

Bone: structure and properties... and how to mimic it

ADVANC

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SUMMER SCHOOL Ceramic and Glass Science & Technology Application to Bioceramics and Bioglasses

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Structure of bone

- Internal support system in all higher vertebrates
- Flat bones
 - Skull bones, Mandible, Ileum
- Long bones
 - Tibiae, Femur, Humerus
- Mineralized living tissue of marked rigidity and strength while still maintaining some degree of elasticity





Structure of bone

Functions of bone

- Mechanical
 - Support and site of muscle attachment for locomotion
- Protective
 - For vital organs and bone marrow
- Metabolic
 - Reserve of ions for the entire organism (especially Ca and P)
 - Hematopoiesis





Structure of boneConstituents of bone

- Cells
 - Osteoblasts
 - Osteocytes*
 - Osteoclasts
 - Bone lining cells
- Mineralised extracellular matrix
 - Highly substituted hydroxyapatite
 - Organic compounds
 - Type I collagen (90%)
 - Glicoproteins
 - Proteoglicans



* Osteocytes are osteoblasts that have been entraped into the extracellular matrix





Compact bone (dense or cortical) Trabecular bone (cancellous or spongy bone) Periosteum Endosteum







Schematic drawing of the bone architecture. Both cortical and spongy bone can be distinguished. The osteons of cortical bone are displayed including the haversian channels that contain blood vessels and nerves. The periosteum (highly vascularised membrane that covers the bone surface) can also be seen.

Adapted from a figure by the Department of Kinesiology & Physical Education, Lethbridge University.



Table 1. Comparison between structures that compose skeleton [9]

Structure	Water Composition	Proteoglycan s Composition	Collagen Composition	Mineral Composition
Tendon/Ligam t	Moderate	Low	High	Low
Cartilage	High	High	Low - Moderate	Low
Bone	Low	Low	Moderate	High



Distribution of calcium, magnesium, and phosphate in the body of a 70-kg adult* [2]

Compartment	Calcium (g)	Magnesium (g)	Phosphate (g)
Bones and teeth	1300 (99)	14.0 (54)	600.0 (86)
Extracellular fluid	1 (0.1)	0.3 (1)	0.2 (0.03)
Cells	7 (1.0)	12.0 (46)	100.0 (14)

Note: *Most of calcium is in bone and almost half of magnesium is in cells. Phosphate, as the principal counter ion to calcium and magnesium, has an intermediate proportional distribution. Number in parentheses is the percentage of total content for that mineral.



Mechanical properties of cortical and trabecular (cancellous) bone

Property	Cortical bone	Cancellous bone
Compressive strength (MPa)	100-230	2-12
Flexural, tensile strength (MPa)	50-150	10-20
Strain to failure (%)	1-3	5-7
Fracture toughness (MPam ^{1/2})	2-12	-
Young's modulus (GPa)	7-30	0.5-0.05





Osteoblast and bone formation

Production of matrix

- Recruitment of osteoprogenitor cells
- Proliferation
- Differentiation into osteoblasts
- Osteoblasts
 - Secrete ECM into which mineral is selectively deposited
 - Control the composition of the matrix



Osteoblast and bone formation

Composition of the organic extracellular ✓ Scaffolding

matrix

✓Type I collagen (90%)

✓ Proteoglycans

✓ Glycoproteins

✓ Osteonectin, Bone sialoprotein, Osteopontine, Fibronectine

\checkmark G-carboxy glutamin acid containing

proteins

✓ Osteocalcin, Matrix gla-proteins

✓ Enzymes

- ✓ Alkaline phosphatase, Collagenase, Proteinases
- ✓ Growth factores
 - \checkmark FGFs, IGFs, TGF β s, BMPs
- ✓ Proteolipids

✓ Provides appropriate concentrations of phosphate ions to initiate mineralisation

 \checkmark Binds and orients other

on HA deposition

proteins that play a role









Figure 2. Hematopoiesis pathway



Structure of bone

Bone remodelling

Throughout life, bone mass is continuously in a remodelling process







Bone remodeling osteoblasts and osteoclasts differentiation





Bone remodelling process. Osteoblasts depend on the osteoclasts to resorb older bone ahead of them. As the bone is resorbed by the osteoclasts, there is the release of cytokines (signalling molecules) that attract osteoblasts and induce them to start laying down new bone tissue. The osteoblasts then incorporate proteins into the bone structure. Once that bone is resorbed by osteoclasts again the proteins are released and act as signals to the osteoblast to return and lay down more bone. This tight coupling of formation and resorption is necessary to prevent a disorganized bone structure from being established. Adapted from *The Science Creative Quarterly*, by Jen Philpot.

Bone matrix composition



The many scales of organization in natural bone (Taton, 2001).













Figure 1. Collagen organization (30).



Collagen molecule: 300 nm long x 1.5nm diameter Collagen alpha chain Assembly into microfibril Assembly into mature collagen fibril Aggregation of collagen fibrils to form a collagen fibre Collagen from rat tail

Figure 4. Collagen structure. Adapted from the source. Source: www.orthoteers.com







Energy minimized structure of 24mer collagen triple helix















Figure 1: The unit cell of hydroxyapatite (45).







Figure 1. The Tissue Engineering Paradigm (19).





Schematic representation of cell based bone tissue engineering. A fraction of bone marrow obtained by biopsy from the patient will be harvested, and cells will be expanded in vitro. The cells will then be seeded on adequate scaffolds and further cultured, eventually being led to express adequate phenotypic character. The tissue engineering construct will then be implanted back to the patient to heal the bone defect.



Case Study 1

Ceramic based granular structures for bone tissue engineering and drug delivery



nanophased HA agglomerates after spray drying







Biological *in vitro* studies on 2D and 3D nanoHA structures



– Confocal Microscopy images of MG-63
Cultures on granules and disks after
3 days (A,B) e 6 ddays (C,D).
Biological *in vitro* studies on 2D and 3D nanoHA structures

A- Alkaline phosphatase activity on granules and disks after 6 days B – Genetic expression of MG-63 on granules and disks after 6 days





nanoHA granules in contact with Endothelial cells and osteoblasts Marta Laranjeira



M^a Helena Fernandes Confocal microscope images of 7d days co-culture of endothelial cell, and osteoblasts

Co-culture 7d



Endothelial 7d



in vitro Biological studies on Nano HA porous granules of HbmMSC's and endothelial cells. CO-



Day 21 HMSC



HDMEC e HMSC in monoculture e co-culture on granules after 21

Co-culture Day 21



HMSC Day 21



NanoHA granules provide adequate environment for adhesion. migration and differentiation of endothelial and HbmMSC, showing to be a promising material for bone regeneration

HDMEC e HMSC in monoculture e co-culture on granules after7,14 and 21 days





Osteomyelitis



Illustration of hematogenous osteomyelitis in a tubular bone (Kibiuk, 2010).







Hydroxyapatite/ Collagen scaffold

Polyurethane Sponges were impregnated with slurries containing ceramics (mixtures of water, HA and surfactant) and heat-treated

Type I collagen solution was prepared from bovine Aquiles tendon , empregnating the HA sponges

Collagen was crosslinked with a mixture of N-(3-dimetilaminopropil)-N'-etilcarbodiimide hydrocloride (EDC) and N-hydroxisuccinimide (NHS)







Osteomyelitis

Current treatment





Organisms frequently isolated from osteomyelitis cases based on patient age. Adapted from (11).

Organisms Frequently Isolated in Osteomyelitis Based on Patient Age		
Infants (<1 year)	Children (1 to 16 years)	Adults (>16 years)
Group B streptococci	Staphylococcus aureus	Staphylococcus epidermidis
Staphylococcus aureus	Streptococcus pyogenes	Staphylococcus aureus
Escherichia coli	Haemophilus influenzae	Pseudomonas aeruginosa
		Serratia marcescens
		Escherichia coli



Scanning Electron Microscopy (SEM) depicted numerous clumps of *S. aureus*. 32000x magnification





Figure 1: Characteristic gram-positive cell wall and *S. aureus* peptidoglycan. (A) The gram-positive cell wall. (B) *S. aureus* peptidoglycan. NAM: *N*-acetylmuramic acid. NAG: *N*-acetylglucosamine. Gly: Glycine.





Figure 1: Pathogenic factors of *S. aureus*, with structural and secreted products both playing roles as virulence factors.

(A) Surface and secreted proteins. (B, C) Cross-sections of the cell envelope. TSST-1: toxic shock syndrome toxin 1



Vancomycin



Low minimal inhibitory concentration (MIC, 1 µg/mL);

Low cytotoxicity for osteoblasts.



Chemical structure of vancomycin (Williams et al, 1999).

Novel approach for the treatment of Osteomyelitis



nanoHA and (nanoHA + Type I collagen composite) scaffolds for bone regeneration and for controlled release of Vancomycin Patent application pending.









Bacterial adherence to nanoHA

Maria Pia Ferraz, Liliana Grenho, Marta Ribeiro



Two examples of the number of adherent bacteria per mm² for each material at different adhesion times (p-value according to Turkey HSD test).

S. aureus ATCC 25923

S. aureus MRSA isolated from an orthopaedic infection

Bacterial adherence to nanoHA





Influence of the presence of proteins on bacterial adherence to nanoHA

FBS-mediated bacterial adhesion

Colony forming units counting

Graphs showing the influence of adsorbed FBS on the adhesion of *S. aureus* MSSA (A)and *S. aureus* MRSA (B) to nanoHA sintered at 725°C and at 1000°C.

FBS

Without adsorbed protein



Influence of the presence of proteins on bacterial adherence to nanoHA

influence of adsorbed FBS on the adhesion of *S. epidermidis* RP62A (C) and S. epidermidis ORT (D) to nanoHA sintered at 725°C and at 1000°C.









SEM



Vancomycin release



* Represents a statistical significant difference when compared to nanoHA and nanoHA/collagen granules for each time point (p < 0.05).





Vancomycin bioactivity

<u>24 h</u>



<u>72 h</u>

Lost bioactivity? Limit of detection?



Vancomycin bioactivity



Total number of *S. aureus* in the absence of vancomycin, for 0 and 24 h of incubation, and in the presence of vancomycin after 24 h of incubation. * represents a statistical significant difference when compared with *S. aureus* 0 h and *S. aureus* 24 h (p < 0.05).

S. aureus adhesion on granules



* Represents a statistical significant difference when compared to nanoHA granules (p < 0.05).

S. aureus adhesion on granules



SEM



Case Study 2

Collagen based (functionalised) spongy-like scaffolds for bone tissue engineering

INEB SIBLING proteins Functionalized Collagen scaffolds for critical bone defects



Abhishek Sahu, Christiane Salgado e Sandra Rodrigues

Collagen/ nanoHA Scaffolds obttained by "cryogelation" crosslinked by EDC/NHS

- Collagen/ nanoHA biocomposites with immobilized SIBLING proteins for Bone tissue engineering
- (OPN(osteopontin e BSP bone sialoprotein are memebers of SIBLING (Small Integrin-Binding Llgand, N-linked Glycoprotein) family
- In vitro and In vivo studies of activity on functionalized scaffolds for bone formation, angiogenesis and bone remodelling

3D porous Collagen-Nanohydroxyapatite Biocomposite Scaffolds

Abhishek Sahu Christiane Salgado and Sandra Rodrigues



1mm

3D porous Collagen-Nanohydroxyapatite BiocompositeScaffolds

Abhishek Sahu, Christiane Salgado and Sandra Rodrigues



3D porous Collagen-Nanohydroxyapatite Biocomposite Scaffolds



Figure . Scanning electron micrographs (SEM) of the cross-sections of (A) collagen scaffold

(B) collagen-nanoHA (70:30) scaffold,

(C) collagen-nanoHA (50:50) scaffold and

(D) collagen-nanoHA (30:70) scaffold. Magnification: x 200.



3D porous Collagen-Nanohydroxyapatite Biocomposite Scaffolds



Figure 3: Swelling Kinetics of collagen and collagen-hydroxyapatite biocomposi cryogel scaffolds in PBS buffer (A) and (B) in distilled water.



Figure 6: Albumin adsorption on the different composition of Col/nanoHA composites compared to collagen scaffols.



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osteoblast culture (MG63).



human mesenchymal stem cells (hMSC).





3D porous Collagen-Nanohydroxyapatite Biocomposite Scaffolds





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SEM images of cryogels' materials D, E and F col/nanoHA 70:30; G, H and I - col/nanoHA 50:50; J and K - col/nanoHA 30:70) with osteoblast culture after 7days (A, D, G and J), 14 days (B, E, H and K) and 21 days (C, F and I).

Confocal Laser Microscopy images of cryogels' materials (A - collagen; B - col/nanoHA 70:30 ; C - col/nanoHA 50:50; D - col/nanoHA 30:70) with osteoblast culture after 21 days.




3D porous Collagen-Nanohydroxyapatite Biocomposite Scaffolds

CLSM images of cells cultured for 7, 14 and 21 days on collagen and collagen-nanoHA biocomposite scaffolds.



Interactions between materials/ Proteins / tissues

Fibronectin

- Fibronectin plays an important role in cell adhesion, migration and differentiation of different sources of mesenchymal cells;
- In bone, it is involved in the early stages of osteogenesis.

Examples:



Characterization of collagen films

• The chemical composition of collagen films with and without adsorbed proteins were proved by FT-IR.



Characterization of collagen films

• The topography of collagen films with and without adsorbed proteins were evaluated by AFM.



AFM images of gold substrates (A) modified with collagen (B), collagen with adsorbed fibronectin (C) and collagen with adsorbed osteopontin (D). Images were obtained using Tapping Mode and the scan size were 2 µm x 2 µm.

Characterization of collagen films

• The fibronectin and osteopontin adsorption was confirmed by immunohistochemistry with CLSM.



Confocal images of collagen films with adsorbed fibronectin (A) and osteopontin (B). (Control with secondary antibody was negative (data not shown)). Magnification: 40x.

MC3T3-E1 culture on collagen surfaces *In vitro* biological studies

Glass Coverslip

Collagen films on glass coverslips.

MC3T3-E1 culture on collagen surfaces



MC3T3-E1 culture on collagen surfaces *In vitro* biological studies

• MC3T3-E1 metabolic activity was evaluated by Alamar Blue (resazurin).



Metabolic activity of MC3T3-E1 cultured on TCPS, Collagen, Coll + FN and Coll + OPN during 7 days, estimated by Alamar Blue assay. Metabolic activity of MC3T3-E1 was expressed in number of cell per well. α1 (Collagen) and α2 (Coll + FN) represent a significant difference comparing with Coll + OPN after 24 hours of culture, while α3 (Collagen) represents a significant difference comparing with Coll + OPN after 3 days of culture (p<0.05).













MC3T3-E1 culture on collagen surfaces

 The functional activity of MC3T3-E1 cells on collagen surfaces was evaluated by measuring the Alkaline Phosphatase Activity (ALP) normalized with Total Protein Content.



Alkaline phosphatase activity for MC3T3-E1 on TCPS, Collagen films, Coll + FN and Coll + OPN for different time-points.

* represents a significant difference from Coll + FN within the respective time-point while ** represents a significant difference from Coll + OPN within the respective time-point (p<0.05); α1 (TCPS), α2 (Collagen), α3 (Coll + FN), and α4 (Coll + OPN) represents a significant difference comparing the respective material in distinct time-points

(p<0.05).

Collagen/ nanoHA cryogel scaffolds functionalized with SIBLING protein for critical bone defects



Salgado C., Sahu A., Rodrigues S., Monteiro F.J.



Composite cryogels for bone tissue regeneration Type I collagen/nanoHA sponges for bone tissue enginnering





Transmission electron microscopy (TEM)



In vivo characterization



Coll/nanoHA 70:30





Histology



H&E staining of, b) collagen-nanoHA (70:30) scaffold, and d) collagen-nanoHA (30:70) scaffold cultured with osteoblast-like cells for 21 days.

Osteoblast-like cells (O) and collagen (C) were observed in all the scaffolds.



In vivo Materials Characterization



H&E stained scaffold sections after 7 days of *in vivo* implantation.



H&E stained scaffold sections after 30 days of *in vivo* implantation.



Optical micrographs of H&E stained scaffold sections after 30 days of *in vivo* implantation (Coll/nanoHA 50:50). (A) Arrows show presence of nanoparticles inside macrophage cells. (B) Arrow shows presence of giant cells.



Calcium ions:

- play an important role in the regeneration of skin and connective tissue (L. Gennero et al., 2011)
- regulate the activation of the MMPs, which is also required for the migration of the keratinocytes (L.H. Cornelissen, 2004).
- play a vital role in the growth and differentiation of keratinocytes (B. Pomahac et al., 1998)



Multi-functional and biospecific hydrogels for cell delivery

Molecularly designed natural polymers (alginate- and pectin-based) as artificial 3D extracellular matrices

Cell adhesion on RGD-alginate



Evangelista, Biomaterials (2007) Bidarra, Biomacromolecules (2010)

Cell adhesion and migration on **PVGLIG**-RGD-alginate



Fonseca, Acta Biomater (2011) Fonseca, Soft Matter (2013) Fonseca, Biomacromolecules (2014)

Cell differentiation on OGP-PVGLIG-RGD-alginate



Maia, Acta Biomater (2013) Maia, J Control Rel (2014) Maia, Acta Biomater (2014)

3D Printing for skin Tissue Engineering



3D bioprinting system with syringes containing different hydrogelbased materials with entrapped skin cells

UV crosslinkable, biodegradable RGD-pectin hydrogels for skin regeneration



Pereira, **Granja** +, Nanomedicine (2013)





Neves, Granja +, J Mater Chem B (2015)

Pereira, Granja +, In Preparation (2015)



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