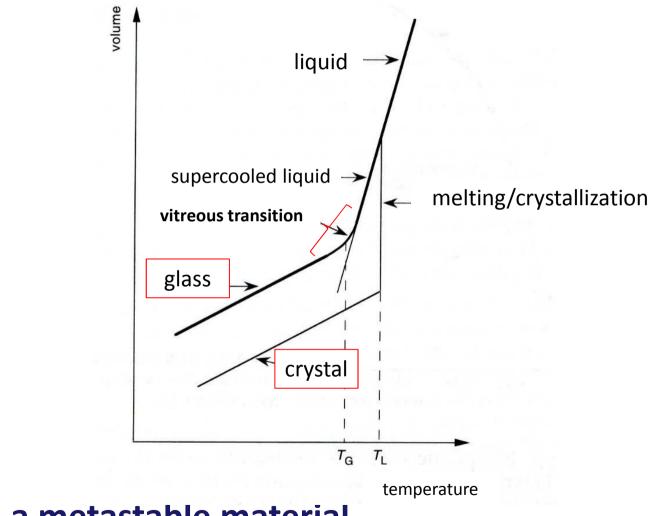


What means « glass »?





What means « glass »?



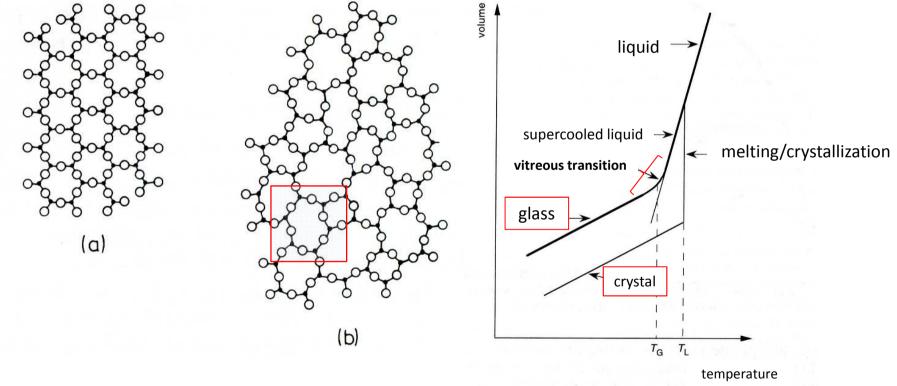
glass is a metastable material

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More scientific definition:

<u>*Glass*</u>: a non crystalline solid characterized by a glass transition phenomenon

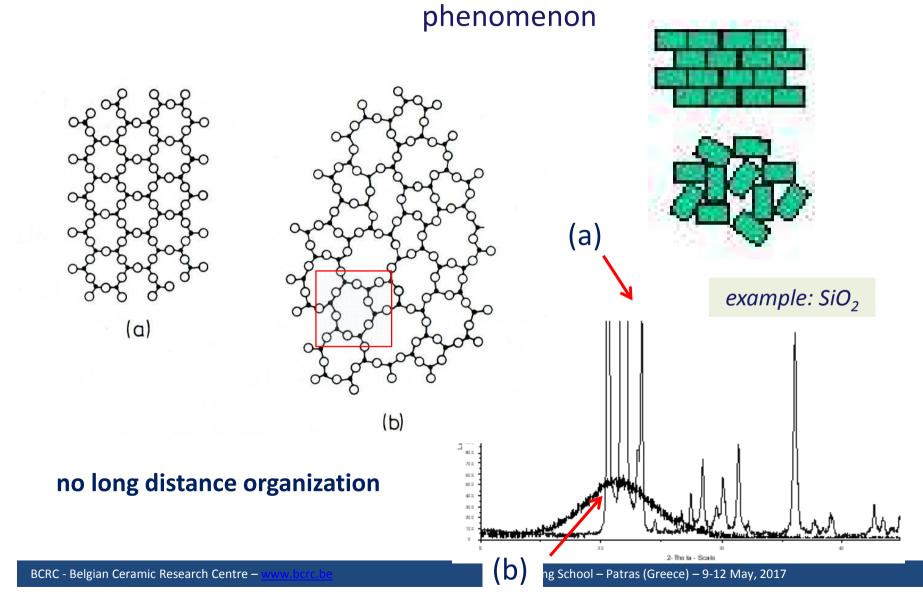


no long distance organization



More scientific definition:

<u>Glass</u>: a non crystalline solid characterized by a glass transition





Glass forming (a)

From liquid

- Idea: keep the structure disorder of a liquid phase
- Most of the melted <u>substances</u> rapidly crystallize at the melting point, even if the cooling rate is very high
- Some substances form when melting very <u>viscous liquids</u> that will crystallize slowly under the melting point
- In such a case, if the cooling rate is enough high, the liquid will freeze without crystallization and form a glass

→ which liquids have a high viscosity? why?

 \rightarrow "organization" within liquids



Glass forming

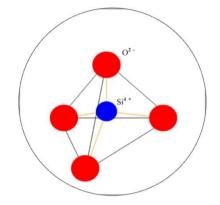
Liquid freezing

The glass making substances are:

a) elements : P, S and Se

b) oxides : SiO₂, GeO₂, B₂O₃ and P₂O₅ are called « network former ions »: they can form tridimensional networks

III	IV	V	VI
В	С	Ν	0
AI	Si	P	S
Ga	Ge	As	Se
In	Sn	Sb	Те
TI	Pb	Bi	Ро





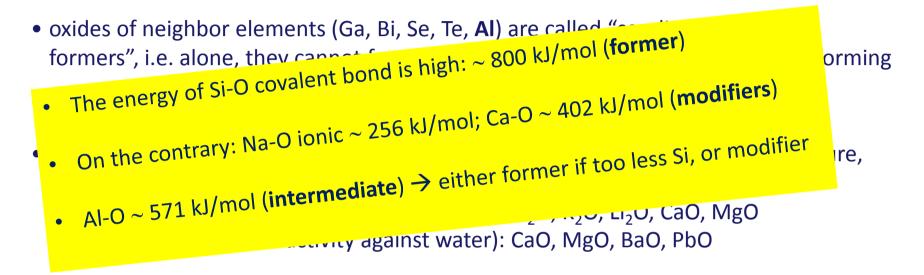
 As_2O_3 and Sb_2O_3 , (As³⁺ et Sb³⁺) are network formers if the cooling rate is very high

- oxides of neighbor elements (Ga, Bi, Se, Te, Al) are called "conditional network formers", i.e. alone, they cannot form glass but if they are associated with non forming oxides (e.g. CaO-Al₂O₃) → they are also called "intermediate"
- Electro-positive cations (Na⁺, K⁺, Ca²⁺, Mg²⁺, etc.) do not take place in the structure, they are called "modifier" → their role:
 - ✓ melting (\downarrow T_{melting} of silica ~ 1700°C) : Na₂O, K₂O, Li₂O, CaO, MgO
 - ✓ <u>stabilizers (</u>↓ reactivity against water): CaO, MgO, BaO, PbO

Oxygen can be substituted by other anions (example S²⁻ or N³⁻) \rightarrow sulfide glasses or oxy nitride glasses



 As_2O_3 and Sb_2O_3 , (As³⁺ et Sb³⁺) are network formers if the cooling rate is very high



Oxygen can be substituted by other anions (example S²⁻ or N³⁻) \rightarrow sulfide glasses or oxy nitride glasses

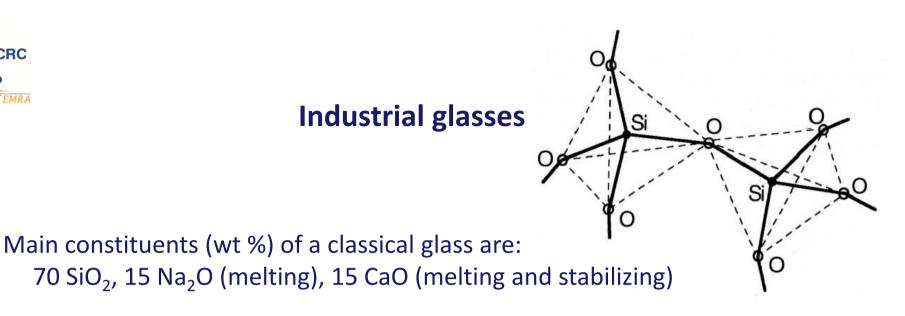


> 95 % of industrial glasses are silicates, however other glass compounds exist:

- With S (binary As–S, As–Se, P–Se, Ge–Se, ...)
- Halogenides (BF₂, ZnCl₂)
- Molten salts (sulfates, carbonates, phosphates, acetates, ...)
- Aqueous solutions of salts, acids, bases, ...
- Organic compounds (methanol, ethanol, glycerol, glucose, ...)
- Organic polymers (PE, PVC, ...)
- Metals (some hyper cooled alloys)

Generally, for those systems, the ranges of compositions are much more limited





Composition changed very few in centuries (except purity)

(wt %)	Modern glass	Palestine (4 th century)
SiO ₂	72.0	70.5
Na ₂ O	13,5	15.7
K ₂ O	0.5	0.8
CaO	10.0	8.7
MgO	2,0	0.6
Al ₂ O ₃ Fe ₂ O ₃	2.0	2.7
Fe ₂ O ₃	0.05	0.4

\rightarrow better **optical properties**

Training School – Patras (Greece) – 9-12 May, 2017



Multiple components oxide glasses

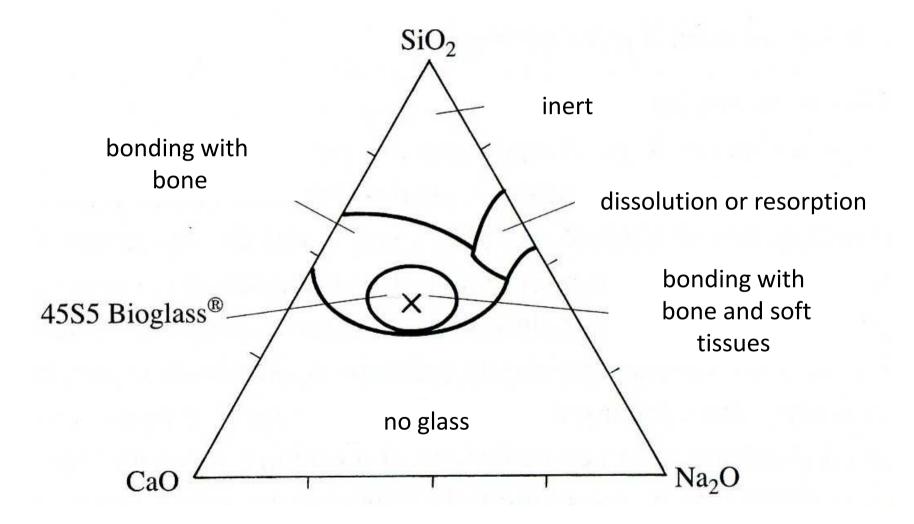
Glass	SiO ₂	B_2O_3	P_2O_5	Al_2O_3	CaO	MgO	Li ₂ O	PbO	K ₂ O	Na ₂ O
Silica	99,5									
Vycor®	96,3	3		0,4					0,2	0,2
Soda-lime (windows)	72			1	9	4			0,2	14
Soda-lime (bottles)	72			2,0	10	2			0,5	13,5
Soda-lime (lamps)	73,6			1,0	5,2	3,6			0,6	16
Low lead content (< 24%)	63	0,2		0,6	0,3	0,2		21,0	6,0	7,6
High lead content (X rays)	35							58,0	7,2	
Borosilicate (low α)	80,5	12,9		2,2					0,4	3,8
Borosilicate (low σ)	70,0	28,0		1,1			1,2		0,5	
Alumina-silicate	57,0	4,0		20,5	5,5	12,0				1,0
Bioglass [®] – ex : 45S5 [®]	46,1		2,5		26,9					24,4

not very stable because very few Si-O bonds

 σ electrical conductivity n refraction index ρ density

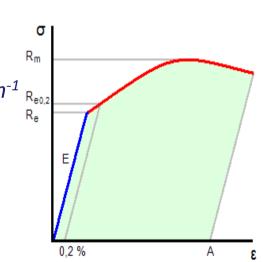


Bio-reactivity domain of glasses





- 1. Viscosity (η) (for shaping): glass transition temperature (T_g) & annealing temperature
 - Density: ~ 2.2 g.cm^{1/3}
 - Mechanical resistance: $\sigma_{F} \sim 30$ to 100 MPa; $K_{Ic} \sim 0.7$ to 1 MPa. $m^{\frac{1}{2}}$;
 - Elastic coefficients ($E \sim 150$ GPa, $v \sim 0.2$ to 0.3) & CTE
 - Electrical properties: insulator at room T ~ 10^{-9} à $10^{-8} \Omega^{1} m^{-1}$ $\uparrow \sim 10^{19}$ at about 1200 °C
 - Optical properties (transparency)
 - Thermal conductivity: 0,8 à 1,4 W.m⁻¹K⁻¹
 - 2. Chemical properties (corrosion resistance)



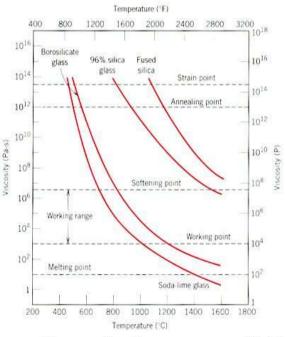


Viscosity (η) (for shaping): glass transition temperature (T_g) & annealing temperature
 Important Temperatures

Melting point = viscosity of 10 Pa.s
Working point= viscosity of 1000 Pa.s
Softening point= viscosity of 4x10⁷Pa.s Temperature above which glass cannot be handled without altering dimensions)
Annealing point= viscosity of 10¹² Pa.s.
Strain point = viscosity of 3x10¹³Pa.s Fracture occurs before deformation

1 poise = 1 dPa.s

 $T_g \sim 10^{13}$ to $10^{13.6}$ poises (between strain and annealing points)



- Viscosity decreases with T
- Impurities lower T_{deform}



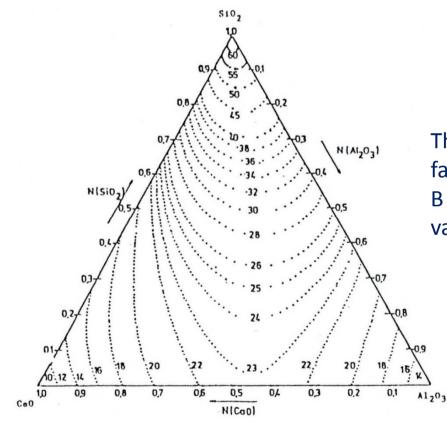
1. Viscosity (η) (for shaping): annealing

quenching and forming induce residual stresses -> annealing

- heating the glass at an uniform T ~ > Tg, during enough time to relax the stresses, then the material is cooled down very slowly
- practically, cooling rate are chosen as a function of part dimensions
 - classically: $v < 5^{\circ}/min$
 - precise optical parts: v < 0,7°/min.



1. Viscosity (η) : how it varies with composition at a given temperature

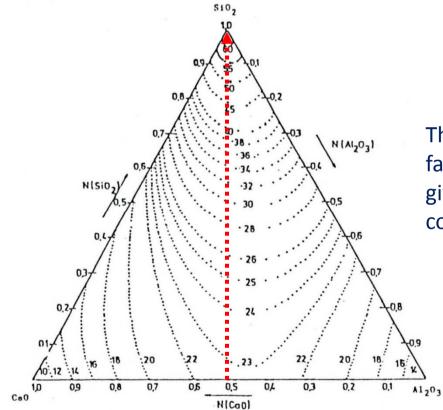


$$\eta = AT \exp\left(\frac{10^3 B}{T}\right)$$

The parameter A is known for a given family of glasses (silicates) \rightarrow therefore B value give a rough idea of how η varies with composition



1. Viscosity (η) : how it varies with composition at a given temperature



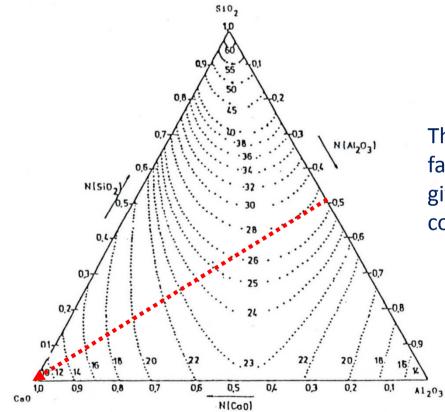
$$\eta = AT \exp\left(\frac{10^3 B}{T}\right)$$

The parameter A is known for a given family of glasses \rightarrow therefore B value give a rough idea of how η varies with composition

 1^{st} example: SiO₂ (network former) ↑ from 0 up to 100%: B (η) increases monotonically



1. Viscosity (η) : how it varies with composition at a given temperature



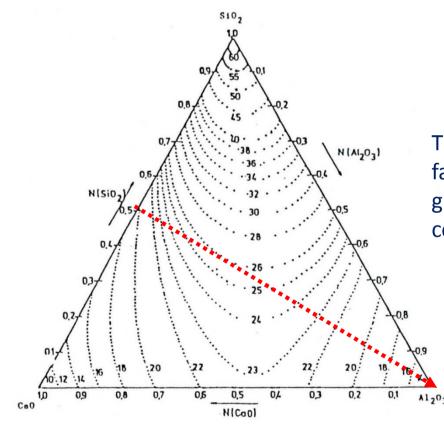
$$\eta = AT \exp\left(\frac{10^3 B}{T}\right)$$

The parameter A is known for a given family of glasses \rightarrow therefore B value give a rough idea of how η varies with composition

 2^{nd} example: CaO (network modifier) ↑ from 0 up to 100%: B (η) decreases ~ monotonically



1. Viscosity (η) : how it varies with composition at a given temperature



$$\eta = AT \exp\left(\frac{10^3 B}{T}\right)$$

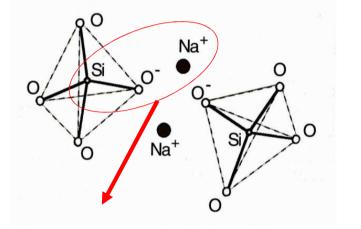
The parameter A is known for a given family of glasses \rightarrow therefore B value give a rough idea of how η varies with composition

<u>3rd example</u>: Al_2O_3 (intermediate) \uparrow from 0 up to 100%:

B (η) increases, reaches a maximum, then decreases: (depending on to the location of Al³⁺ in the glass network)



2. Chemical properties (corrosion resistance) – ex soda-lime glass

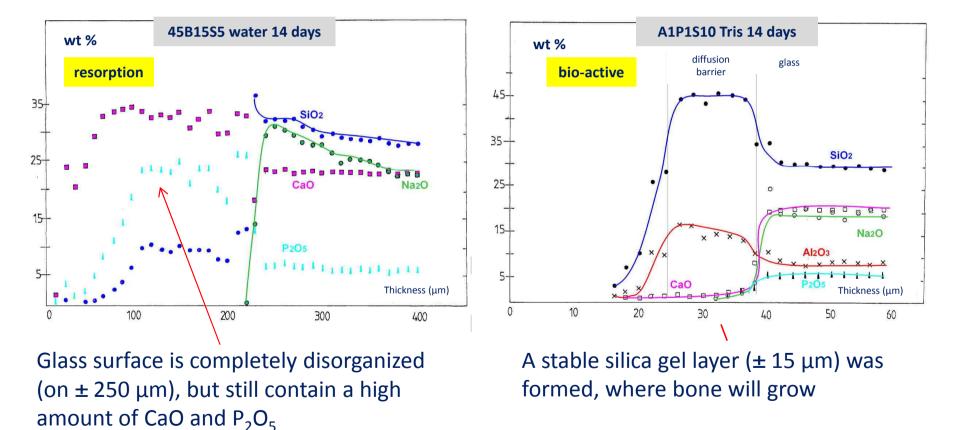


 $-Si-O^{-}Na^{+} + H_2O \rightarrow Si - O^{-}H^{+} + Na^{+}OH^{-}$

<u>With aqueous solutions</u>: exchange between the modifiers ions and protons \rightarrow increase of pH; then without pH control, elimination of silicate anions (which are soluble)



2. Chemical properties (corrosion resistance) – example of bio-glasses



Types of bioactive glasses



1969 : discovery of the first bioactive glass (Prof Larry Hench, Univ. Florida)

45S5 : known as Bioglass[®] 45S5

Bioactivity depends on: composition (Ca or P are not necessary), **solubility** of constitutive ions, **texturing**, **structure**, etc.

Commercial name	Composition (mol %)	Process	
45S5 (Bioglass [®] , PerloGlas [®] , Novabone [®] , Biogran [®] , Novamin [®])	46.1 SiO ₂ -24.4 Na ₂ O-26.9 CaO-2.6 P ₂ O ₅	Melting	
S53P4 (BonAlive [®])	53.8 SiO ₂ -22.7 Na ₂ O-21.9 CaO-1.7 P ₂ O ₅	Weiting	
13-93	54.6 SiO ₂ -6 Na ₂ O-22.1 CaO-1.7 P ₂ O ₅ -7.9 K2O-7.7 MgO		
58S	60 SiO ₂ -36 CaO-4 P ₂ O ₅		
S7030C	70 SiO ₂ -30 CaO	Colord	
MBG95	85 SiO ₂ -10 CaO-5 P ₂ O ₅	Sol-gel	
B75-Sr5	75.5 SiO ₂ -21.6 CaO-2.9 SrO		

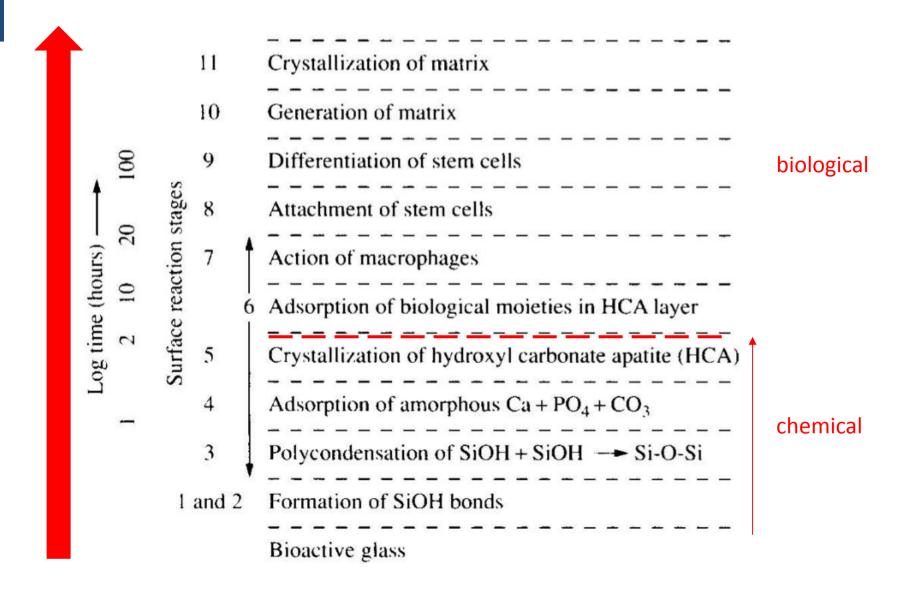
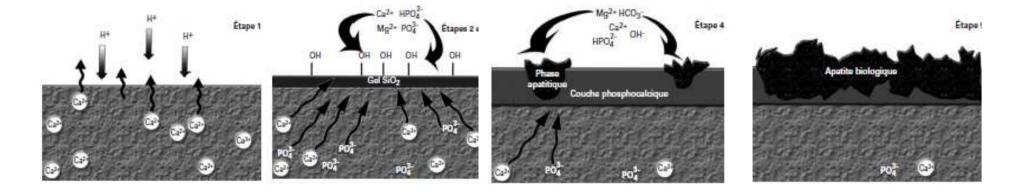


Fig. 3. Sequence of interfacial reactions involved in forming a bond between tissue and bioactive glasses.

Mechanism of interaction



First step: exchange of H⁺ from biological medium with modifier ions at the glass surface → silanol formation, medium pH increases If P is present, could also leave the glass surface Step 2 : Increase of pH → rupture of Si-O-Si bonds of the glass network by hydrolysis, giving soluble $(SiO_4)^{4-}$ and formation of more Si-OH at the surface

Step 3: Polymerization of a silica gel layer by silanol condensation at the surface \rightarrow the bioactive surface is poor in terms of alkaline and/or alkaline-earth ions <u>Step 4</u>: Migration of Ca²⁺ et PO_4^{3-} (both coming from the biological medium and/or the glass) through the SiO₂ layer to the glass surface \rightarrow the surface becomes rich in calcium and phosphorus

<u>Step 5</u>: Nucleation of calcium phosphates – incorporation of OH⁻ and $CO_3^{2^-}$ from the biological medium – partial crystallization of a HAC layer

Processing & applications

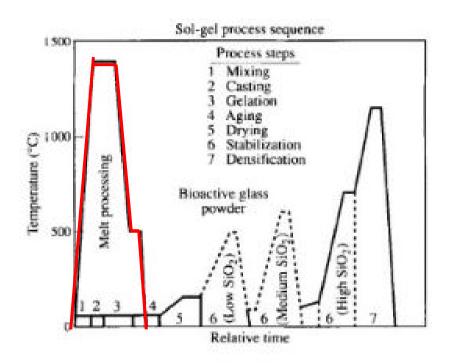


Fig. 5. Processing steps in making bioactive gel-glasses by the sol-gel method.⁷⁴

Hench's 45S5 has been implanted to more than one million patients from its discovery <u>Monoliths:</u> orbital and jaw bones restauration, intern ear bones

<u>More common: as particles</u>, i.e. Perioglass[®] commercialized by NovaBone (USA), as synthetic bone substitute to regenerate jaw bone, stabilize healthy teeth or allow to place a metal implant, also as bone filling in orthopedic surgery

<u>From 2004</u> \rightarrow 45S5 is added in toothpaste (commercialized by GSC from 2010) to reduce the dental hypersensitivity

Very few coatings tests

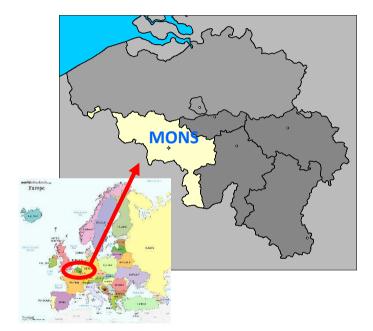




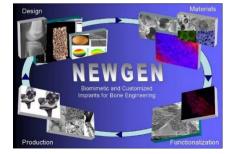




Thank you for your attention!







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