

Influence of porous architecture of scaffolds obtained from different routes on the cell colonization.

A.Leriche, J.C. Hornez, F.Bouchart, E.Meurice

Laboratoire Matériaux Céramiques et Procédés Associés

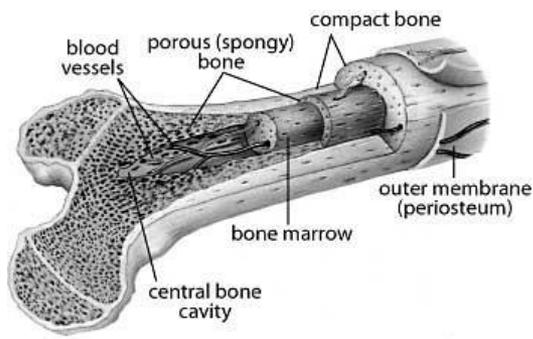
Collaboration with

D.Hautcoeur, V.Lardot, F.Cambier, *Belgian Ceramic Research Centre, Mons*

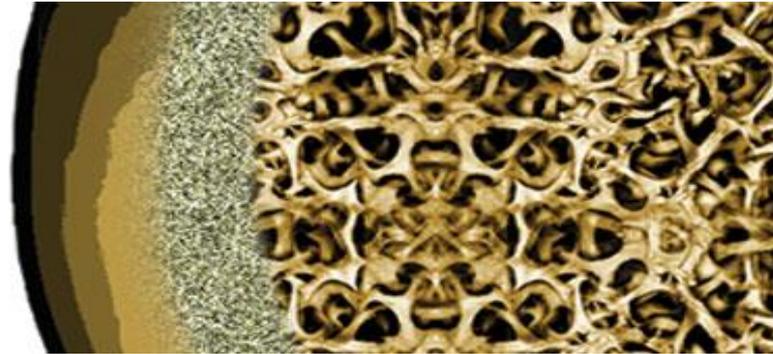
M-H Fernandes, *Faculdade de Medicina Dentara da Universidade do Porto*

F.Monteiro, *Instituto de Engenharia Biomédica , Porto*

Introduction



Carlyn Iverson



Os compact

Os spongieux

Compact
bone

Spongy bone

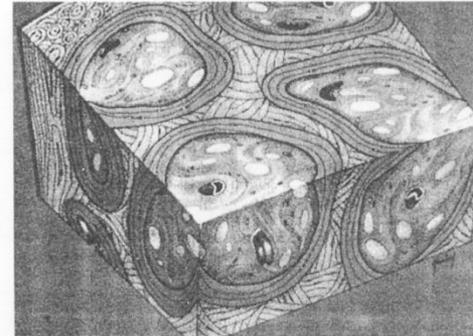
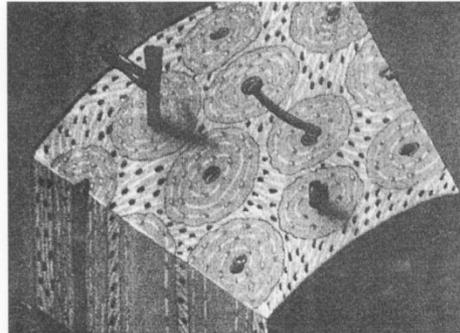


Porosity

Φ : 190-230 μm

V : 65%

$\sigma_c = 80-200 \text{ MPa}$

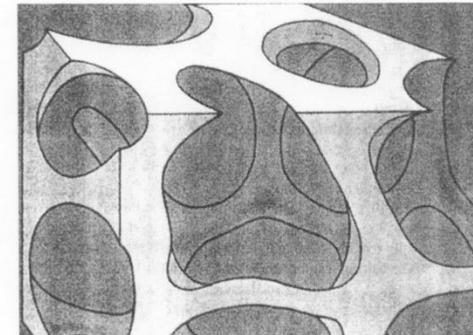
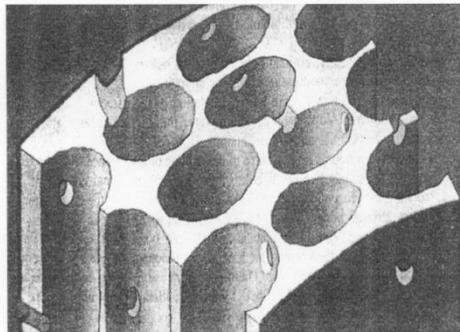


Porosity

Φ : 500-600 μm

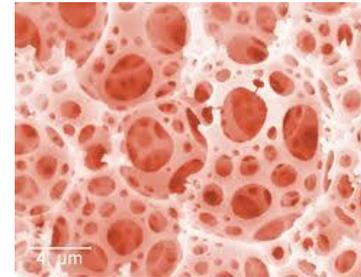
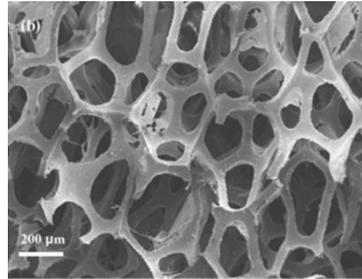
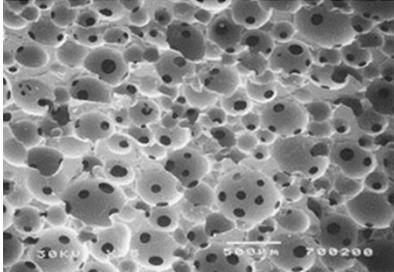
V : 80%

$\sigma_c = \text{a few tenths MPa}$

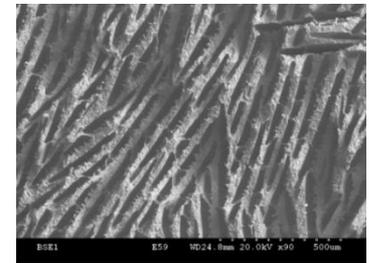
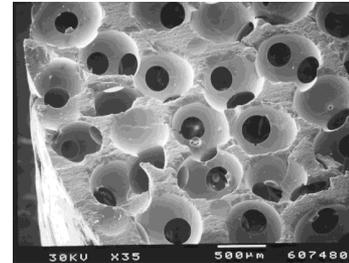
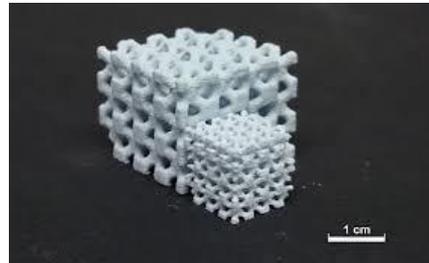
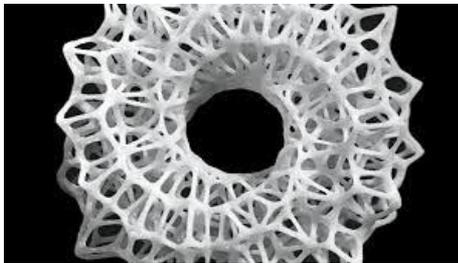
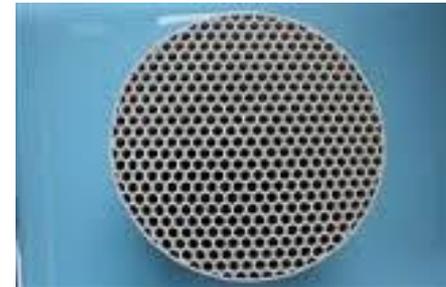


Introduction

- **Porous ceramics :** wide range of structures
- **Foams with cell walls randomly oriented in space**



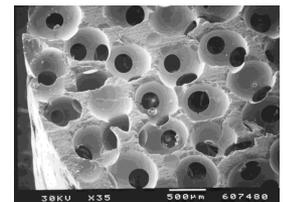
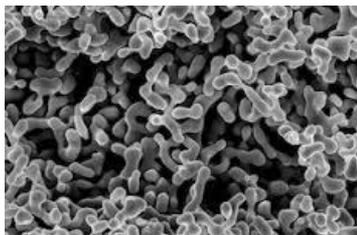
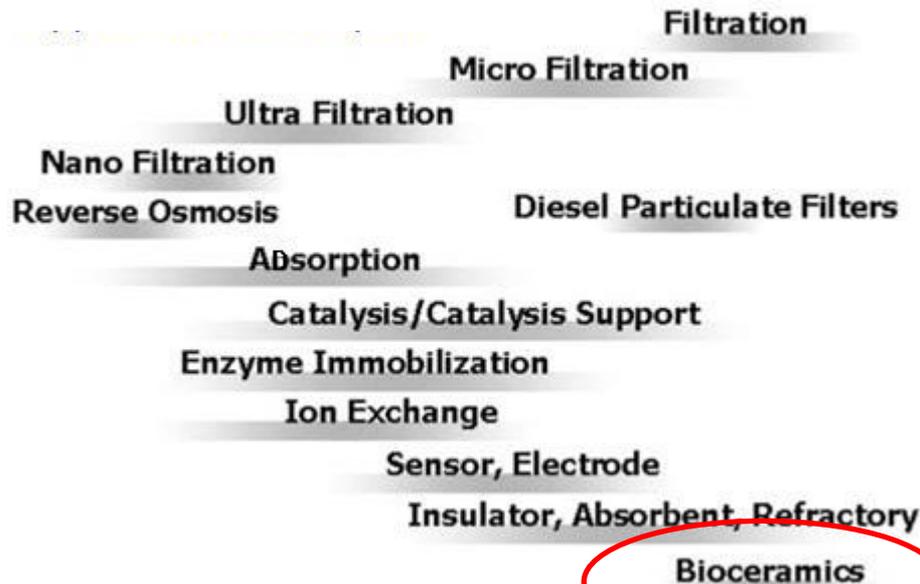
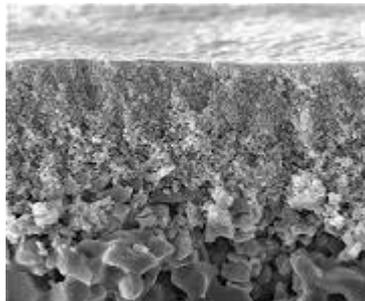
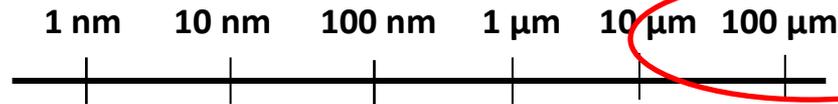
- **Honeycombs with polyhedral cells 3D arranged**
- **Connected hollow spheres or rods or fibres...**



P. Colombo, Phil.Trans.R.Soc.A 2006

Introduction

- Large applications fields in advanced engineering such as filtering liquids and particles in gas streams, porous burners, lightweight load-bearing structures,...and biomedical devices such as bone substitutes.



Ohji and M.Fukushima. *International Material Reviews* 57, 2, 2012

Introduction

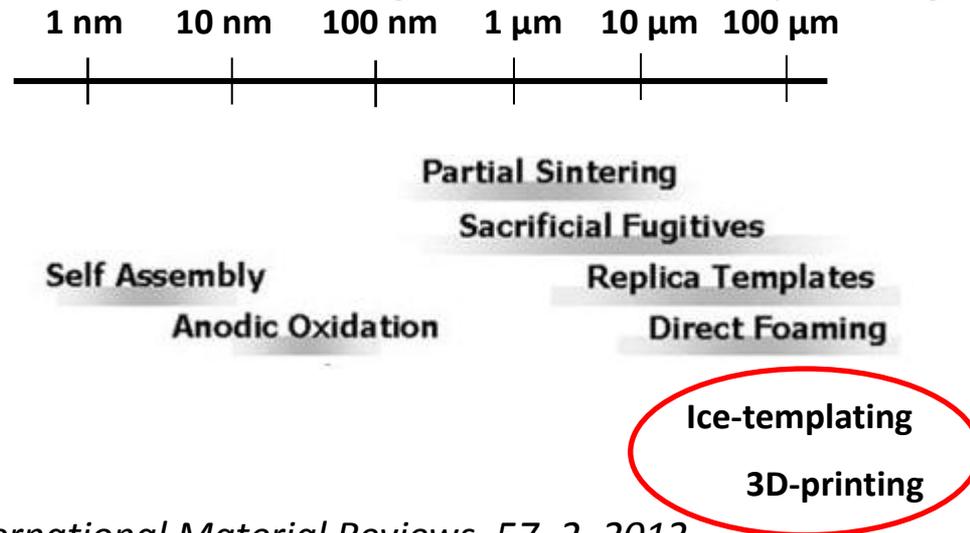
➤ Various processing routes :

Conventional methods :

partial sintering, sacrificial fugitives, replica templates, direct foaming ,
extrusion, aerogels...

Innovative methods:

ice-templating, additive manufacturing methods as 3D-printing,...



Ohji and M.Fukushima. International Material Reviews 57, 2, 2012

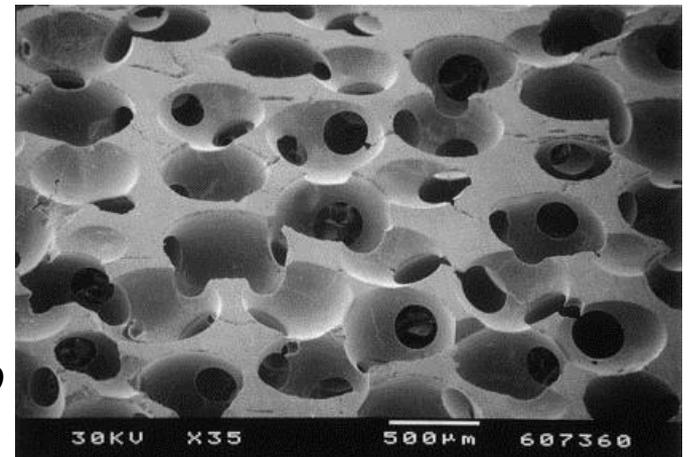
Introduction

Three methods to manufacture macroporous and microporous ceramic scaffolds:

- The first one by **ceramic slurry infiltration of organic bead skeleton**, permits to have an isotropic structure with close control of the pore size and the interconnection size but relatively low mechanical resistance.

**Patent FR2823305, Biocetis SARL,
M. DESCAMPS, P HARDOUIN, J LU, F MONCHAU**

M. Descamps et al., J. Eur. Ceram. Soc. 28 (2008) 149



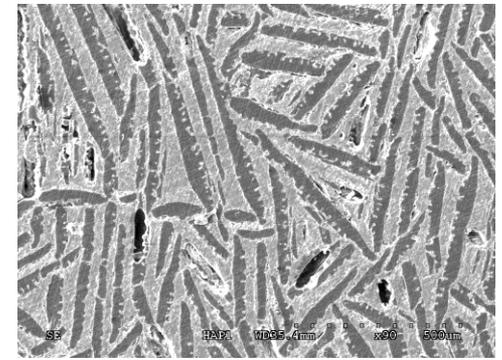
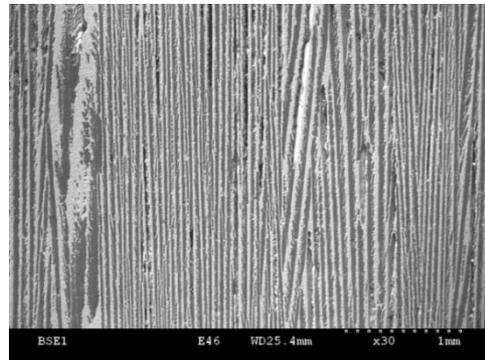
This technique type has been industrially applied by SOFAMOR – DANЕК, BIOСETIS and BIOLU since a few years.

Introduction

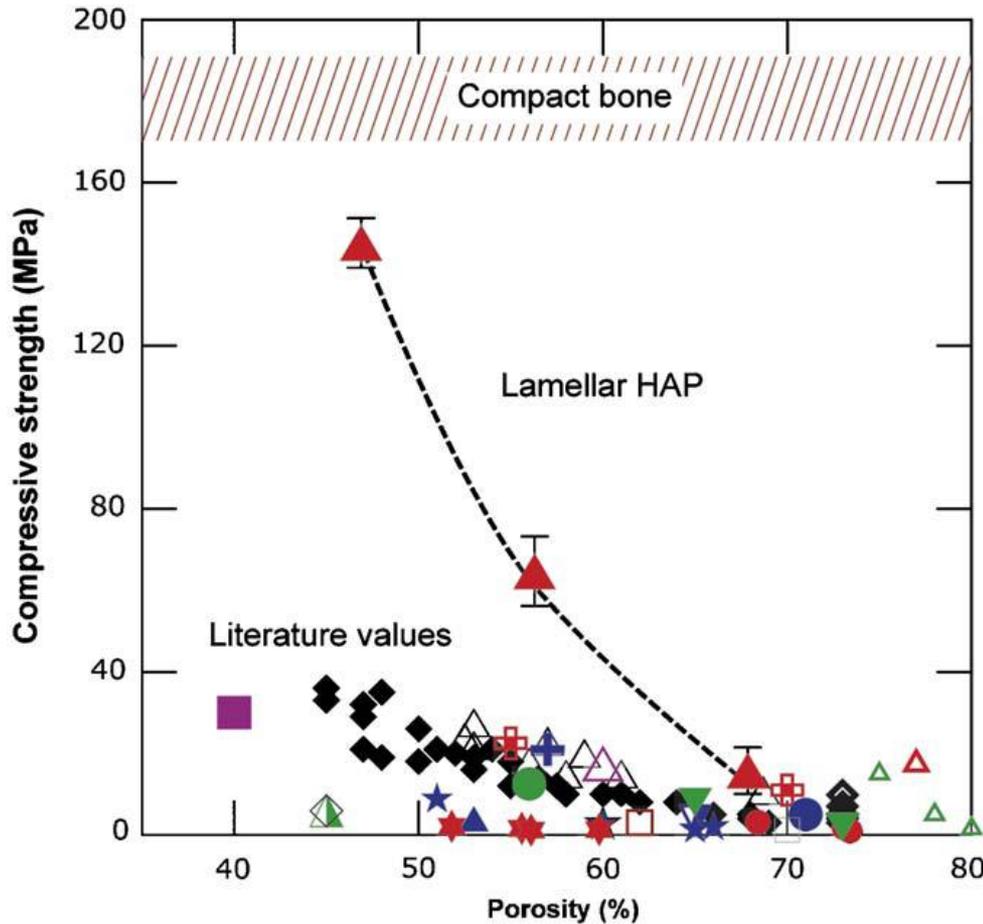
Three methods to manufacture macroporous and microporous ceramic scaffolds:

- The first one by **ceramic slurry infiltration of organic bead skeleton**, permits to have an isotropic structure with close control of the pore size and the interconnection size but relatively low mechanical resistance.

- The second one by **ceramic slurry casting using ice templating**, permits to develop anisotropic structure which allows higher compressive strength but compromise has to be found between σ_c and pore size (S. Deville).



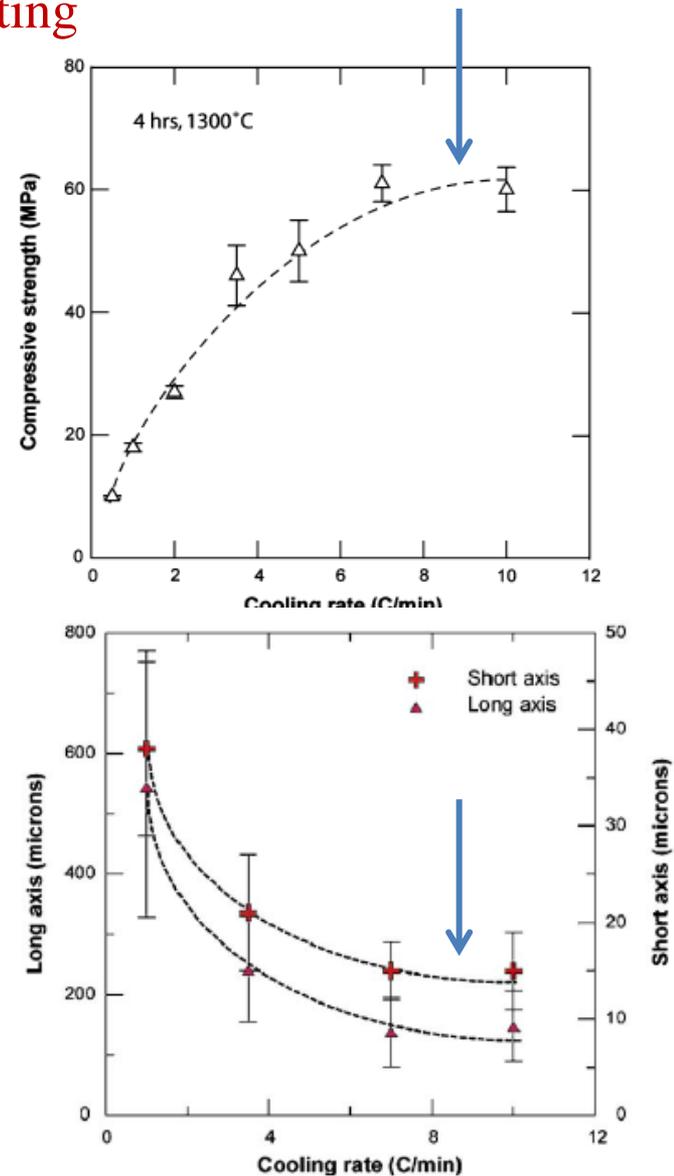
Ceramic casting by ice templating



S. Deville et al., *Biomaterials* 27 (2006) 5480–5489

Up today substitutes present lower σ_c values than compact bone one's, the freeze casting excepted.

But high σ_c values correspond to smaller pore sizes than usually used for bone substitutes.



Introduction

Three methods to manufacture macroporous and microporous ceramic scaffolds:

- The first one by **ceramic slurry infiltration of organic bead skeleton**, leads to an isotropic structure with close control of the pore size and the interconnection size but relatively low mechanical resistance.

- The second one by **ceramic slurry cast using ice templating**, permits to develop anisotropic structure which allows higher compressive strength but compromise has to be found between σ_c and pore size.

- The third one by **3D printing of ceramic slurry in UV sensitive resin** permits to develop anisotropic structure with regularly continuous channels with bigger size and square shape.

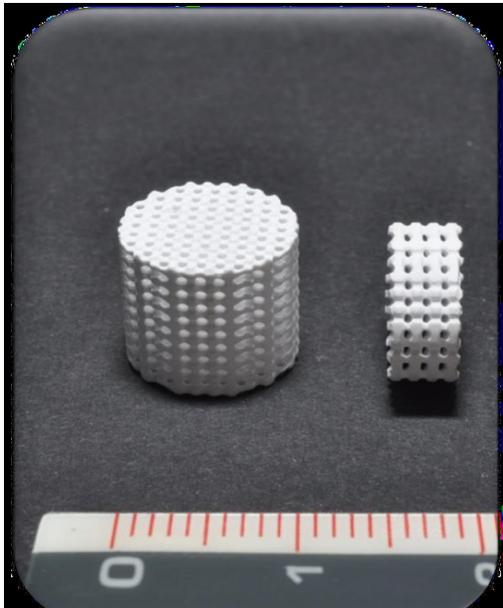
3D Printing of ceramic slurry in UV sensitive resin

Ceramic stereolithography is an additive manufacturing process which employs a ceramic slurry in a liquid ultraviolet curable photopolymer and an ultraviolet dynamic mask to build parts' layers one at a time.

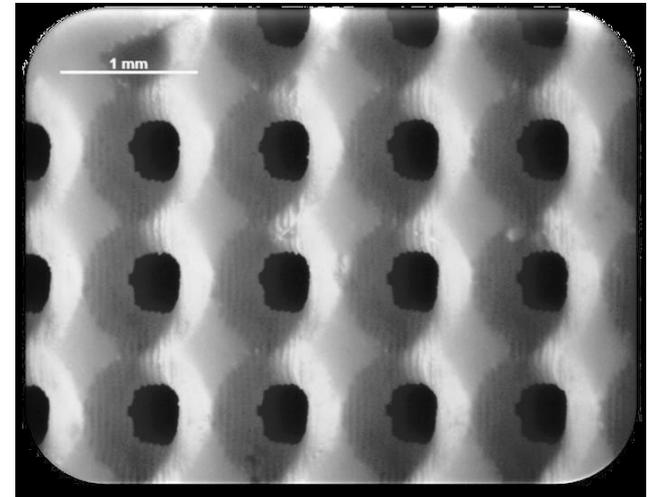
This layer by layer deposition technology is today commercialized by various companies such as 3DCERAM, SIRRIS (high-viscosity paste slurries) and Admatec Europe BV and Lithoz GmbH (low-viscosity slurries).

J.Deckers , J.Vleugels, J.P. Kruth

Additive Manufacturing of Ceramics: A Review J.Ceram.Sci.Tech 05 [04] 245-260 (2014)



Lithoz GmbH



By courtesy of Dr Johannes Homa

Introduction

The objectives of our study is to compare the mechanical properties and cell colonization ability of these different structures

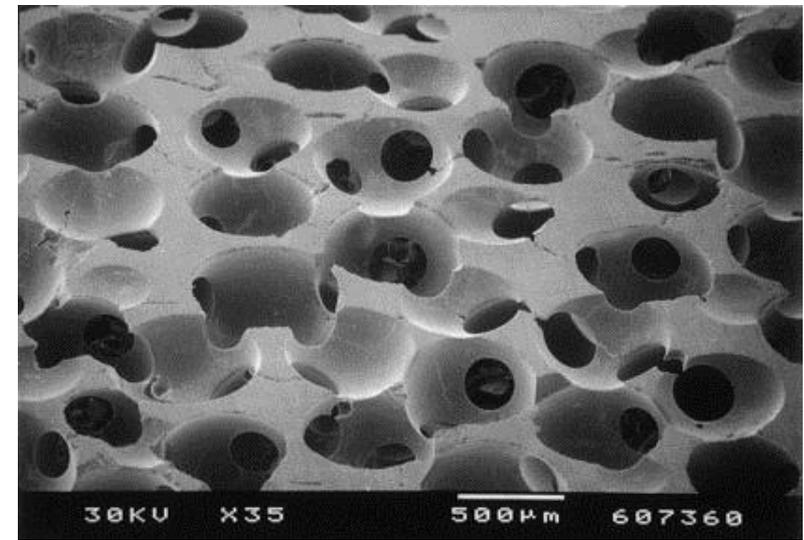
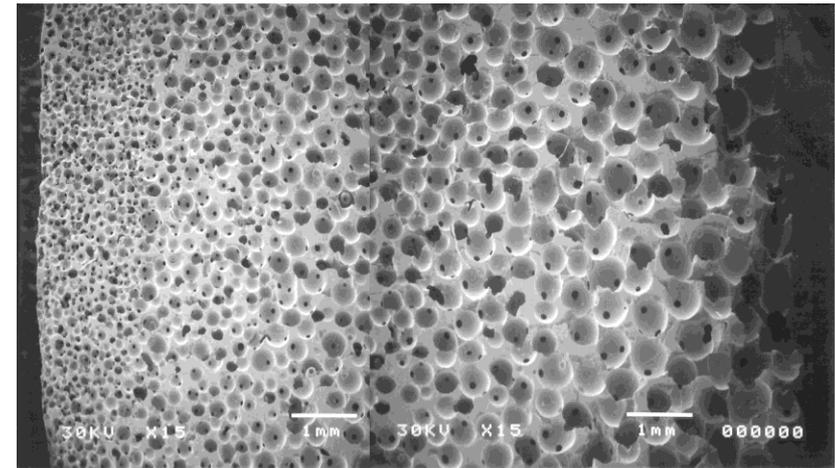
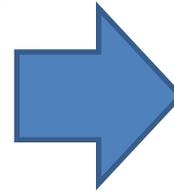
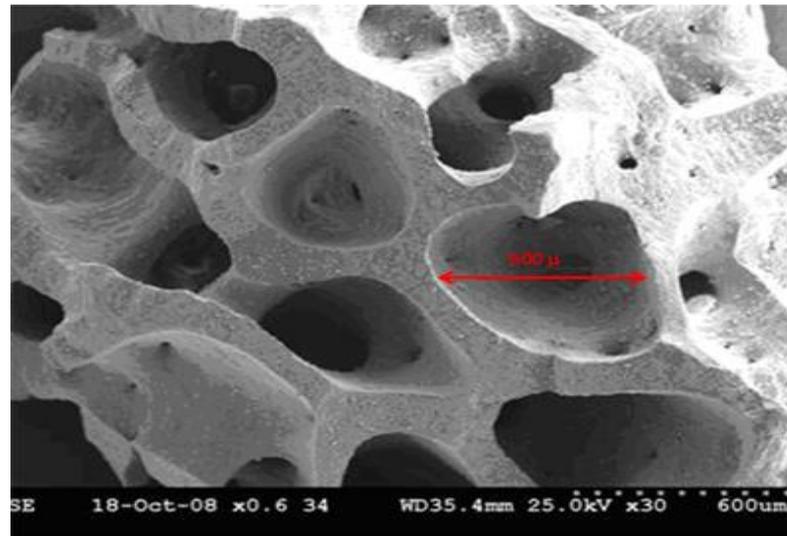
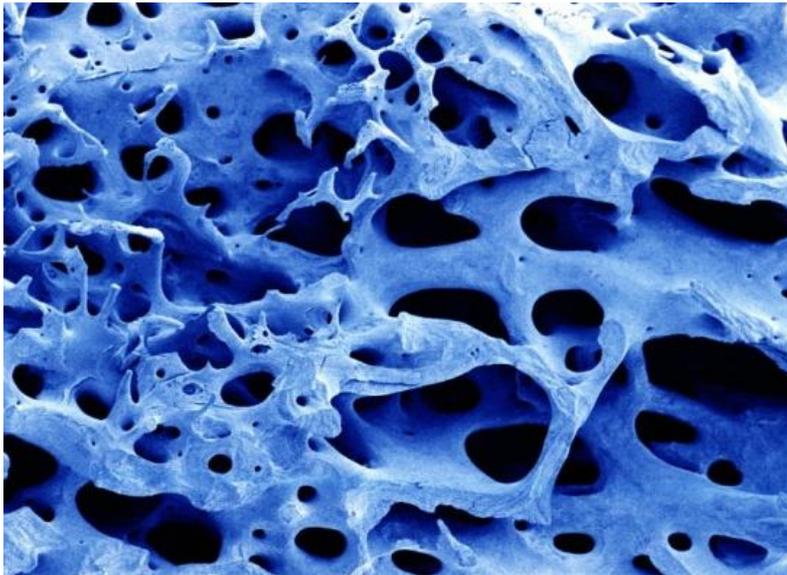
Part I: Presentation of the three shaping methods applied to calcium phosphate materials and the material structural properties

Part II: Comparison of cell colonization ability by static in vitro tests for the two methods: replica and freeze casting

Part III: Functionalization of as-prepared scaffolds by drug and phage impregnation through microporosity

First method: Ceramic slurry infiltration of organic skeleton

Human bone



Patent FR2823305

First method: Ceramic slurry infiltration of organic skeleton

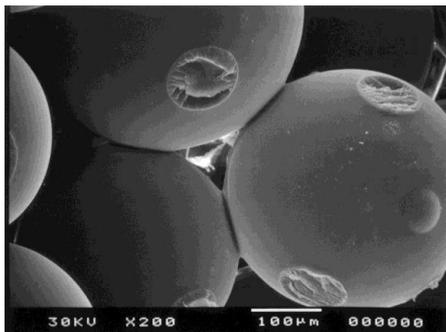
Organic skeleton preparation



Chemical forming
with acetone

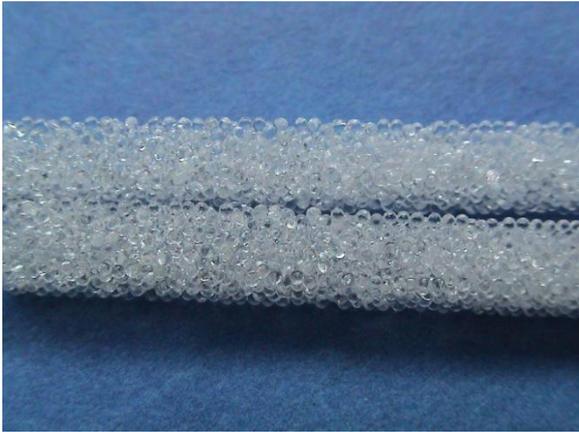


under pressure



- Bonding between PMMA beads (scaffold)
- Controlled diameter bonding (Interconnection) depends on time, temperature, pressure

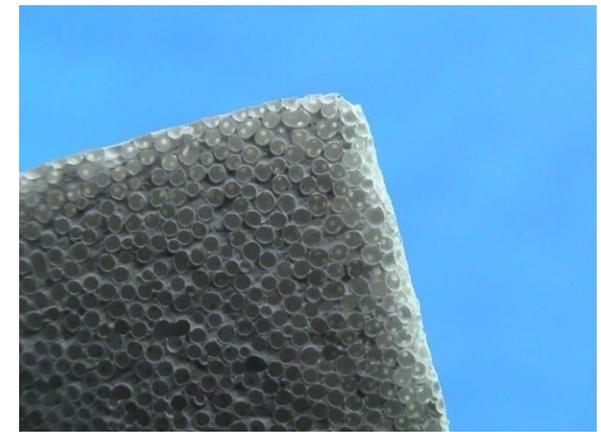
First method: Ceramic slurry infiltration of organic skeleton



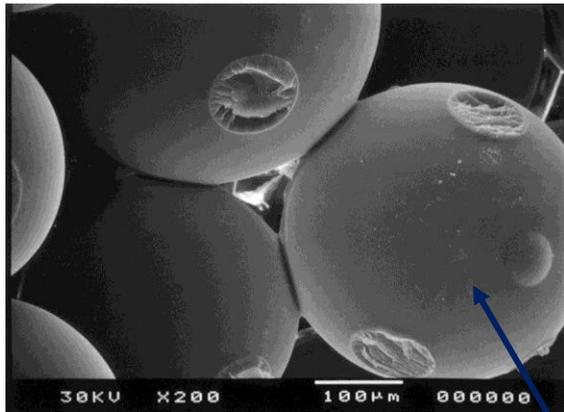
Shaping



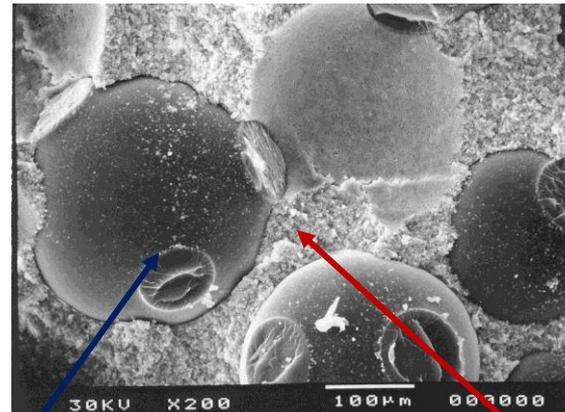
Impregnation



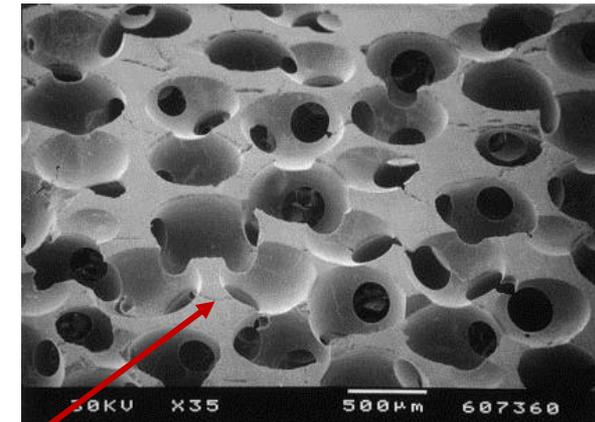
Debinding



PMMA beads



ceramic



First method: Ceramic slurry infiltration of organic skeleton

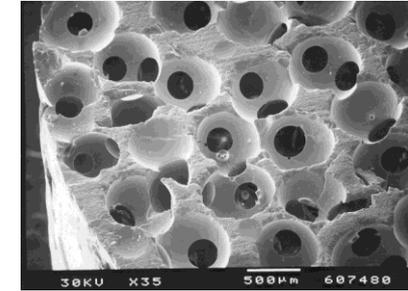
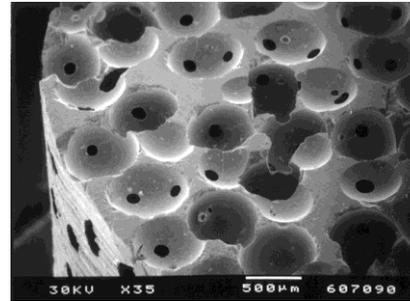
➤ Control of pore size depending on PMMA beads size

➤ Control of interconnection diameters: l_d

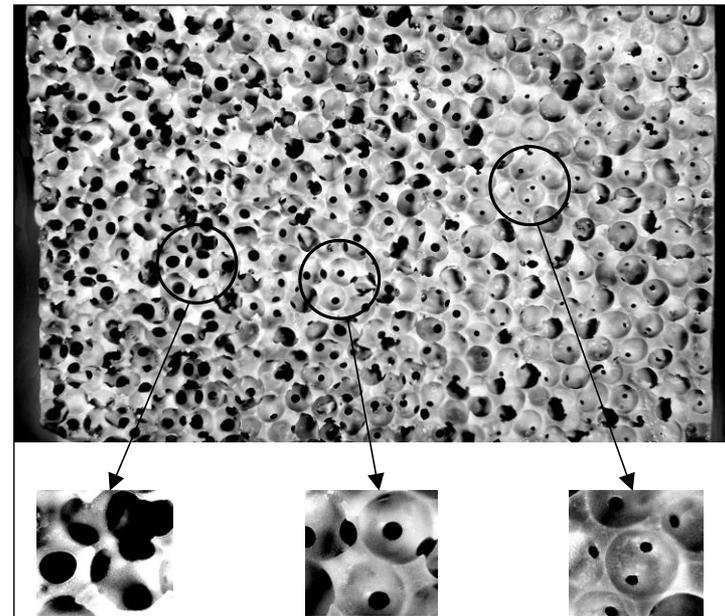
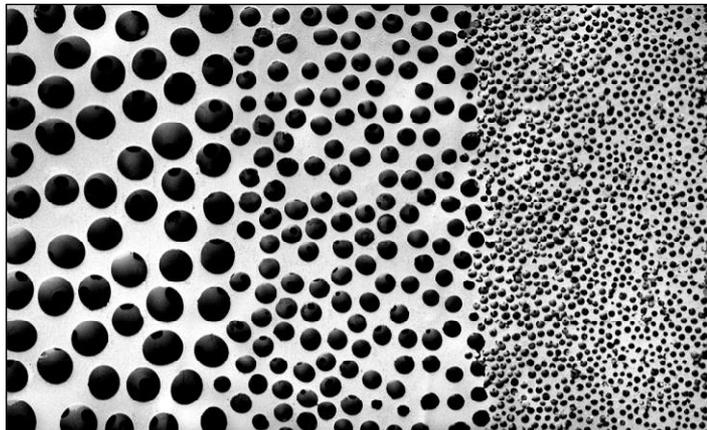
PMMA beads (500 - 600 μm)

l_d : 60 μm

l_d : 260 μm

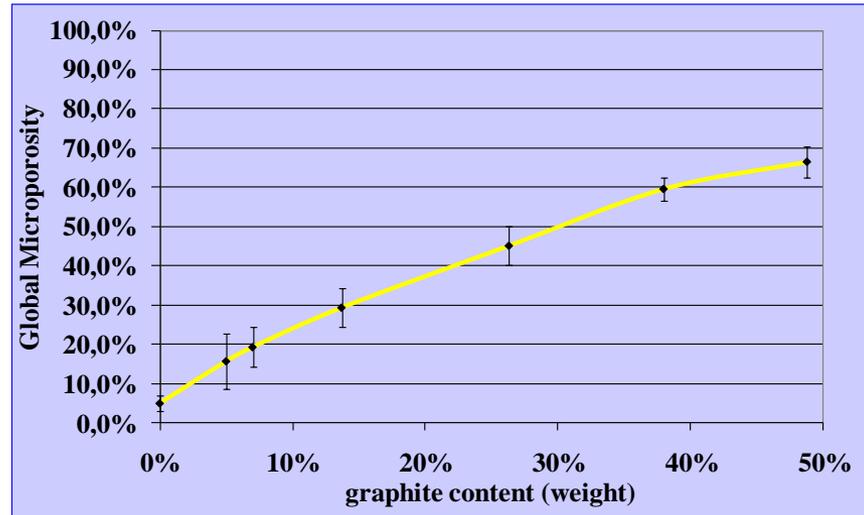
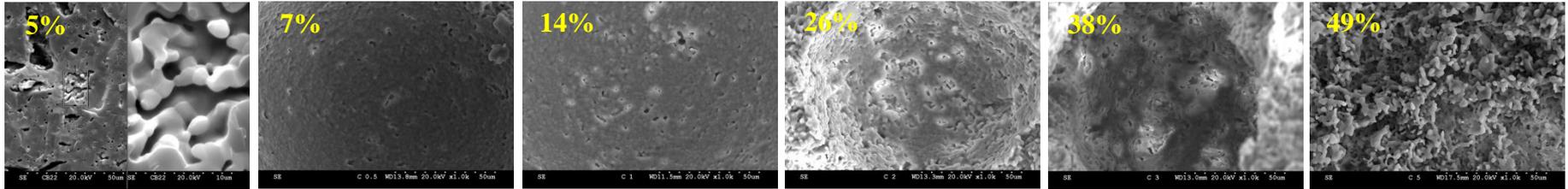


➤ Control of porosity gradient in pore size and interconnection size



First method: Ceramic slurry infiltration of organic skeleton

Possibility to add microporosity by mixing graphite as micropore forming agent.

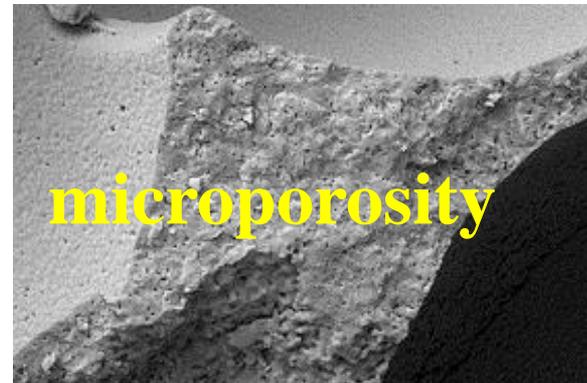
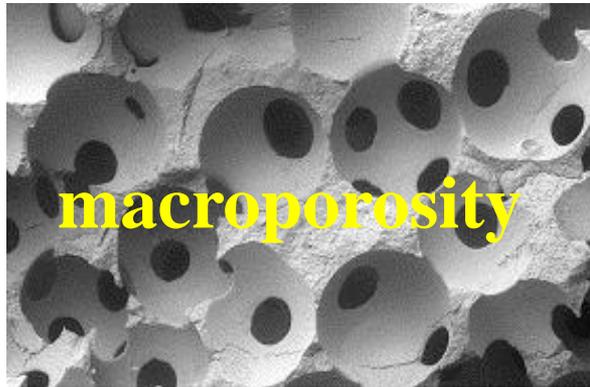


Controlled

macroporosity

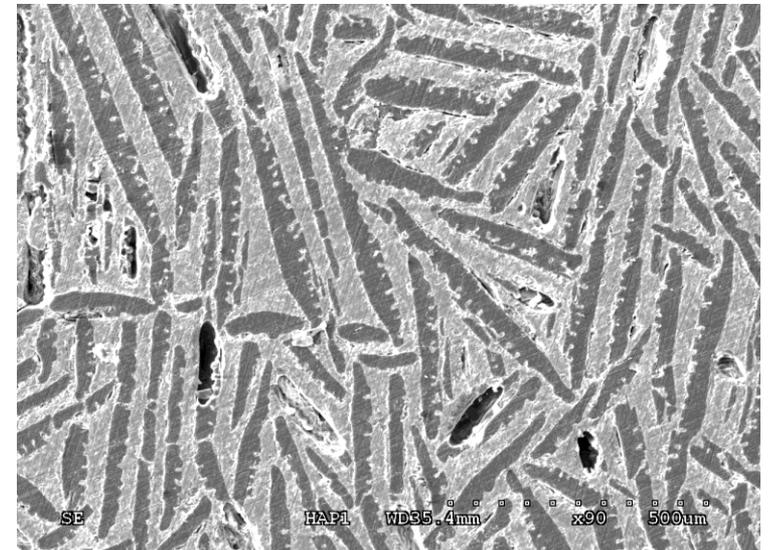
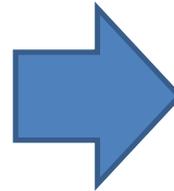
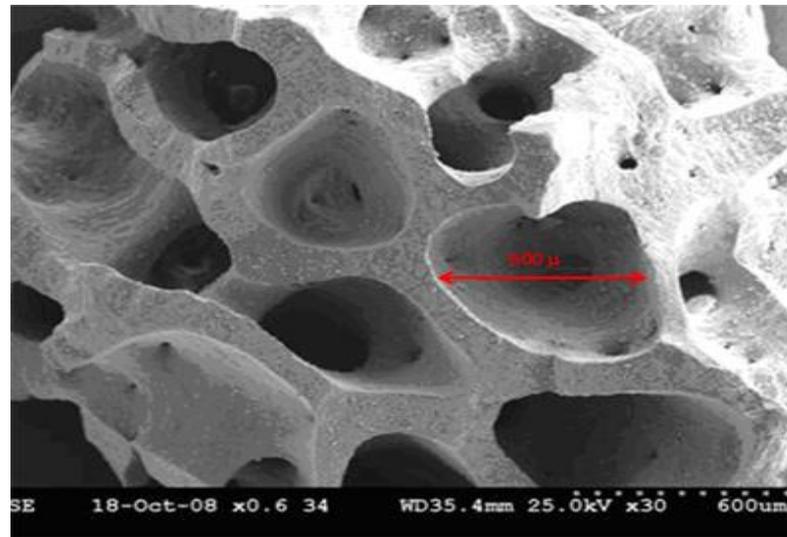
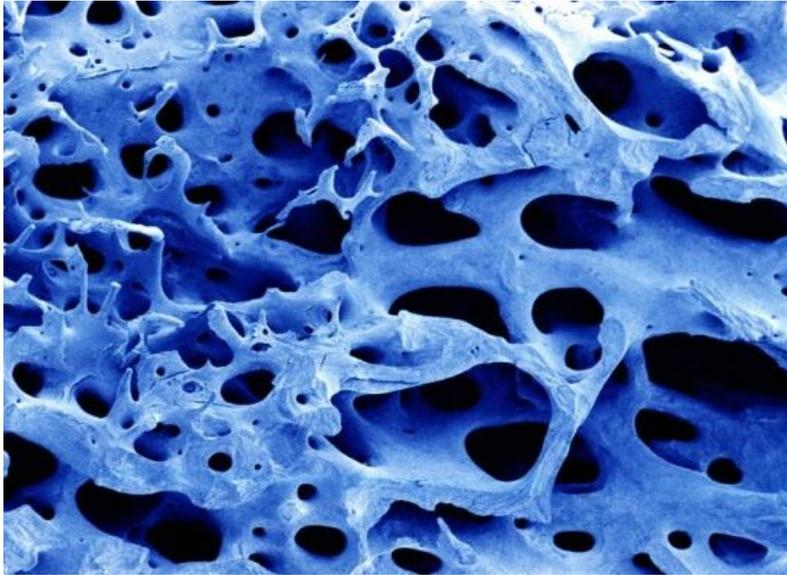
and

microporosity



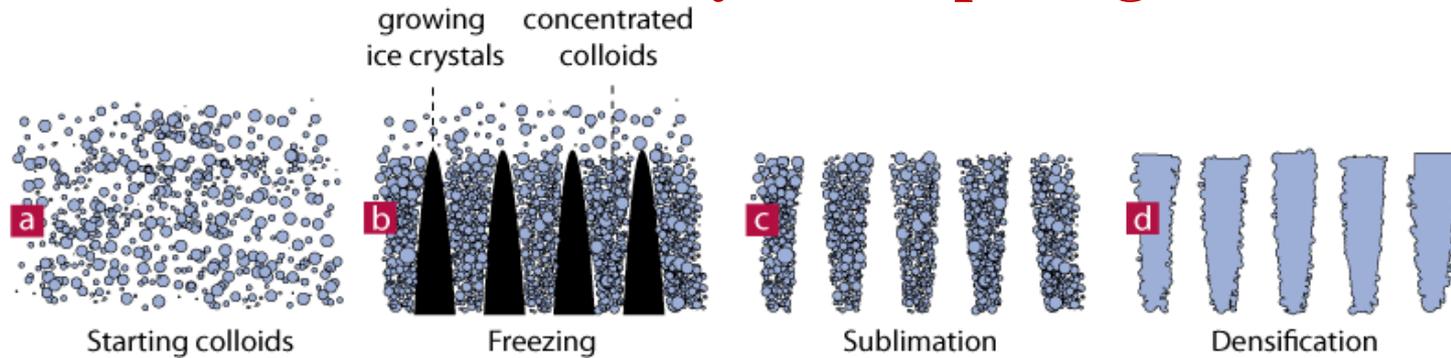
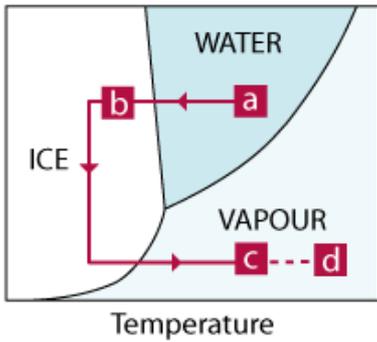
Second method: Ceramic slurry ice templating

Human bone



D. Hautcoeur Ph D UMons-BCRC Nov 2014

Second method: Ceramic slurry ice templating

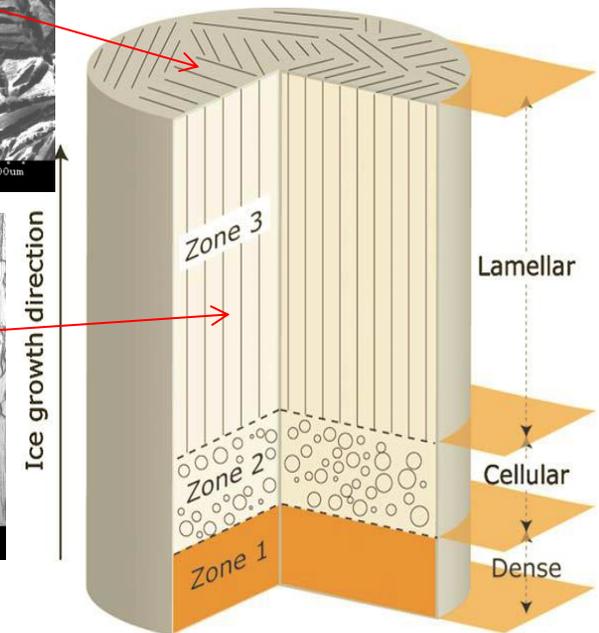
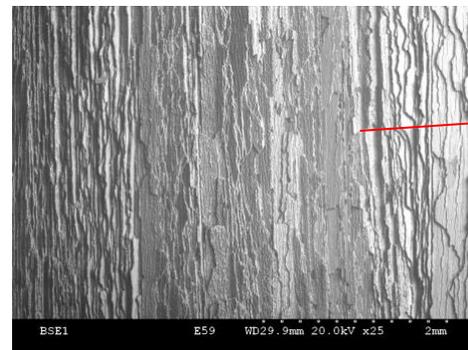
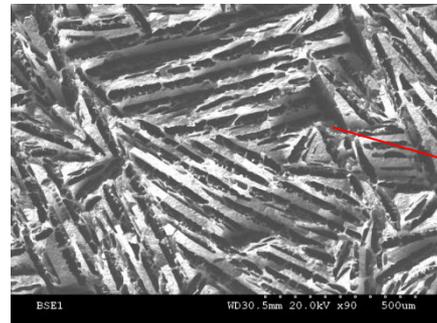
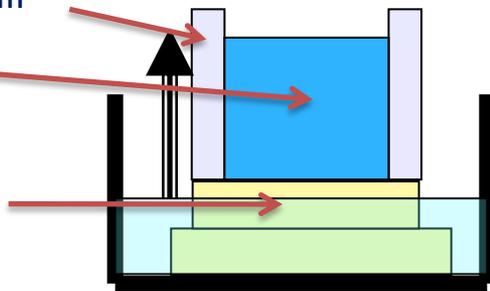


Mold
insulating wall

Slurry

Conductive
material

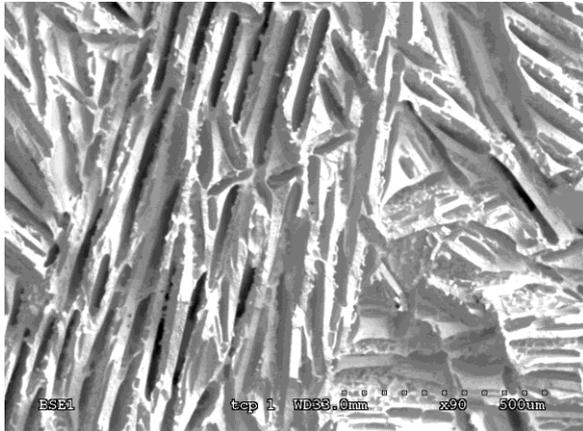
Cooling liquid



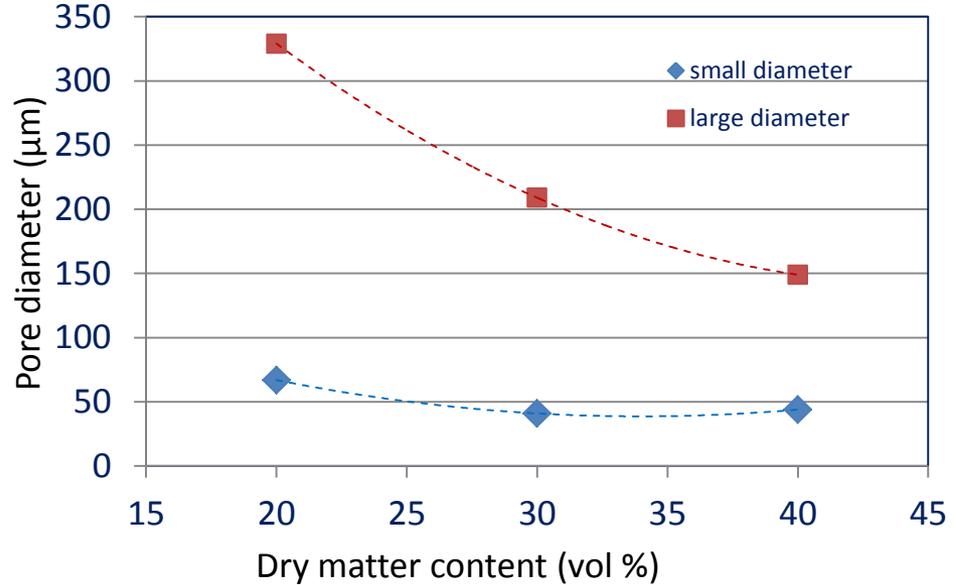
D. Hautcoeur Ph D UMons-BCRC Nov 2014

S. Deville et al., *Biomaterials* 27 (2006) 5480–5489

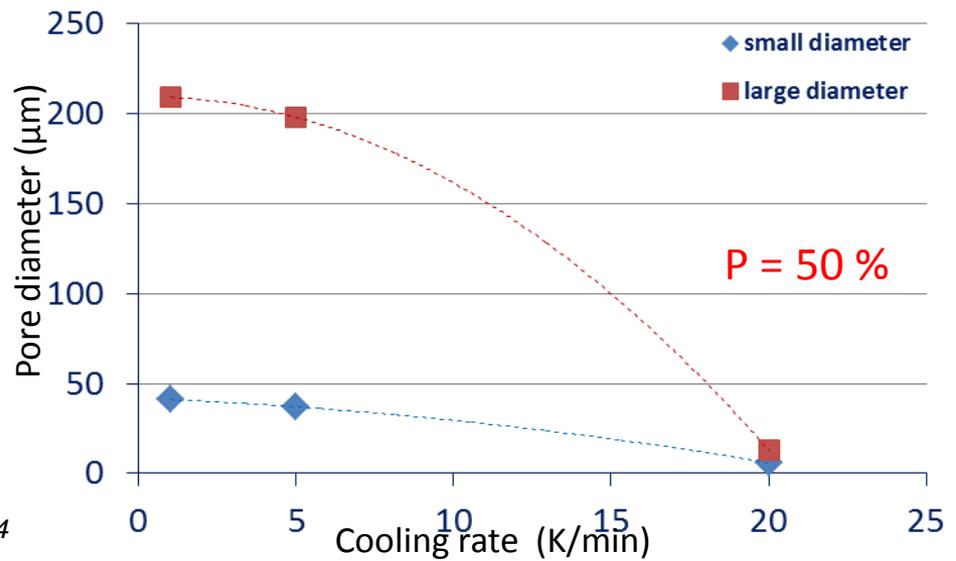
Second method: Ceramic slurry ice templating



β -TCP, 1 K/min, 3% binder



β -TCP, 30 vol % DM, 3% binder



Pore long axis size:

- between 150 and 340 μm versus dry matter content
- between 13 and 210 μm versus cooling rate .

Total porosity:

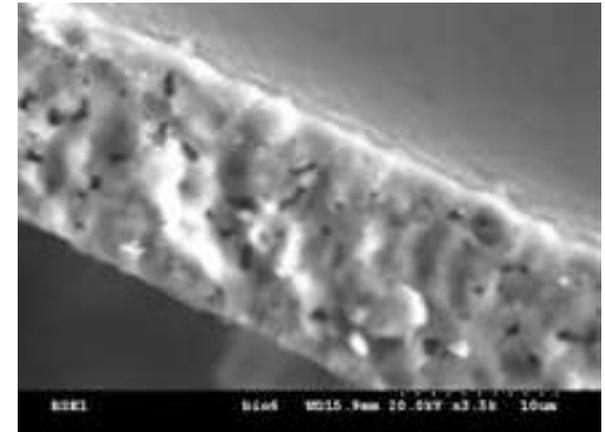
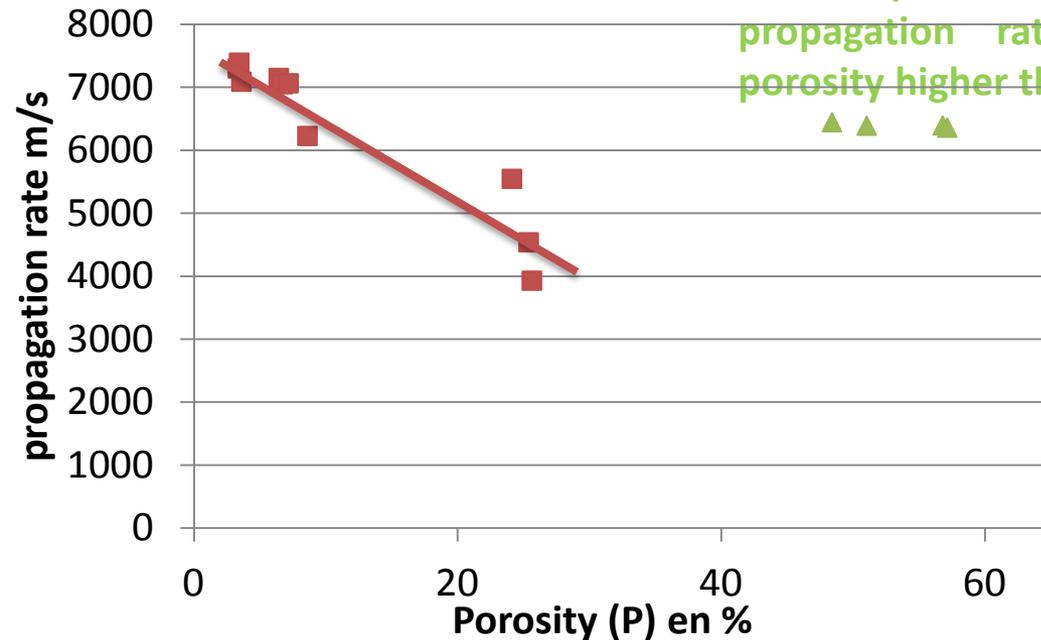
36 to 67 % versus dry matter %

Second method: Ceramic slurry ice templating

Relationship between porosity and propagation rate for **isotropic samples** (calibration curve) and **anisotropic samples**

isotropic samples

Anisotropic sample = high propagation rate despite a porosity higher than 40 %.

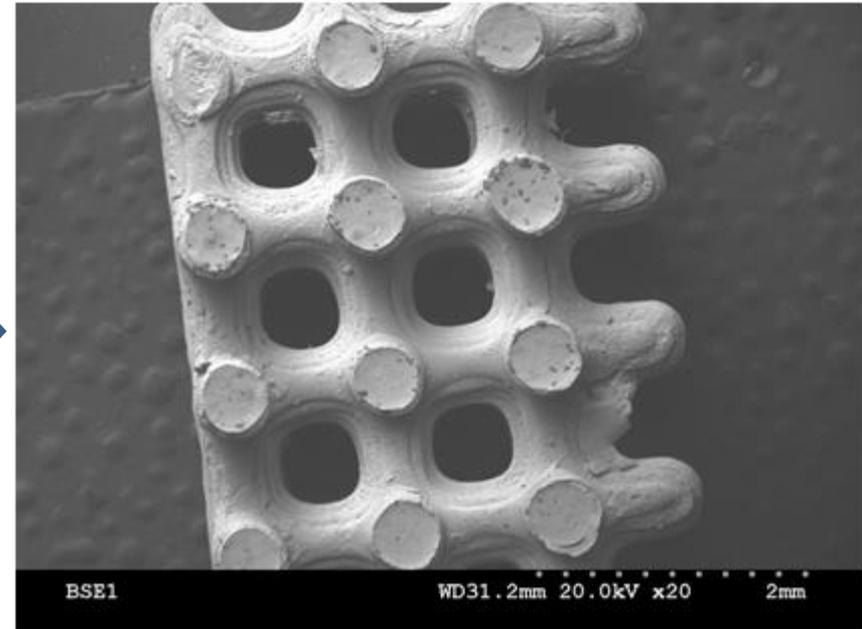
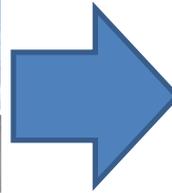
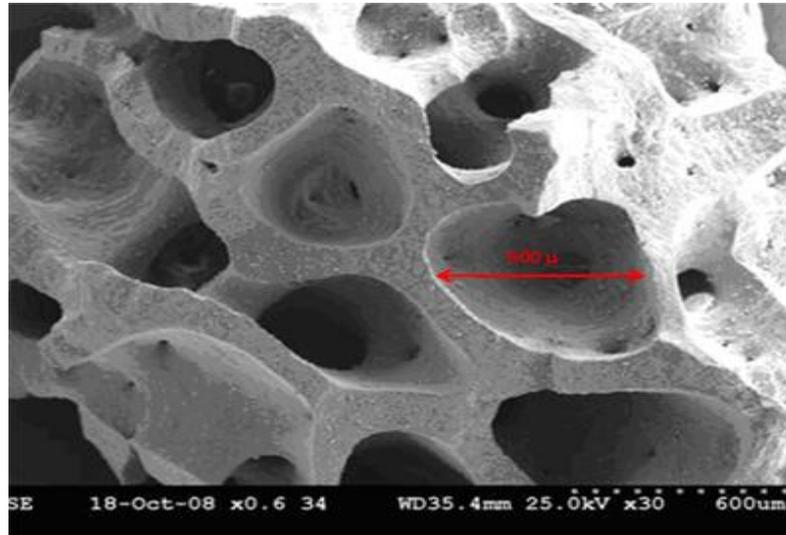
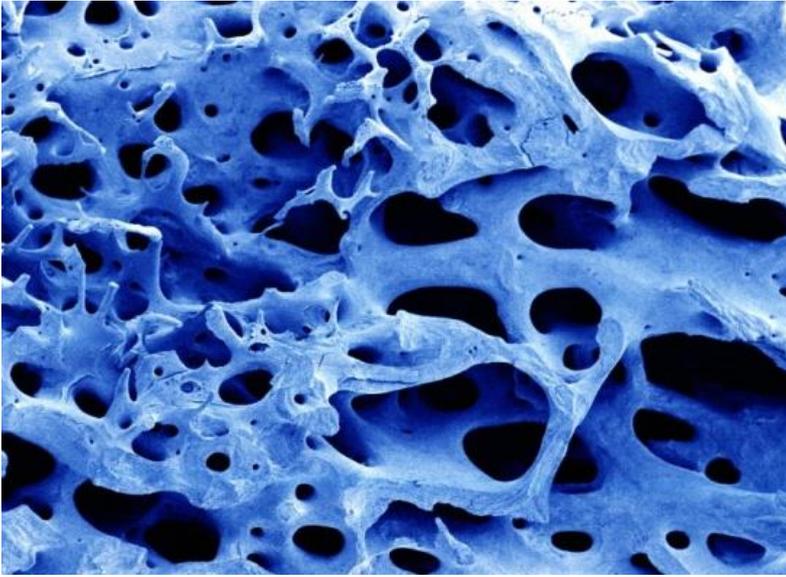


10 % microporosity

Slurry composition and freezing rate	Ceramic walls porosity % (average)
28% Vol.+ 3% PEG1000 and 1.3°C/min	11.5± 0.2
33% Vol. + 3% PEG1000 and 1.3°C/min	11.2 ± 0.2

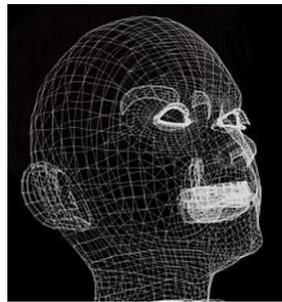
Third method: 3D printing of ceramic slurry

Human bone

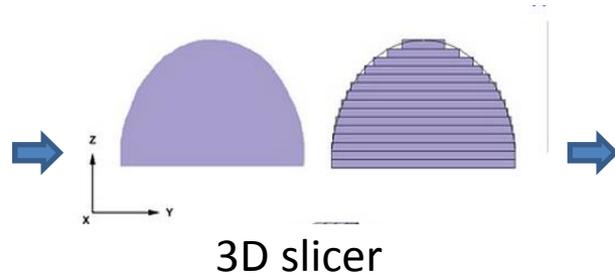


JC Hornez LMCPA January 2015

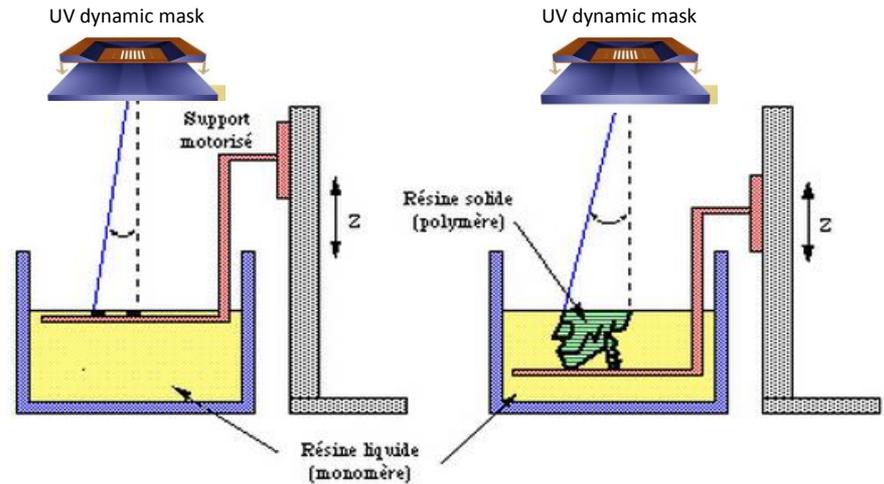
Third method: 3D printing of ceramic slurry



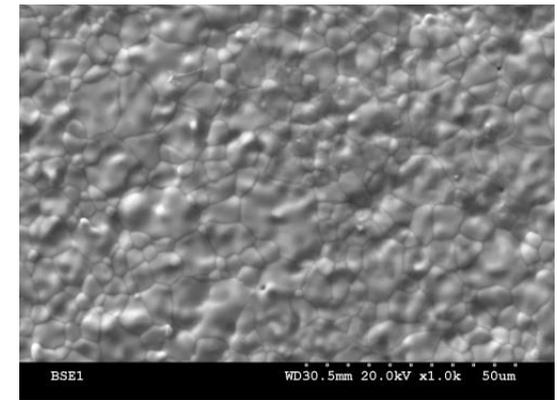
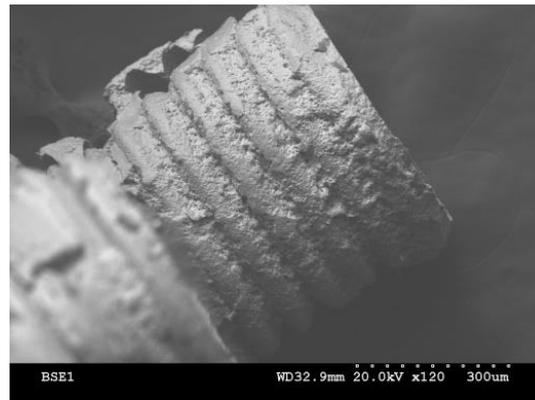
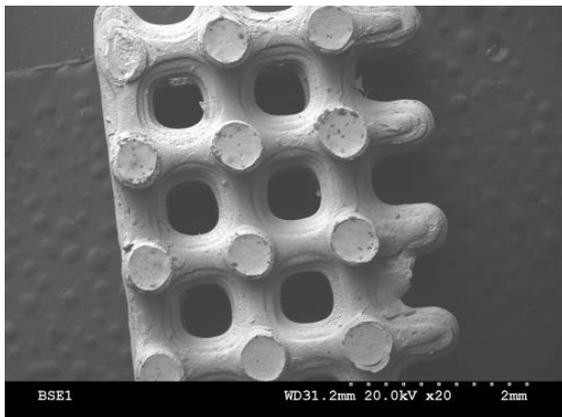
CAO



3D slicer

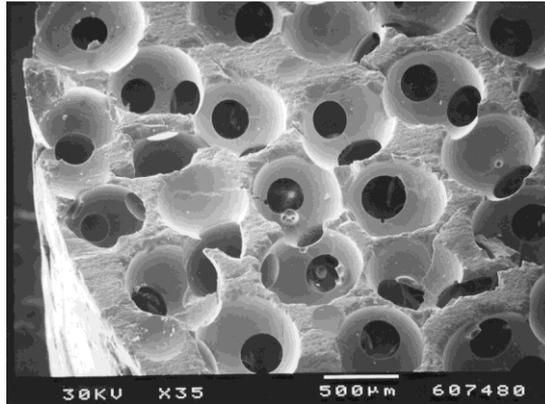


- The thickness of a single layer, typically $20\ \mu\text{m}$ to $100\ \mu\text{m}$
- Close control of porosity shape, size and orientation



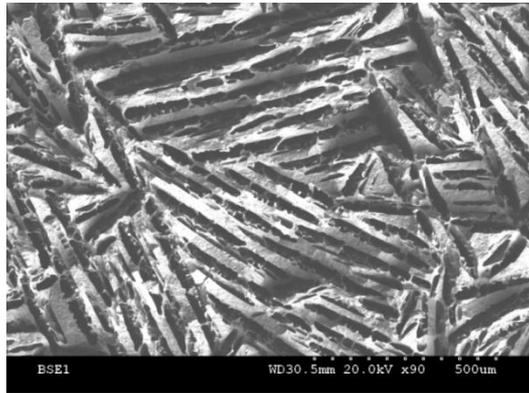
Comparison of the three different macroporosities

Isotropic porosity



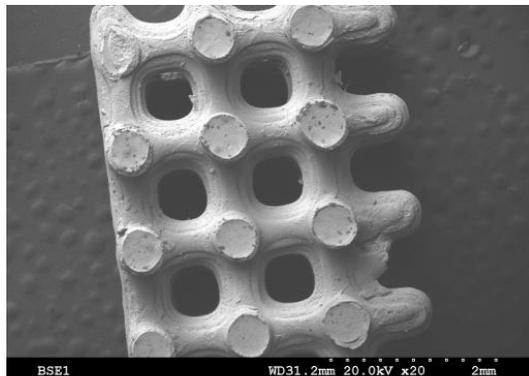
- 65% porosity (limits 65-75%)
- 100 µm interconnection
- 500-600 µm spherical pore diameter
- HA: 15 MPa, TCP: >15 MPa
- Possibility for pore size and content gradient

Anisotropic porosity



- 55% porosity (limits 40-75%)
- Ellipsoidal porosity
- 13-400 µm pore large diameter
- 6 -70 µm pore small diameter
- 10 - 50 µm width of wall
- HA: 51% porosity, 180/35 µm pore Ø
 σ_c : 21 MPa
- β -TCP: 40% porosity, 280/35 µm pore Ø
 σ_c : 35 MPa

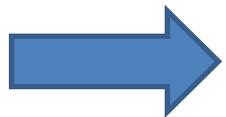
Controlled porosity



- 500-700 µm tubular porosity
- Up to 80 % porosity
- Any sizes and shapes are achievable

Part II Comparison of cell colonization ability by static in vitro tests for the two methods: replica and freeze casting

- What will be the impact of these two different macroporosities (size and morphology) on human cell invasion?
- Is the ice-templated samples porosity size enough large to permit the human cell invasion?



Colonization tests with MG63 osteoblasts

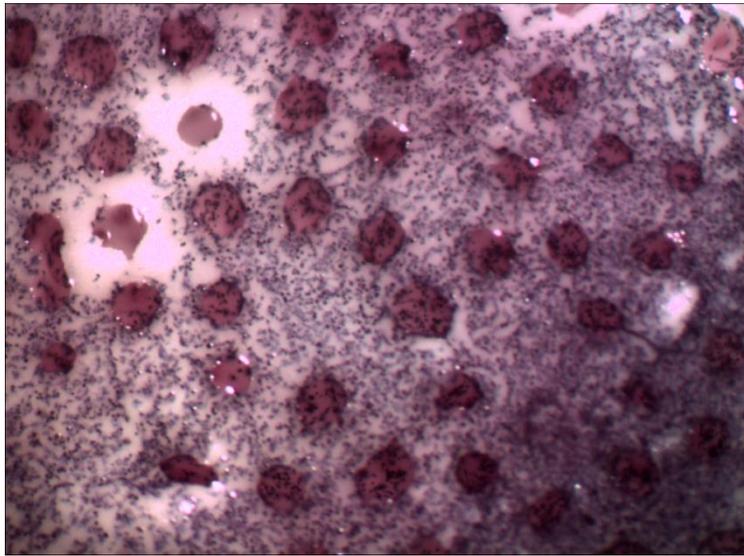
STSM E.Meurice at INEB, Porto July 2014

Colonization tests with MG63 osteoblasts

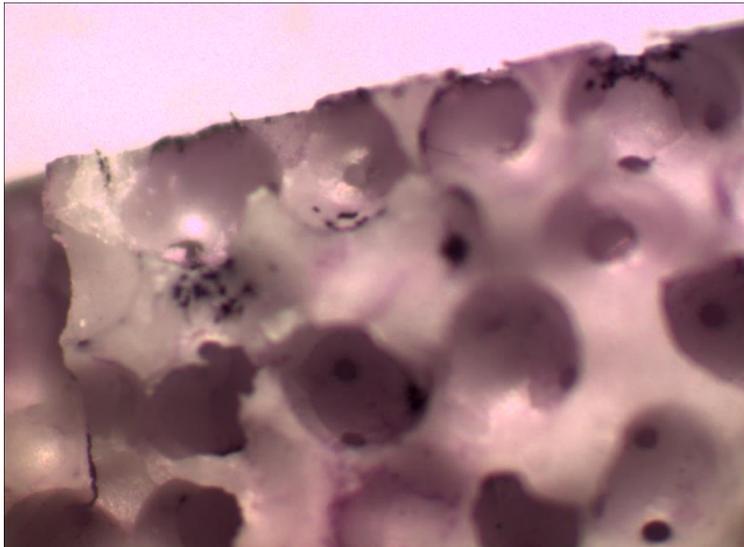
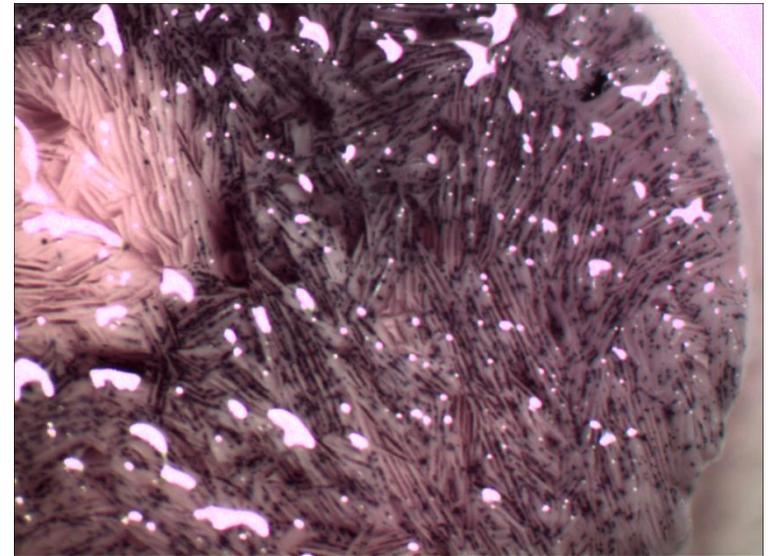
Organic bead skeleton infiltration

1 day

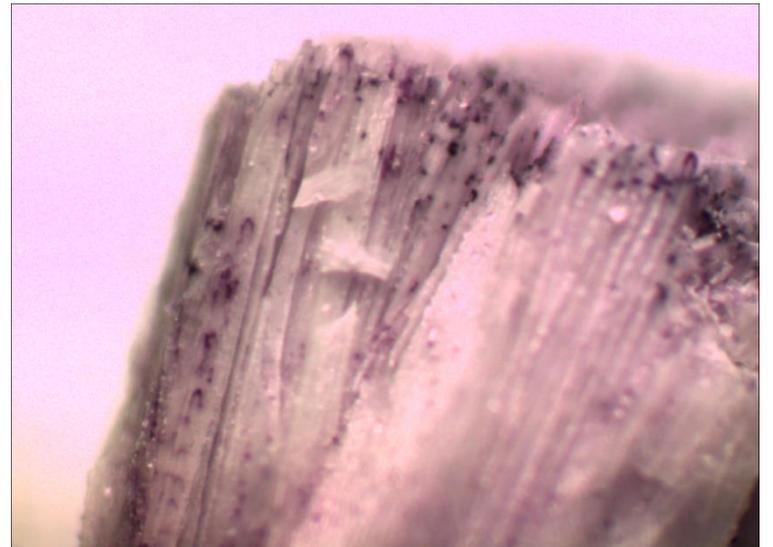
Ice - templating



Top



Slice

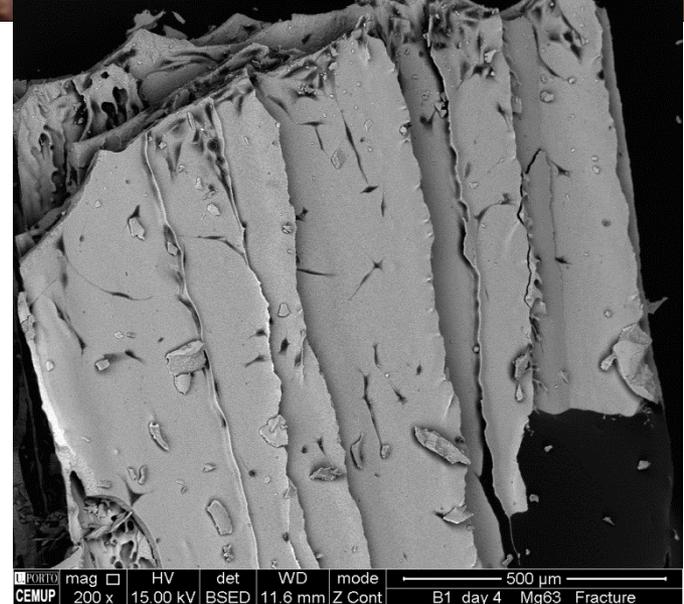
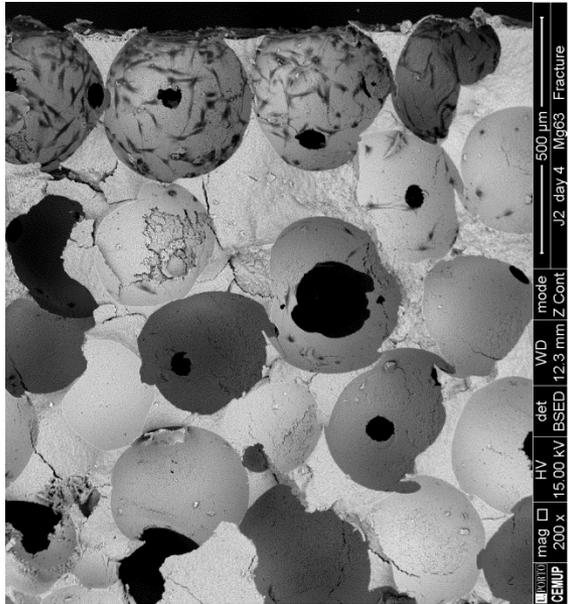
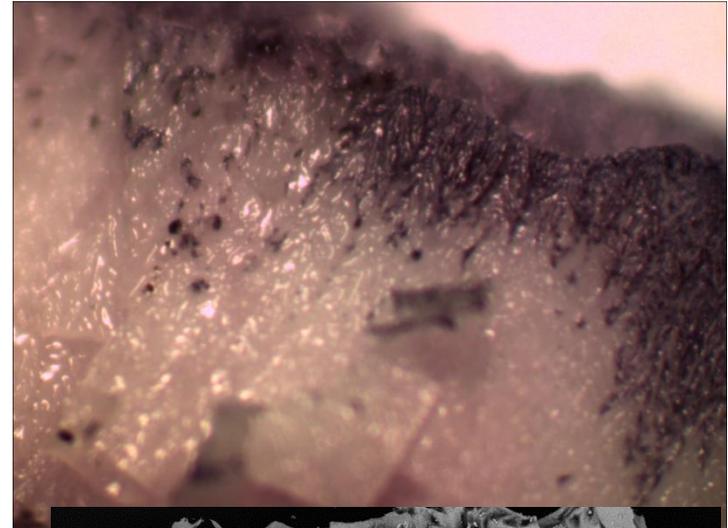
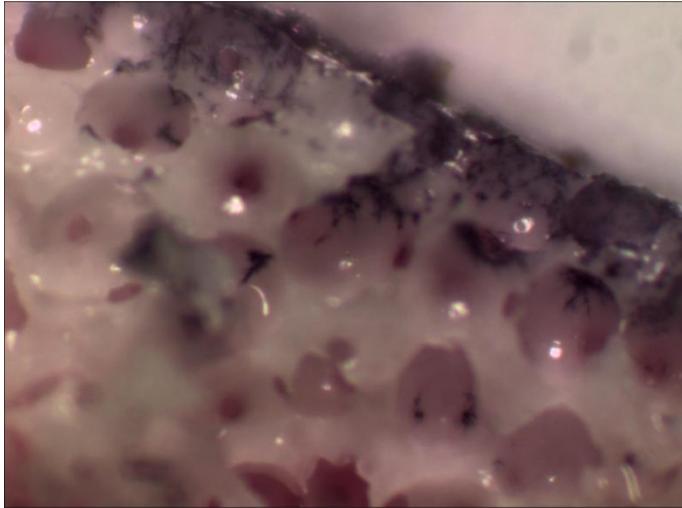


Colonization tests with MG63 osteoblasts

Organic bead skeleton infiltration

4 days

Ice - templating

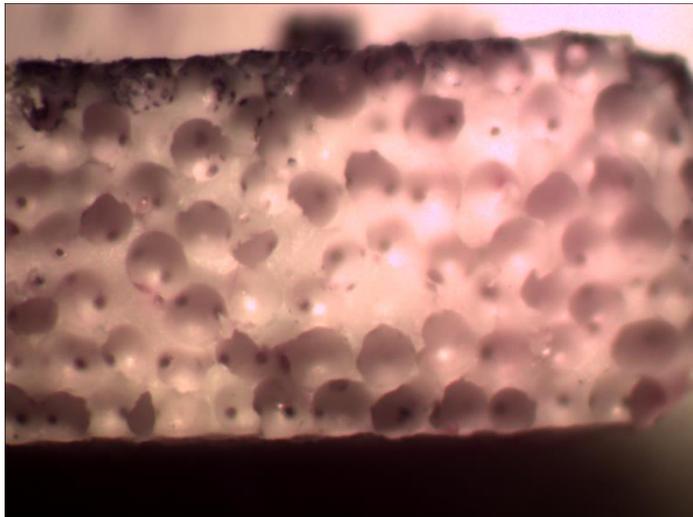
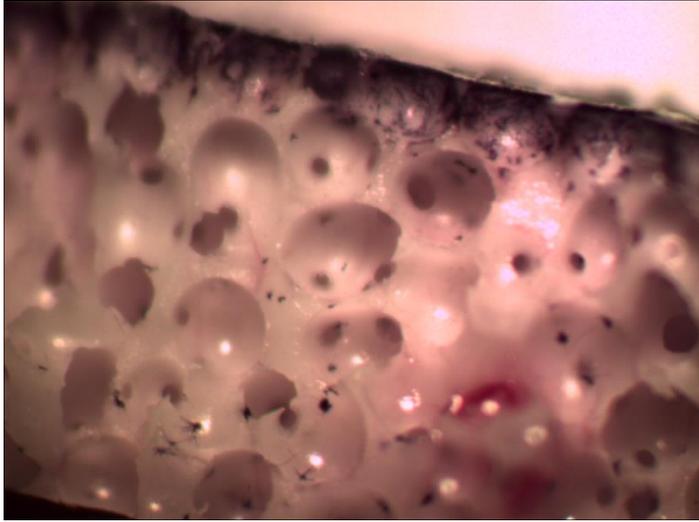


Colonization tests with MG63 osteoblasts

Organic bead skeleton infiltration

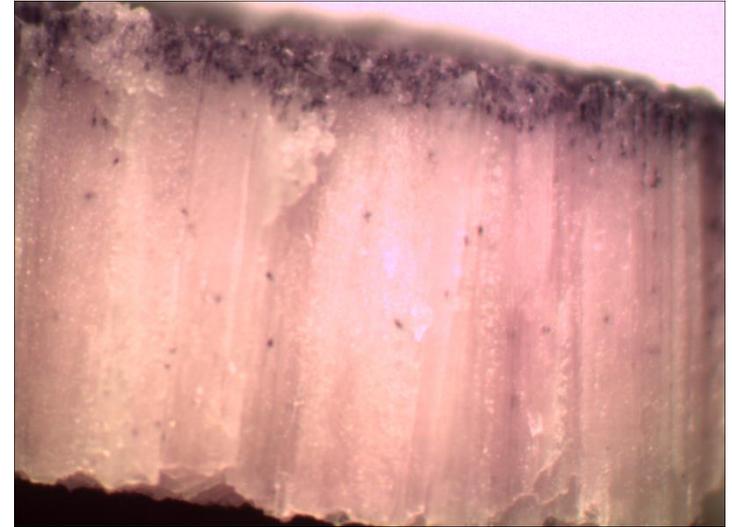
7 days

Beads 750 μm



Ice - templating

37/200 μm

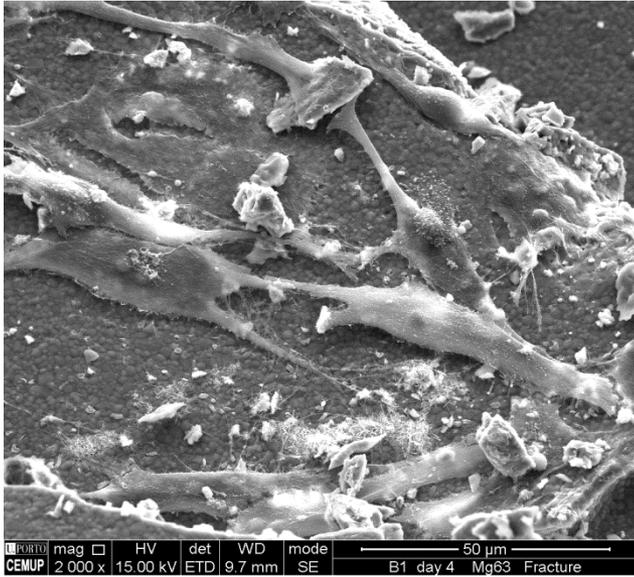


Beads 350 μm

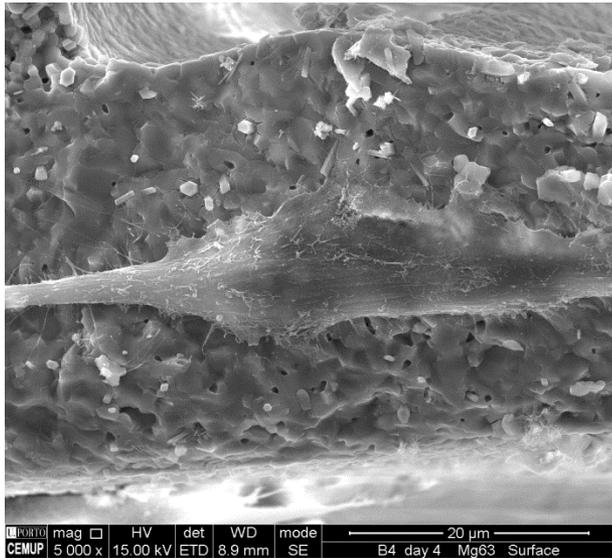
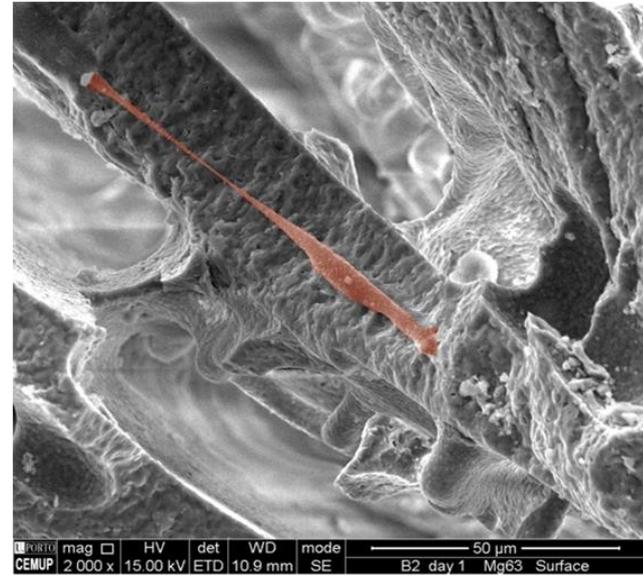
Colonization tests with MG63 osteoblasts

198 μm /37 μm

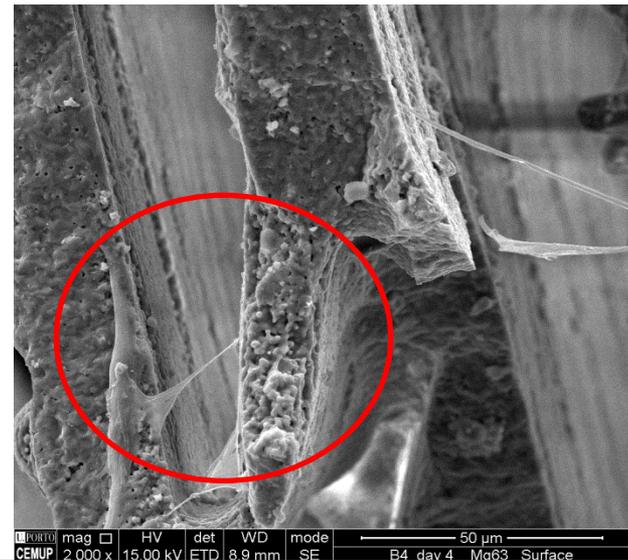
Ice - templating



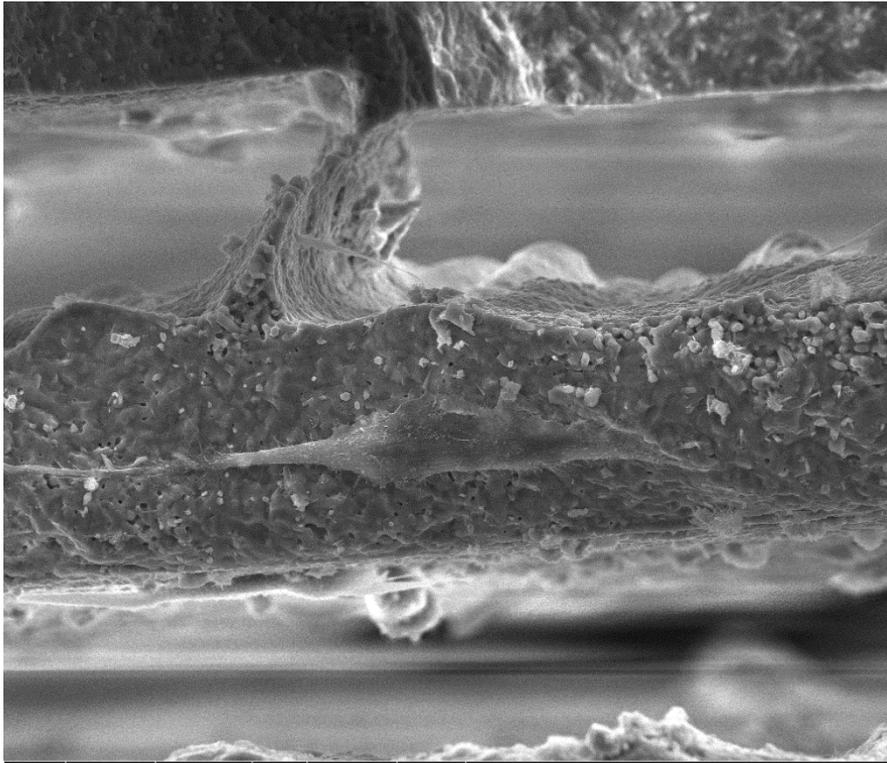
1 day



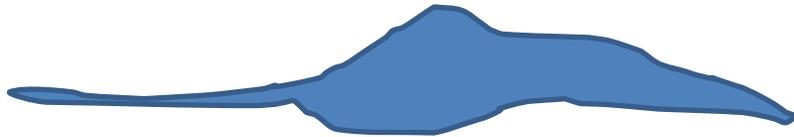
4 days



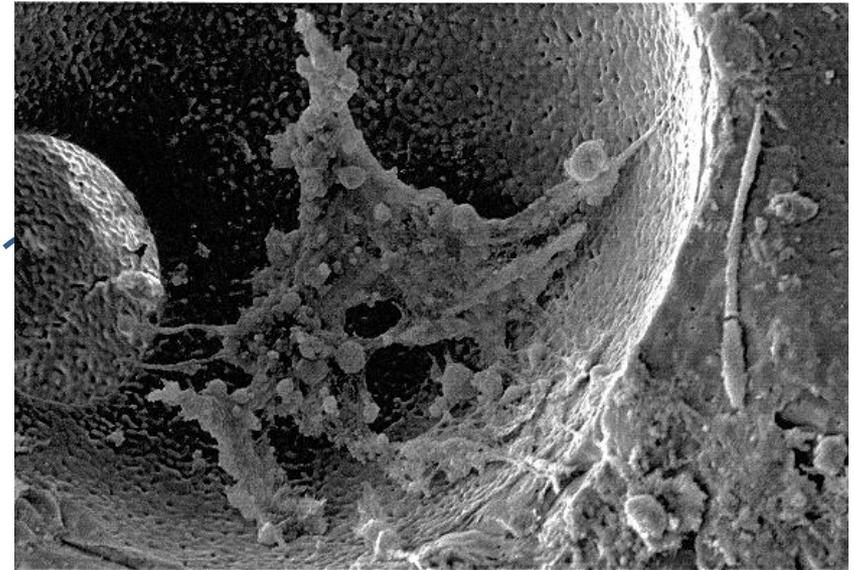
Colonization tests with MG63 osteoblasts



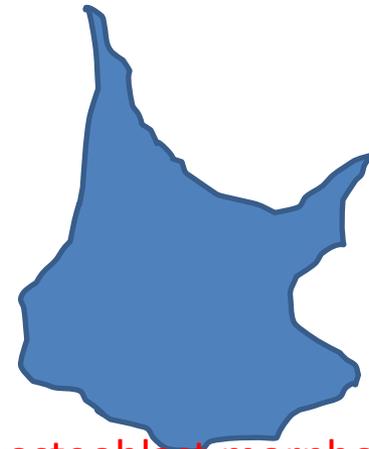
PORTO	mag	HV	det	WD	mode	50 μm	
CEMUP	2 000 x	15.00 kV	ETD	8.9 mm	SE	B4 day 4 Mg63 Surface	



Moving osteoblast morphology



SE **b** 23J22 WD30.2mm 20.0kV x500 100um



Static osteoblast morphology

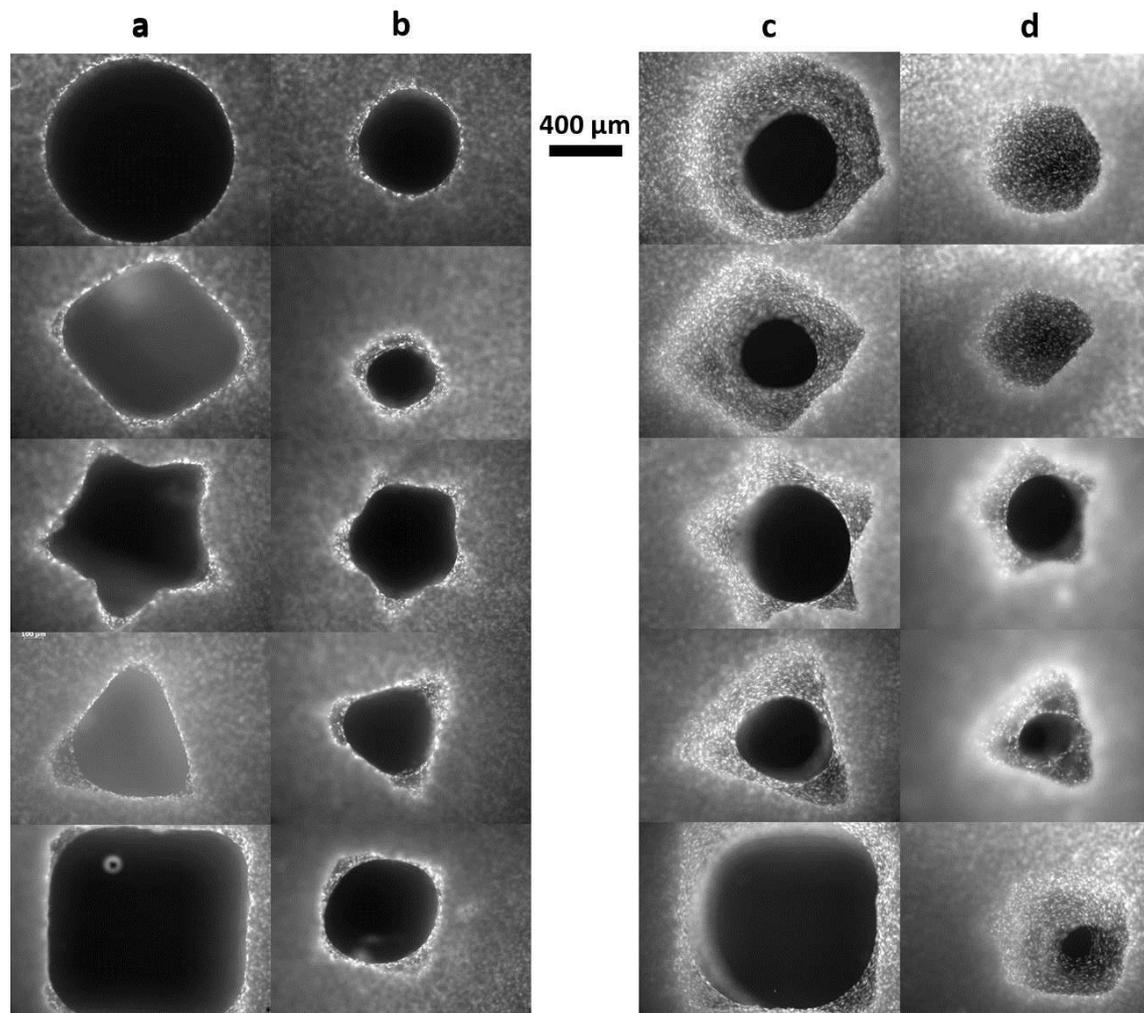
- What will be the impact of these two different macroporosities (size and morphology) on human cell invasion?

The columnar porosity seems to be preferable for osteoblast mobility inside the substitute.

- Is the ice-templated samples porosity size enough large to permit the human cell invasion?

Yes

- What could be the benefit of 3D printing technique for cell invasion? *Marie Lasgorceix Ph thesis (SPCTS Limoges)*



Micrographs by immunofluorescence of porous substrates in SiHA obtained by micro-stereolithography: PhD of Marie Lasgorceix SPCTS Limoges 2014
 large pores (a) and small pores (b), after 7 days of incubation with MC3T3 cells,
 large pores (c) and small pores (d) after 14 days

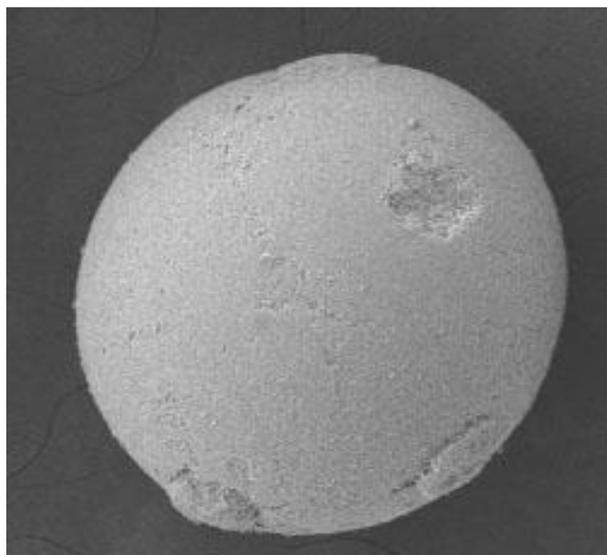
Part III Functionalization of as-prepared scaffolds by drug and phage impregnation through microporosity

Chemical functionalization

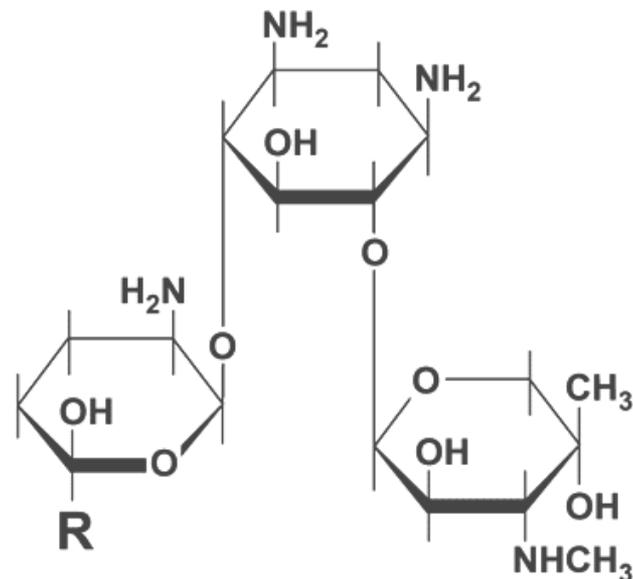
Biological functionalization

Chemical functionalisation

20% μ -porosity



1 mm



gentamicine :

R :

C1A

—CH₂NH₂

C2

—CH(CH₃)NH₂

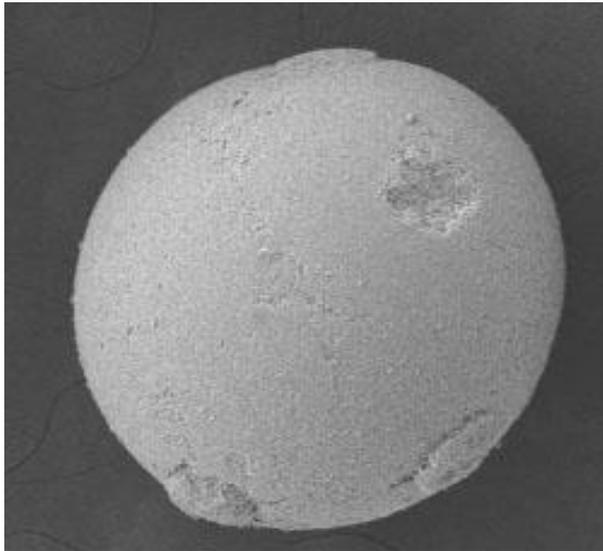
C1

—CH(CH₃)NHCH₃

The micro-porosity allows functionalisation of the ceramic by loading the microstructure with various active substances.

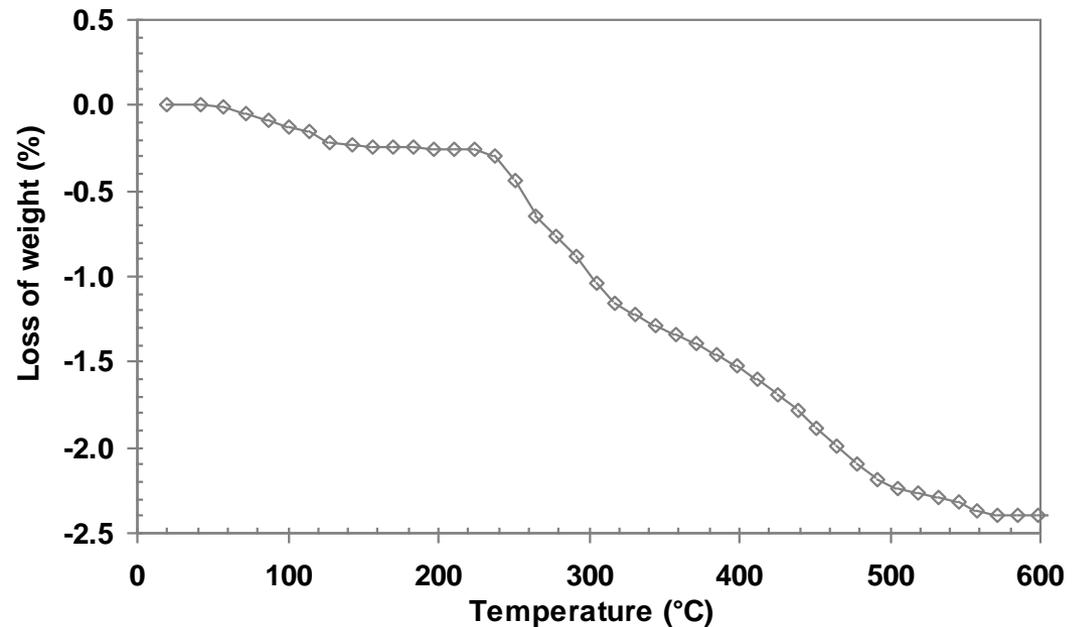
Chemical functionalisation

20% μ -porosity



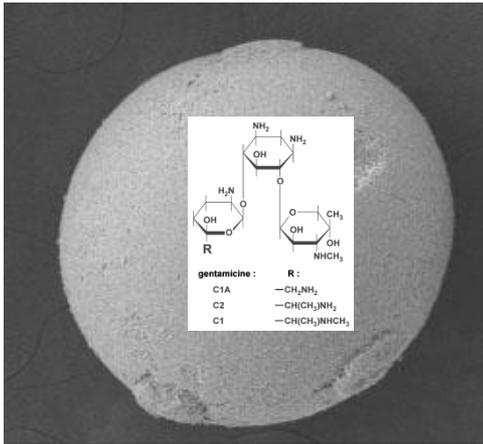
1 mm

TGA of gentamicin loaded HA microporous beads

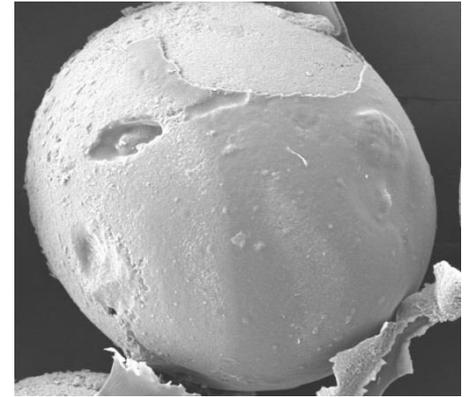


The HA beads are loaded with 40 mg gentamicine /g HA

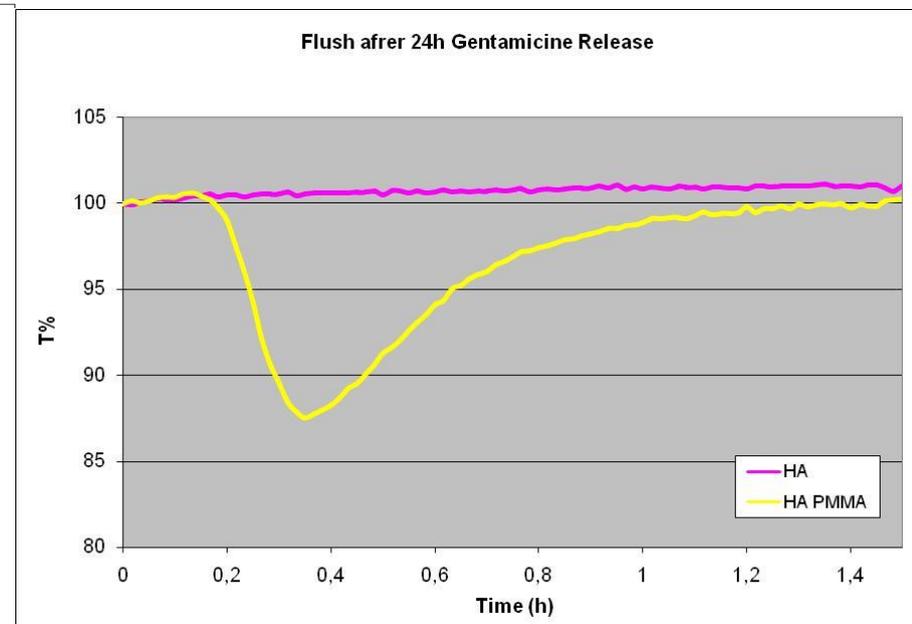
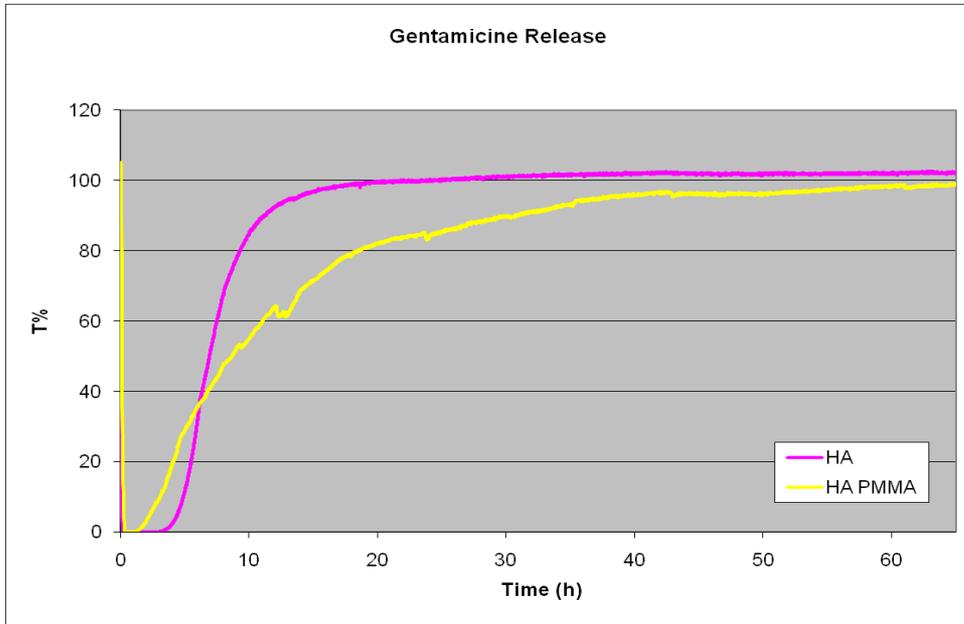
Chemical functionalization



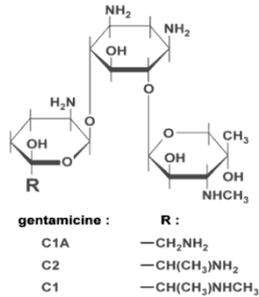
Polymer coating



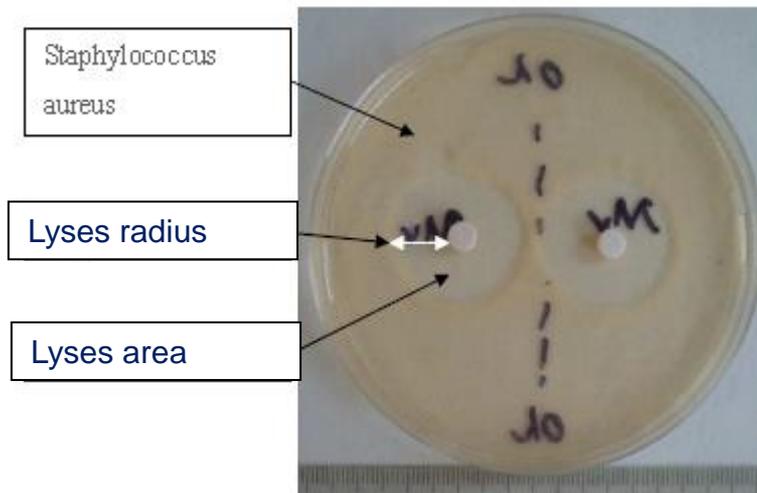
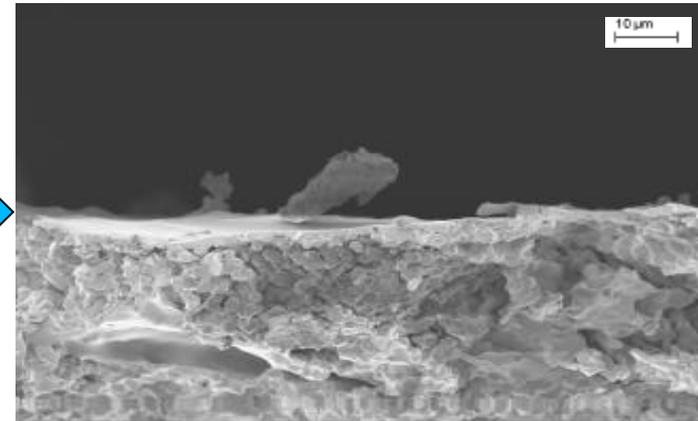
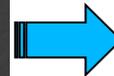
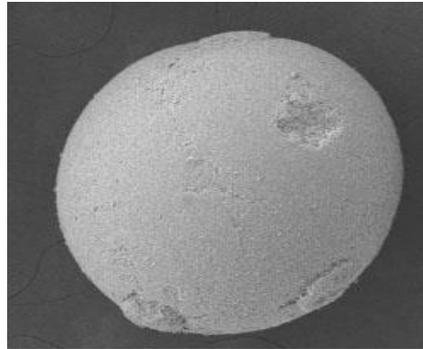
By protecting the surface, it is possible to control the drug delivery



Chemical functionalization



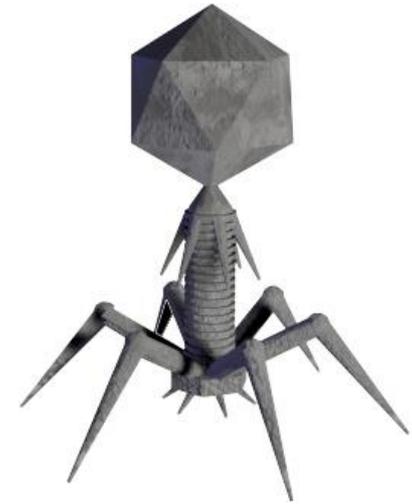
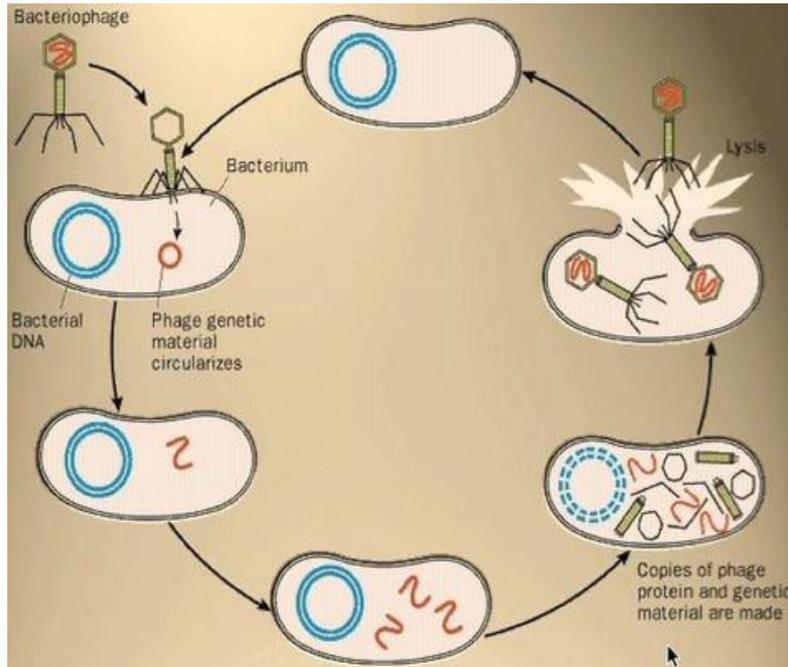
+ polymer



« Functionalisation of porous HA for bone substitutes » E.Meurice et al *JECS* 32 (2012) 2673-2678

Biological functionalization

A bacteriophage (phage) is a virus that infects and replicates only within a specific bacterium



Diameter
24 to 200 nm

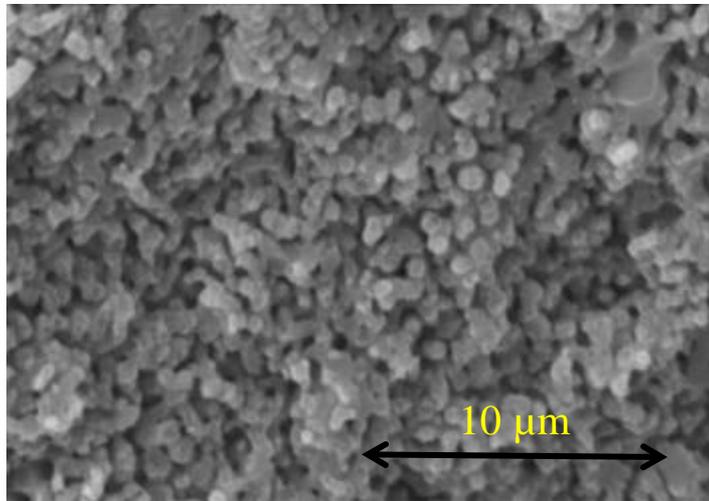
Bacteriophage lytic cycle

The antibacterial activity of ceramics loaded with λ phage was tested on the bacterium Escherichia Coli K12.

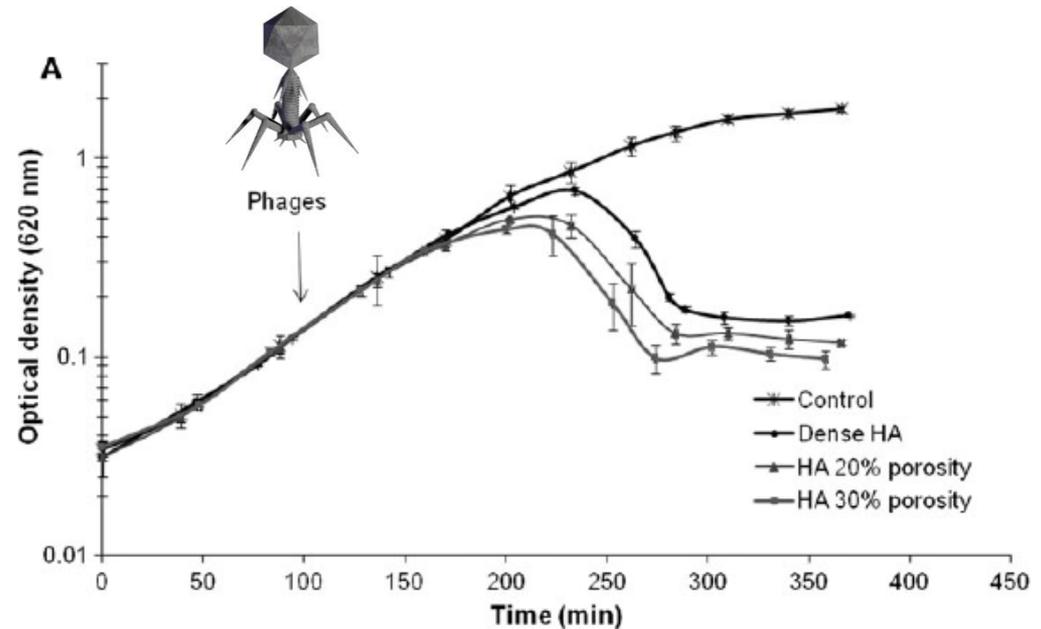
Biological functionalization

Bacterial growth kinetics (*Escherichia coli* K12) was measured by optical density at 620 nm in presence of λ vir phage in ceramic supports with various porosity.

HA samples with different microporosity level (0, 20 and 30%) were incubated for 24 h with 5 ml of λ phage stock and added into culture tubes after obtaining a growth of bacterial two generations.



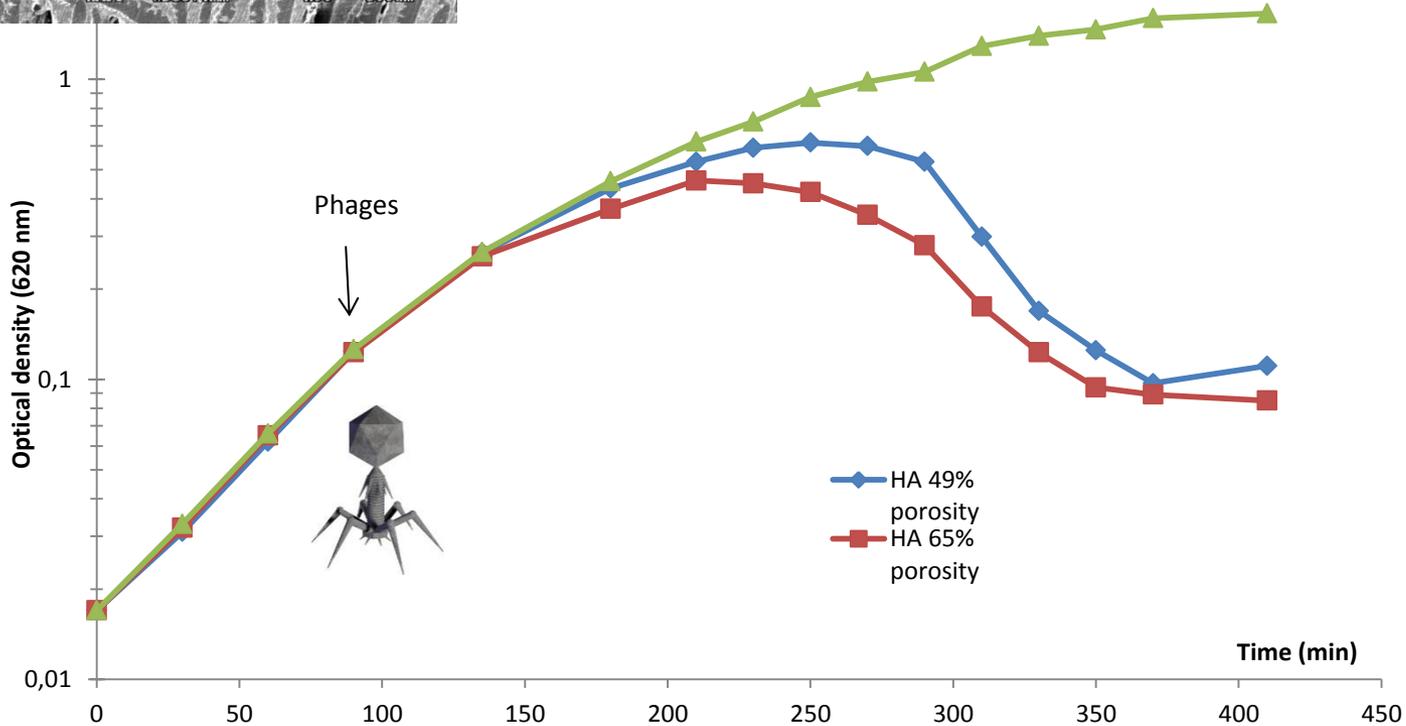
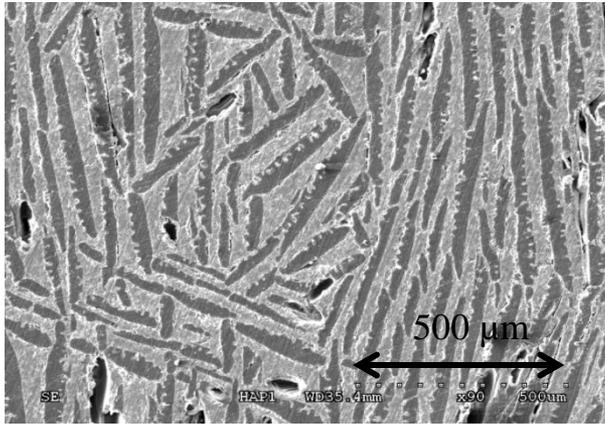
HA 30% μ porosity



A slow down of bacterial growth kinetic was noted after 80 min (HA) followed by the death of bacteria. This phenomenon appears sooner as the microporosity is higher.

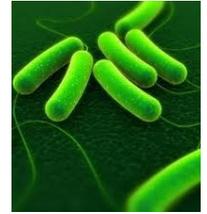
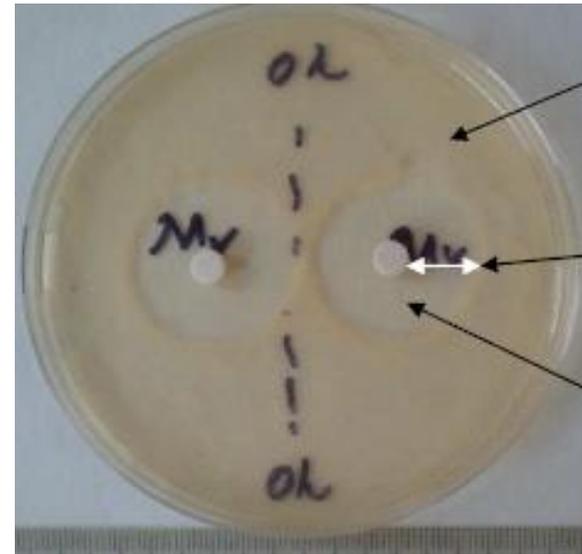
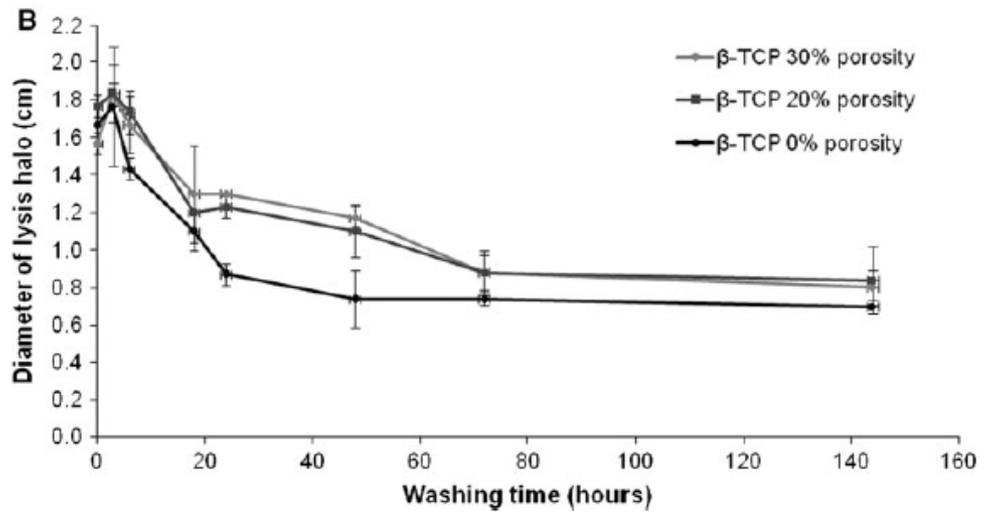
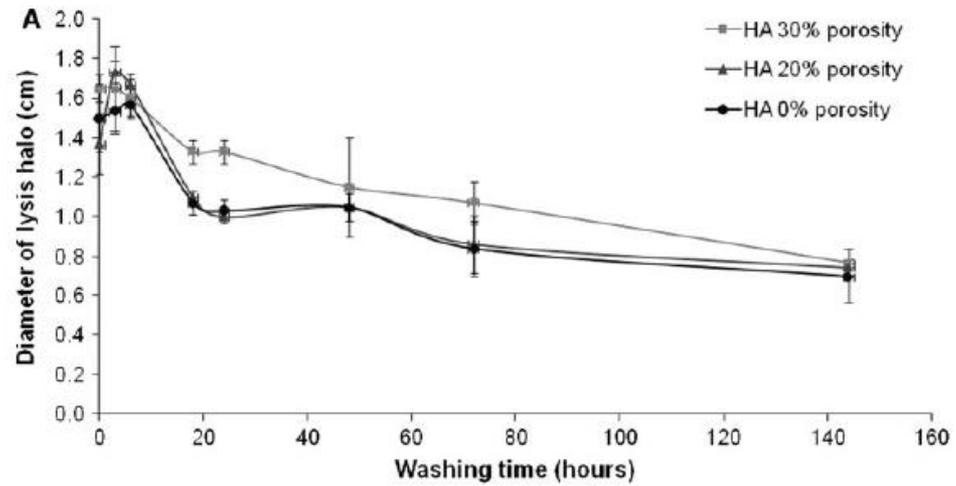
« New antibacterial microporous CaP materials loaded with phages for prophylactic treatment in bone surgery » E.Meurice et al. *Journal of Materials Science: Material of Medicine* 23,10, 2012, 2445-2452.

Biological functionalization



Same effect with ice-templated samples with higher porosity level

Biological functionalization



E. coli



phage

Antibiogram (*Escherichia coli* K12) with lyses diameter measured in presence of phage in ceramic supports with various porosity

Conclusion

The structure of bone substitute obtained by different processes have been compared:

◆ Process using a PMMA bead skeleton allows to obtain an isotropic spherical porosity with a close control of size:

- microporosity: 0 to 40 vol %, μm sized

- macroporosity: 60 to 75 vol %, 200 to 3000 μm pore size and 20 - 400 μm interconnection size.

It is possible by this method to build porosity gradient to mimic the natural bone structure.

◆ Process using ceramic slurry ice templating leads to an oriented porosity structure:

- microporosity: 10 vol%

- macroporosity: 40 to 75 vol%, 180 - 300 μm size (large diameter).

◆ Process using 3D printing should allow to build up continuous pore channels with control of shape and size with gradient from piece core up to the surface.

- macroporosity: up to 80 vol%, customized pore size

Conclusion

◆ Concerning the human cell invasion tests, the columnar porosity obtained by ice-templating method seems surprisingly very favorable for the mobility of osteoblasts inside the substitute.

The shape and size of pores would influence also the cell colonization kinetic.

These results have to be confirmed by dynamic tests which will be performed in the following months by our partners from INEB Instituto de Engenharia Biomedica, University Porto.

This STSM has initiated a collaborative research with INEB. The following actions are a co-direction with F.Monteiro of a starting PhD thesis and a financial support for the PhD student has been obtained from JECS Trust for a 2 month stay at INEB.

◆ The microporosity allowing a better control of resorbability can be also used as biological substances and phage supports.

This study has shown that phage loaded ceramics could be used in bone prophylactic treatments.



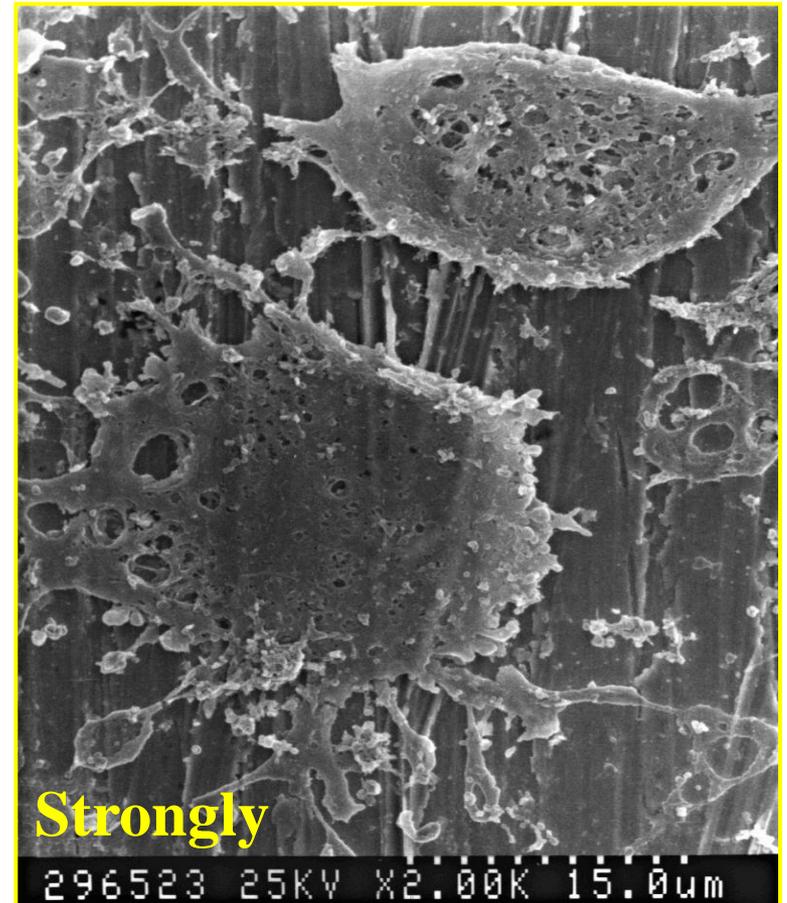
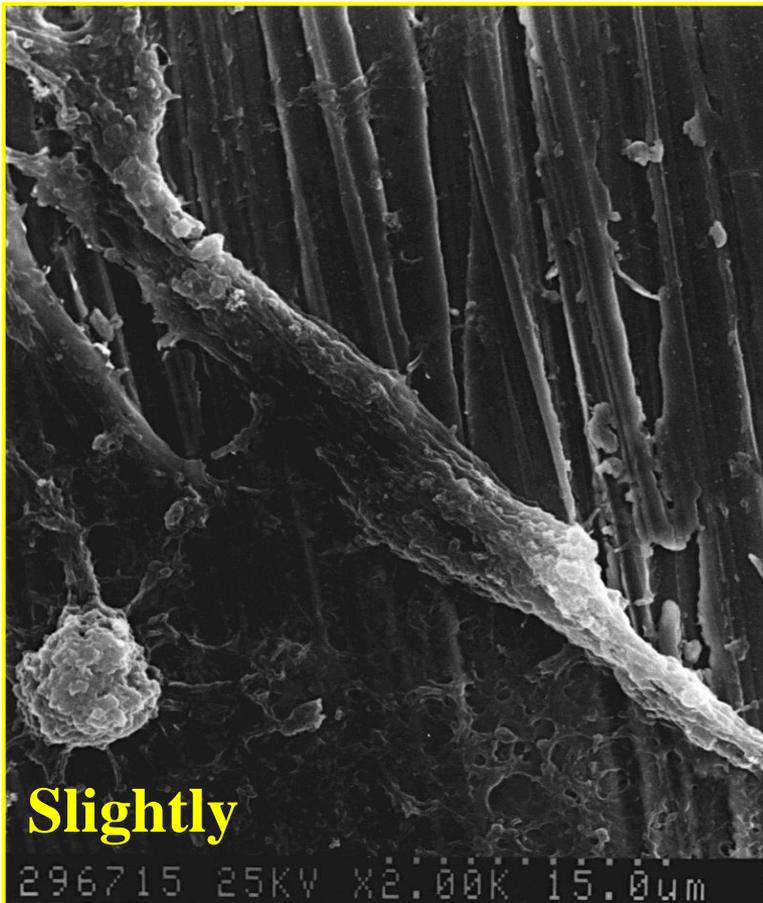
Thank you
for your attention

Osteoblasts MG63

- 2 multi-well plates (48 wells)
- 2×10^5 cell/ml α -MEM + 10% FBS, 1% ascorbic acid, 1% penicillin, 1% fungicide.
- 37°C under 5% CO₂.
- After 24 hours or 4 days if incubation: coloration with MTT (0,5 mg/ml) during 3 hours.

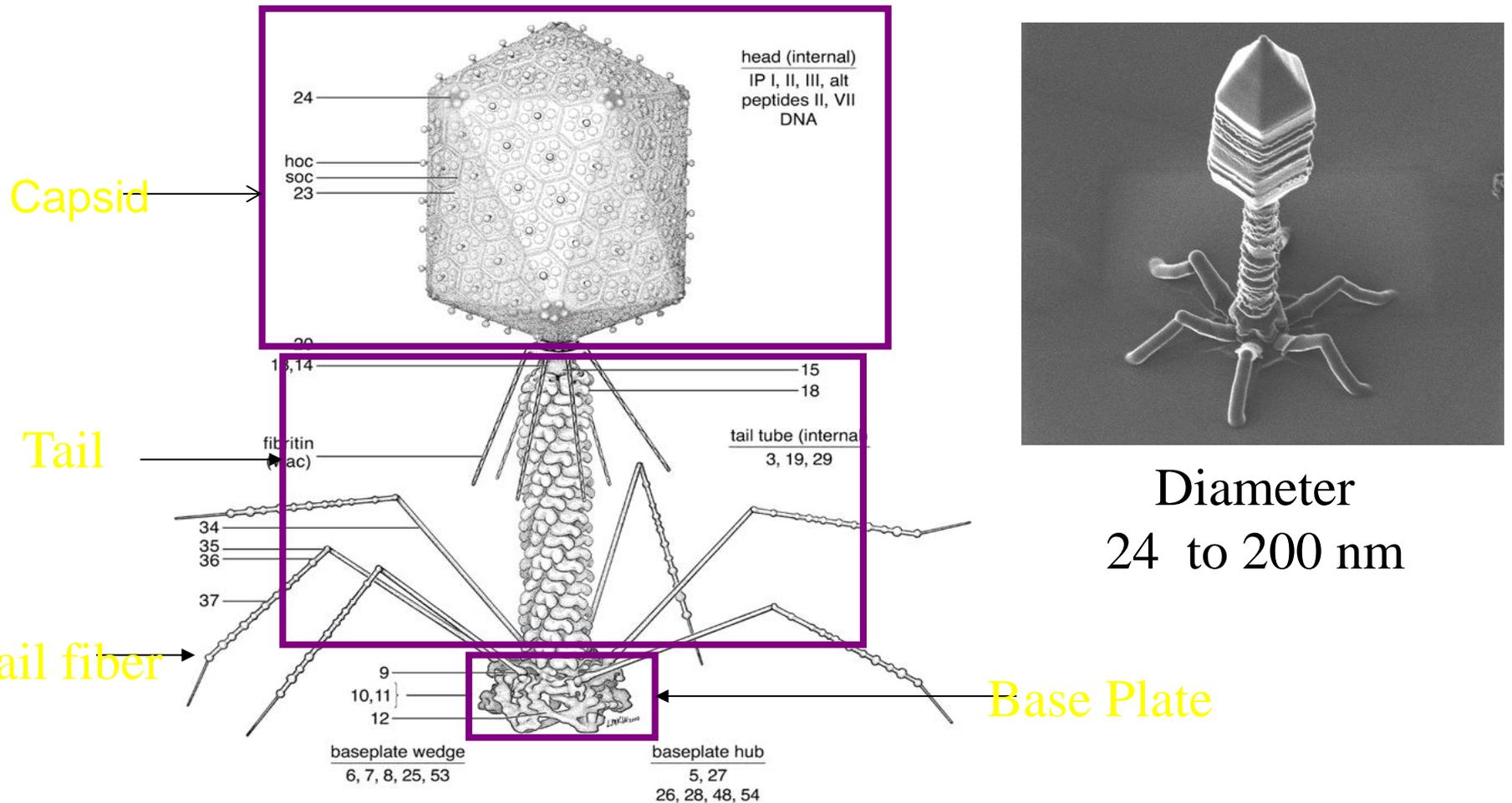


NIH 3T3 Fibroblasts (6 days)



Biological functionalization

A bacteriophage (phage) is a virus that infects and replicates only within bacteria.



Discovered in 1915 by Frederick W. Twort and Felix d'Hérelle

Biological functionalization

The bacterium *Escherichia coli* K12 strain is lytic λ phage sensitive.

-The bacterium was grown at 150 rpm and incubated at 37°C, in agitation 170 rpm in Luria-Bertani broth

-Solid media used is the R-medium (added agar at 15 g/L).

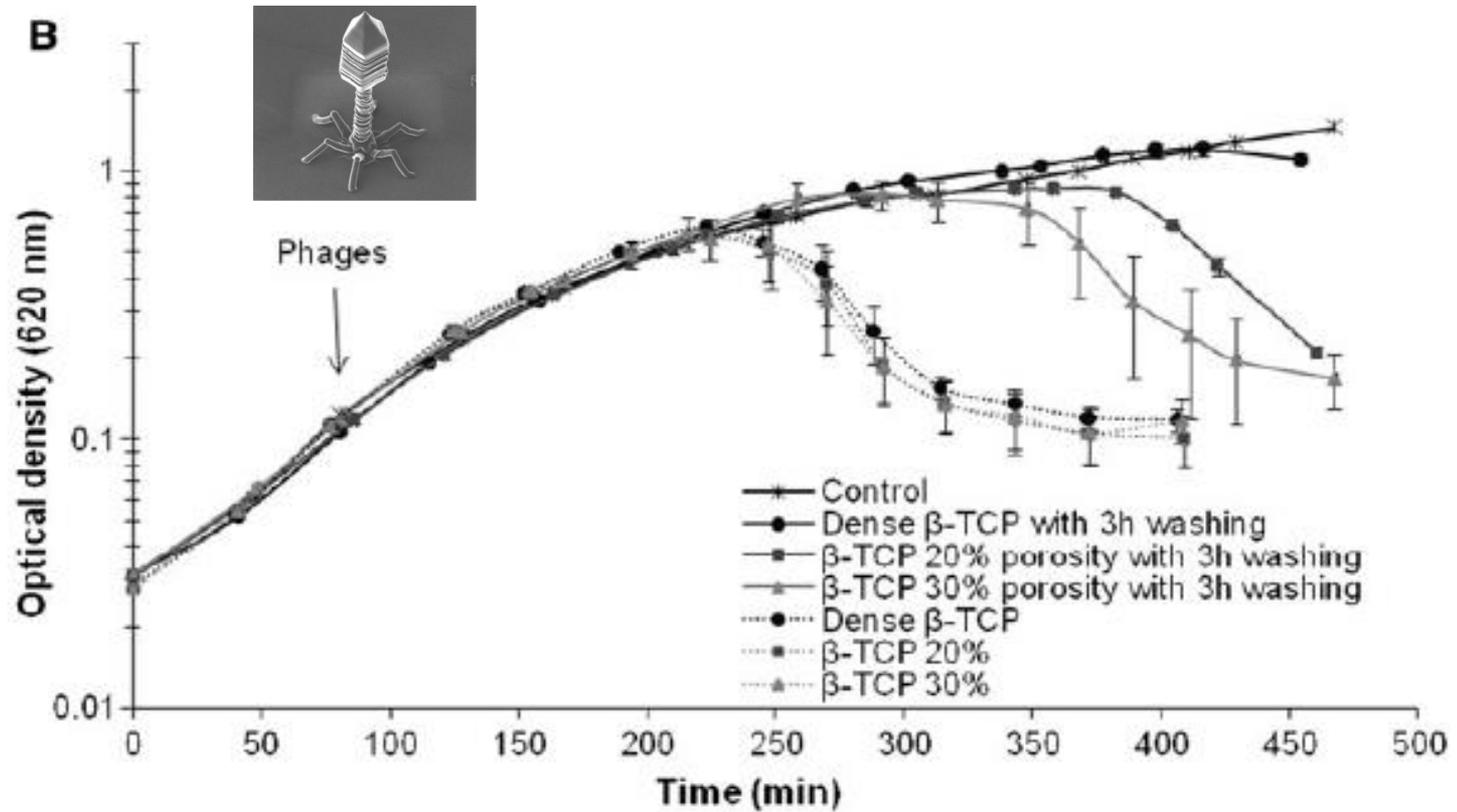
-Phage λ vir stock was prepared by infecting *Escherichia coli* K12 strain (A324).

-HA and TCP samples with different porosity level (0, 20 and 40%) were incubated for 24 h with 5 ml of stock λ phage.

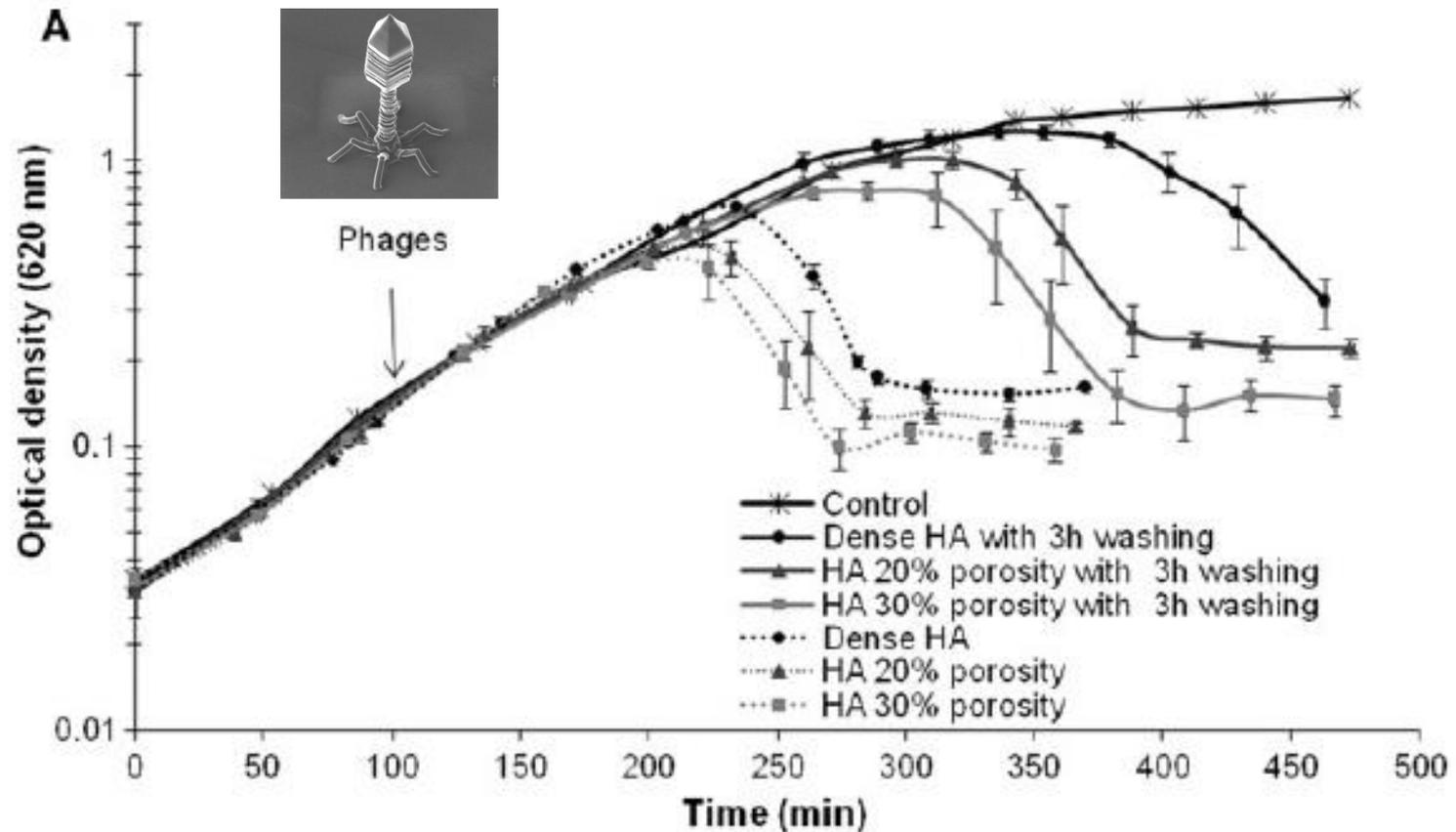
-After incubation, the sample was washed once with LB medium to remove excess phage suspension.

-Cultures of 30 ml of *Escherichia coli* K12 (A324) in LB liquid medium were performed for each condition. The growth of *E. coli* was performed at 37°C with agitation at 170 rpm.

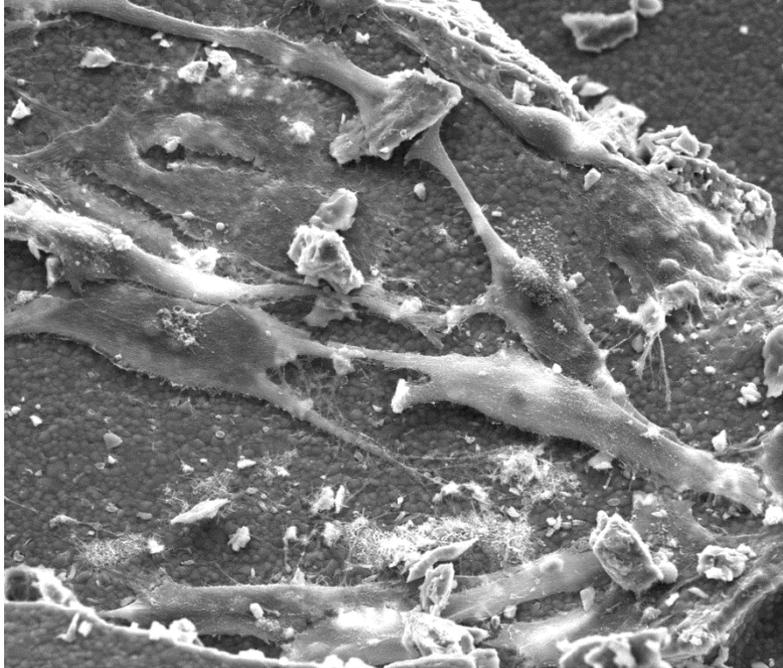
Biological functionalisation



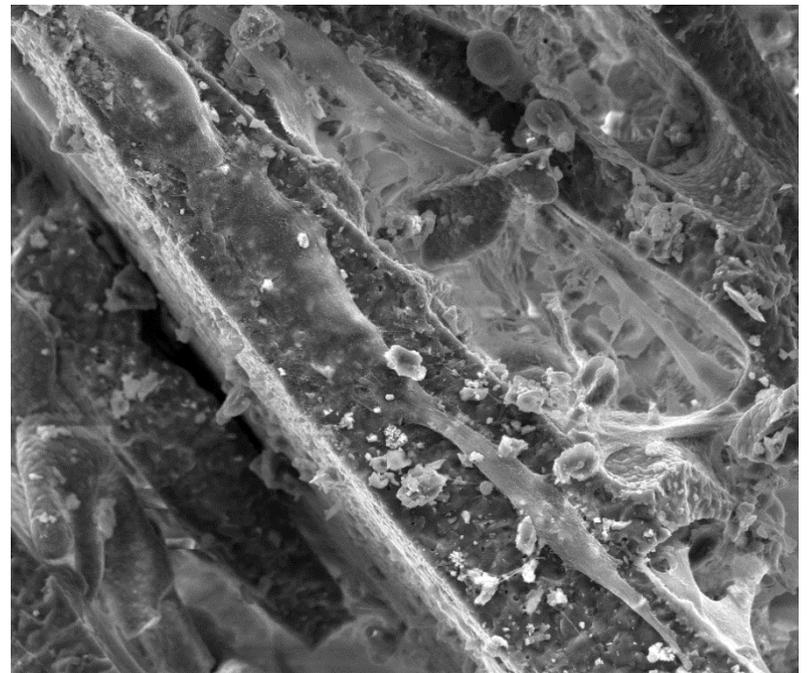
Biological functionalisation



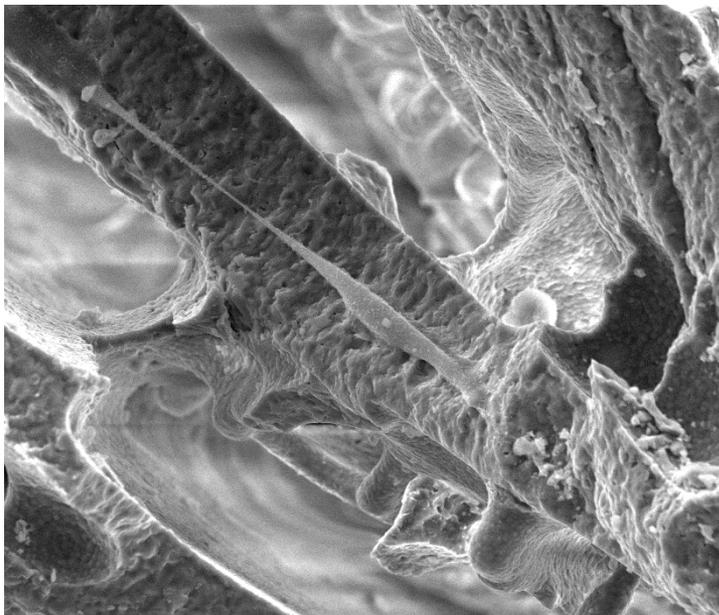
Bacterial growth kinetics (*Escherichia coli* K12) measured by optical density at 620 nm in presence of phage in ceramic supports with various porosity



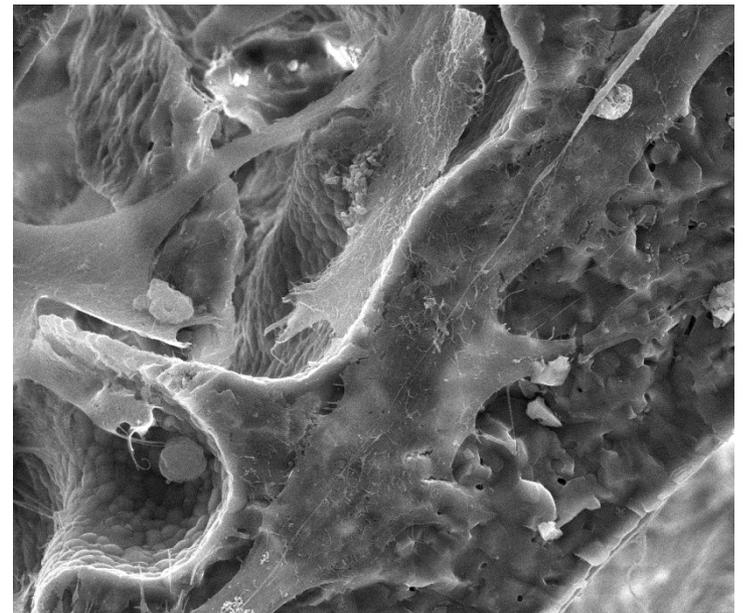
PORTO CEMUP mag 2 000 x HV 15.00 kV det ETD WD 9.7 mm mode SE 50 µm B1 day 4 Mg63 Fracture



PORTO CEMUP mag 2 000 x HV 15.00 kV det ETD WD 10.1 mm mode SE 50 µm B1 day 4 Mg63 Surface

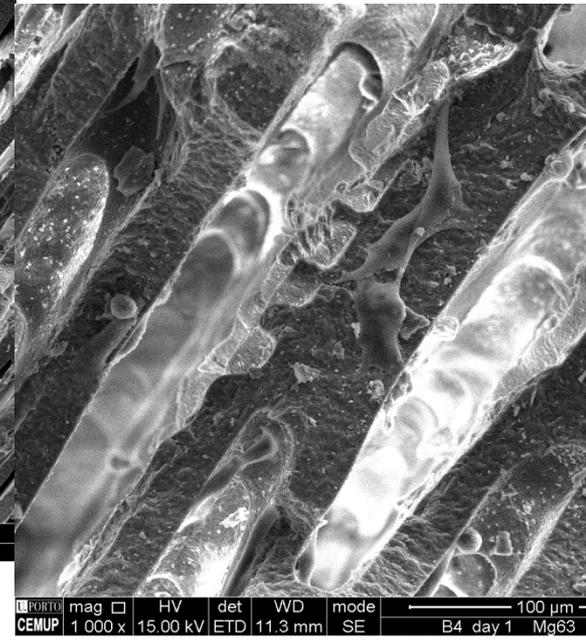
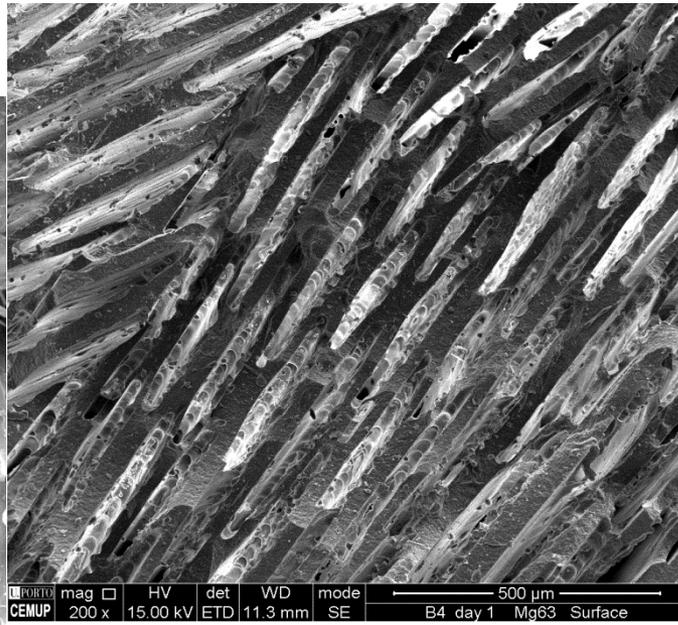
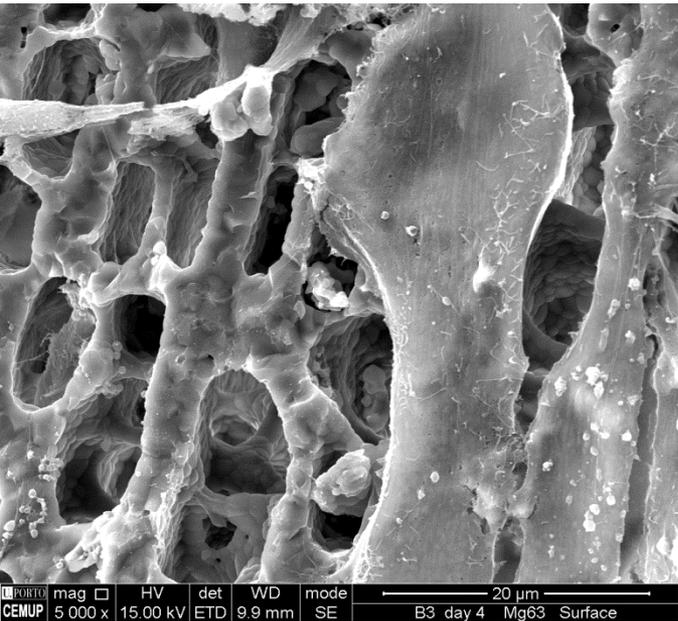
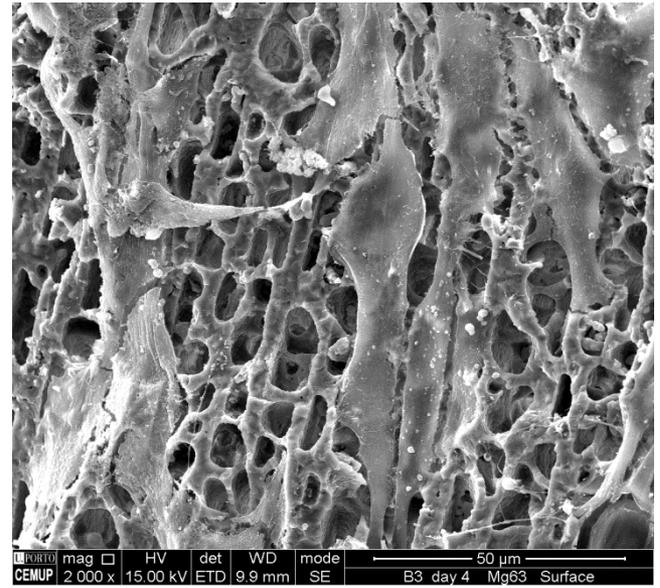
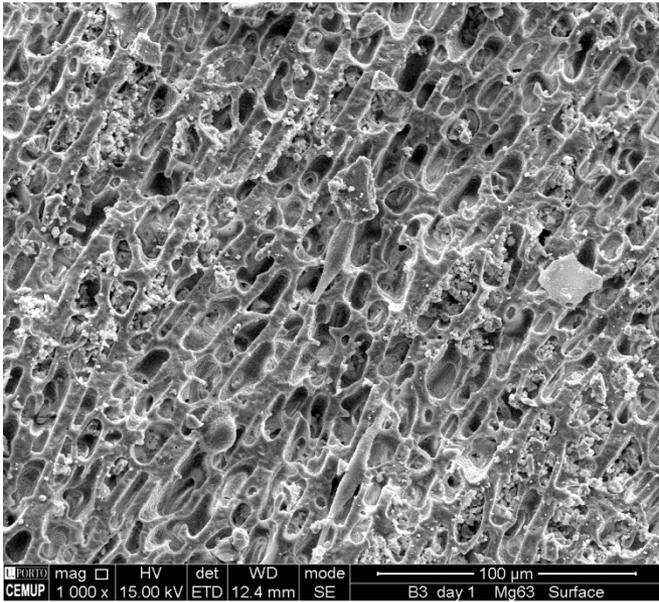


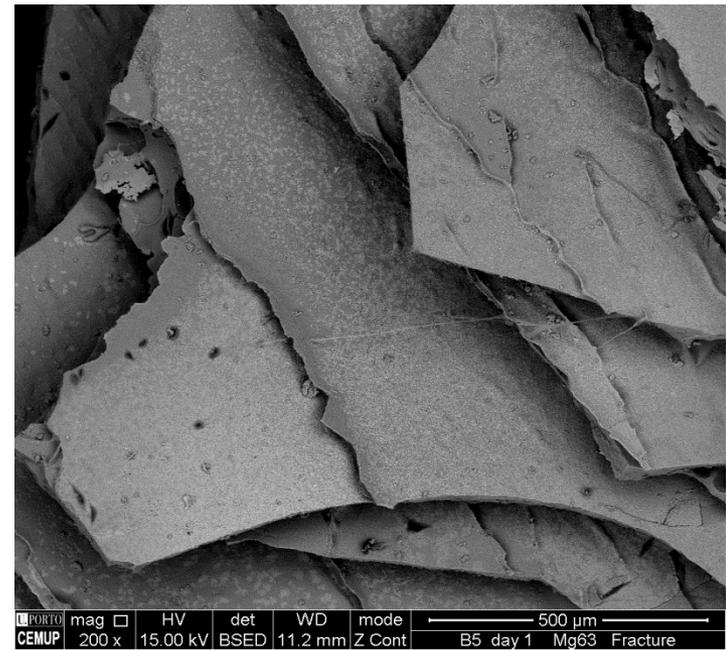
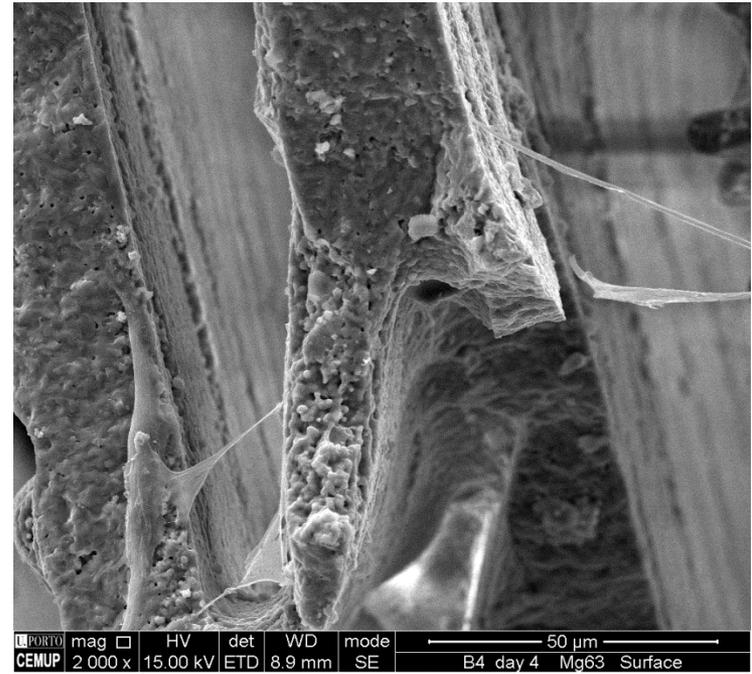
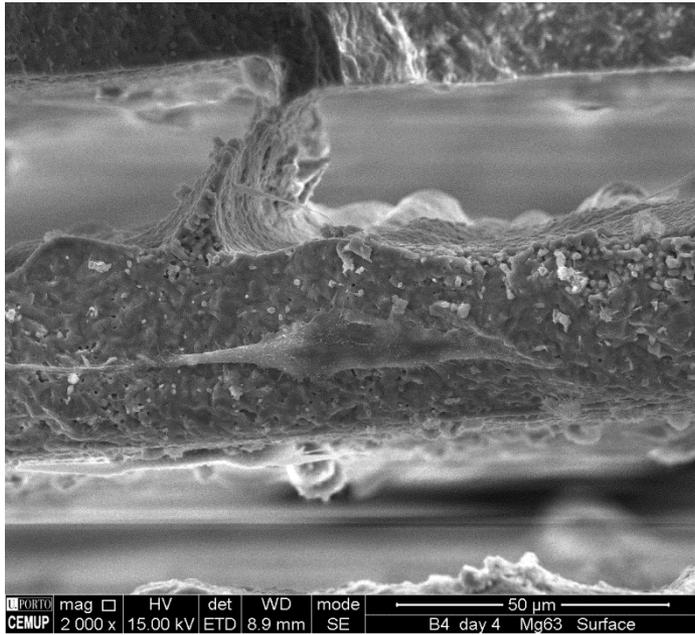
PORTO CEMUP mag 2 000 x HV 15.00 kV det ETD WD 10.9 mm mode SE 50 µm B2 day 1 Mg63 Surface

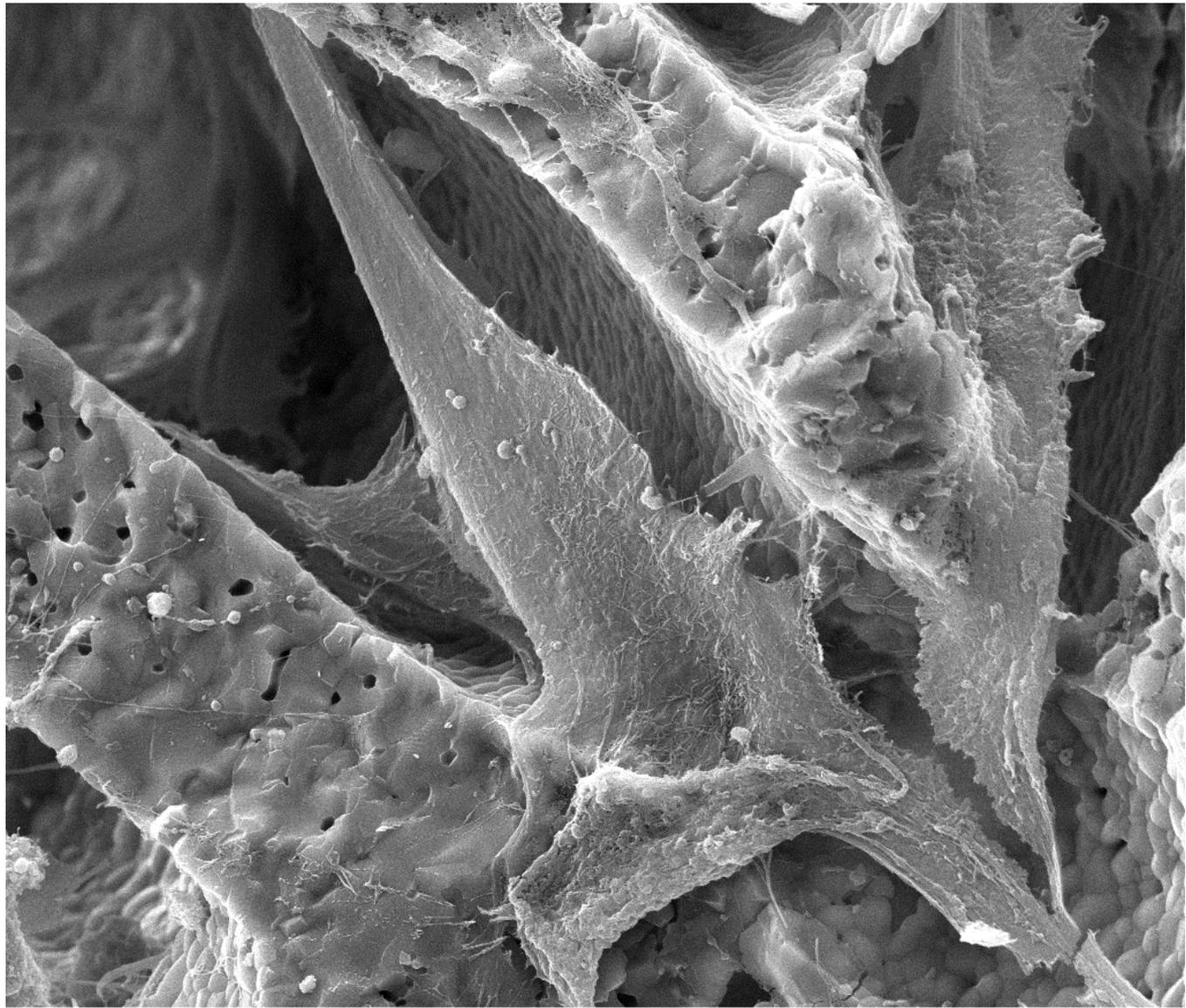


PORTO CEMUP mag 5 000 x HV 15.00 kV det ETD WD 9.1 mm mode SE 20 µm B2 day 4 Mg63 Surface

OK







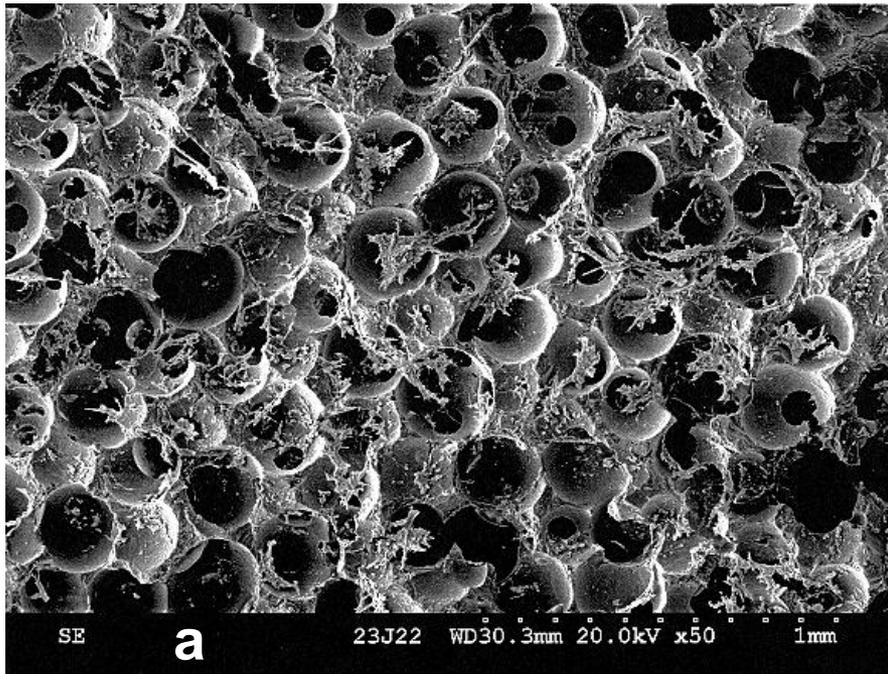
PORTO	mag □	HV	det	WD	mode	← 20 μm →
CEMUP	5 000 x	15.00 kV	ETD	9.6 mm	SE	B6 day 4 Mg63 Surface

Ceramic slurry infiltration of organic skeleton

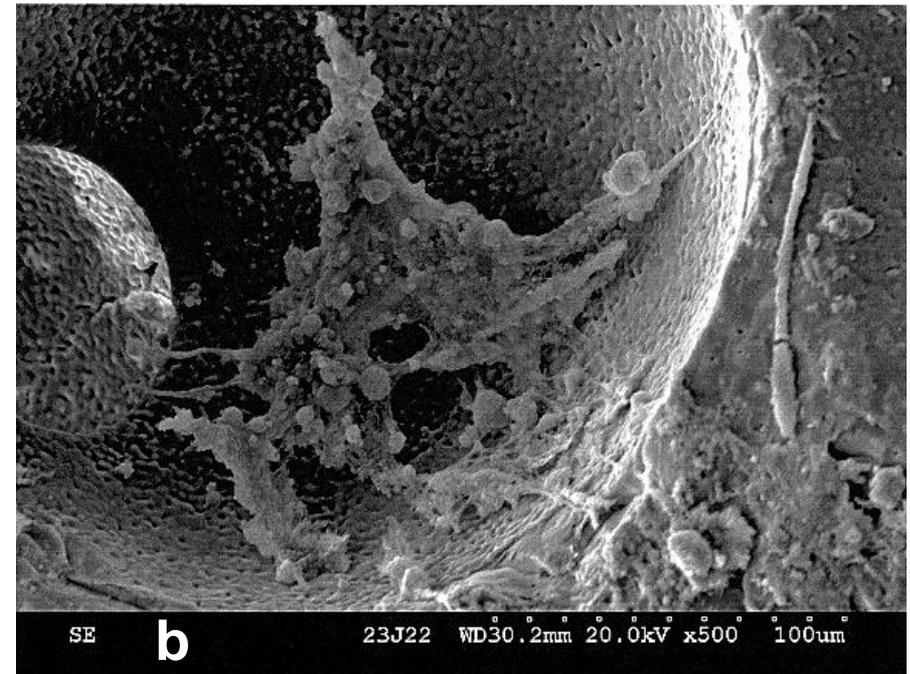
- 65% porosity (limits: 65-75%)
- 100 μm interconnections
- 500-600 μm pore diameter



- HA 15 MPa
- TCP >15 MPa



Macro/meso-porous HA samples colonized by MC3T3-E1 osteoblasts after a 6-days culture (a).



First mineralized bone particles can already be detected (b).

With the collaboration of GRB University Lille2 (Prof Hildebrand's team)