

A photograph of a light-colored ceramic disc with a porous, honeycomb-like top surface. The disc is centered in the frame, and the background is a plain, light-colored surface. The porous layer is uniform in thickness and covers the entire top surface of the disc.

**CeramTec**

T H E C E R A M I C E X P E R T S

**„CeraPore“ –  
Structural surface modification  
of dense load-bearing ZTA**

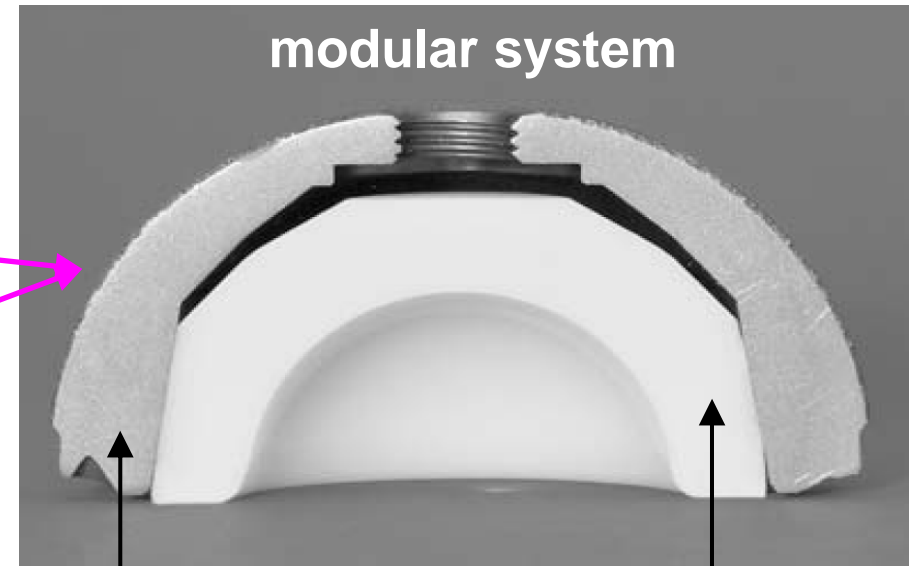
*Norbert Schneider*



- ▶ **Background**
- ▶ Coating and sintering process
- ▶ Surface properties
- ▶ Mechanical properties
- ▶ Cellbiological / Clinical results
- ▶ Regulatory aspects
- ▶ General project risks



TrilogY<sup>®</sup> IT Acetabular System by Zimmer



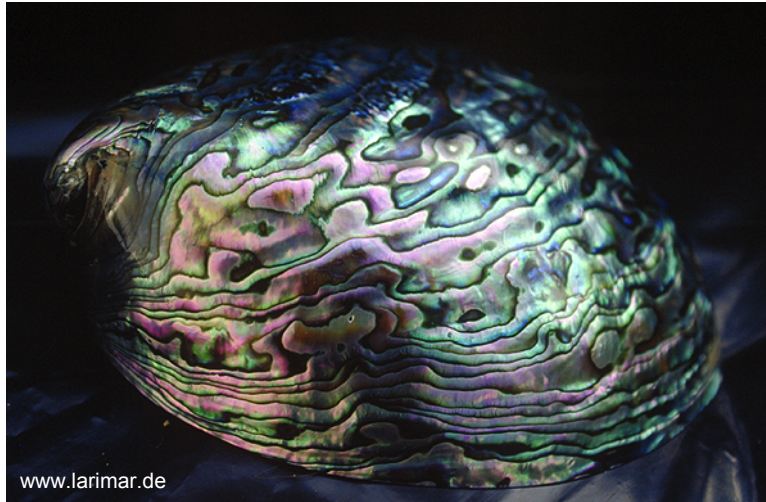
metal shell with  
osseointegrative coating  
(ingrowth of bone)

ceramic insert  
excellent tribological  
performance

- ▶ high wall thickness of the system
- ▶ risk of surgical error when seating ceramic insert
- ▶ risk of aseptic loosening due to metal ions



nacre



www.larimar.de

Damascene-steel



Hochschule Göttingen

bone

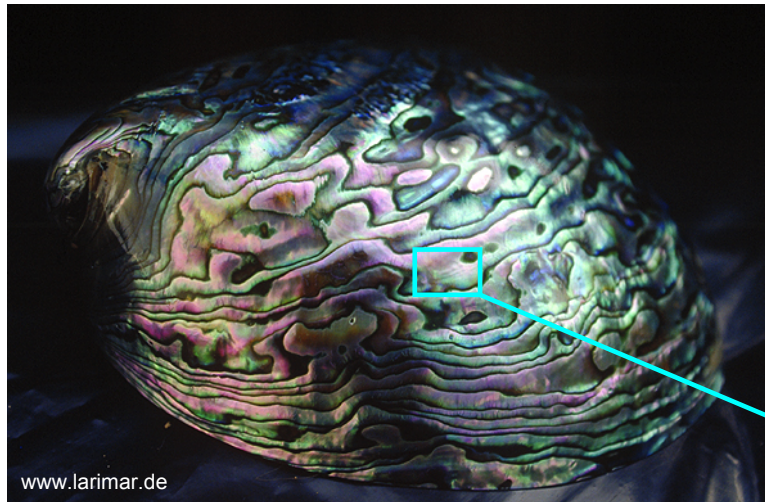


www.digitalefolien.de

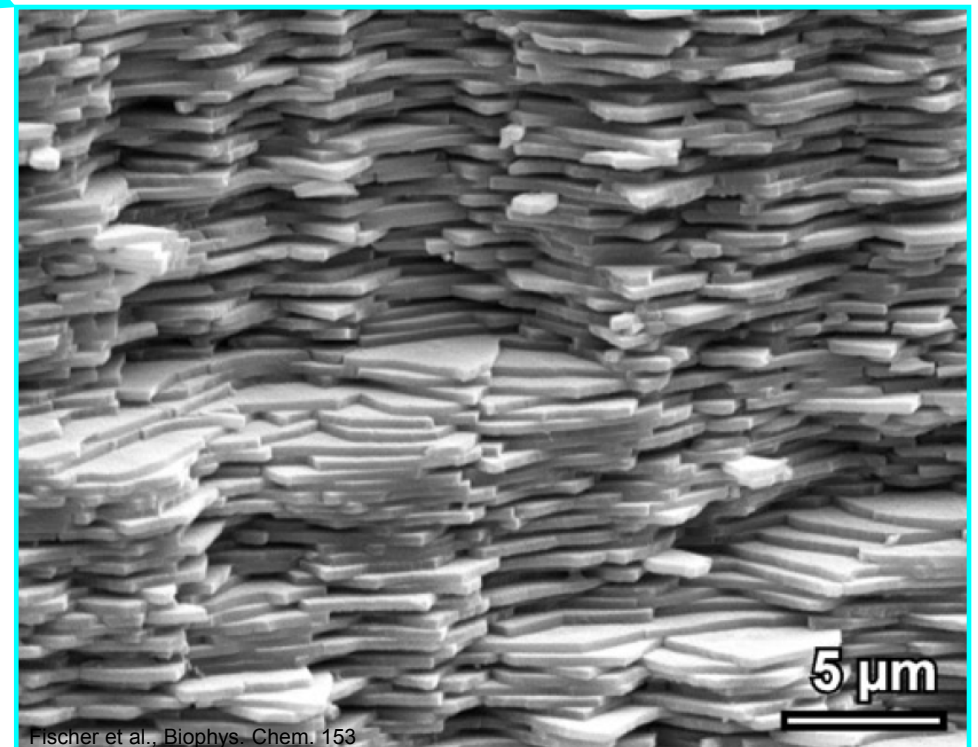
BIOLOX<sup>®</sup> delta



▶ nacre

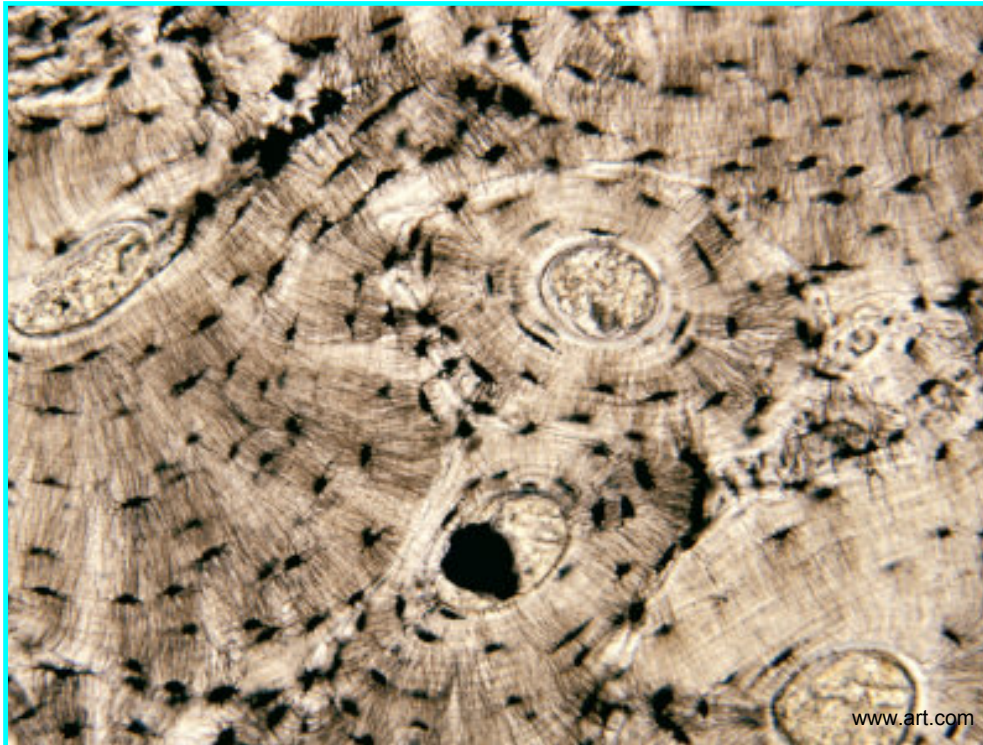
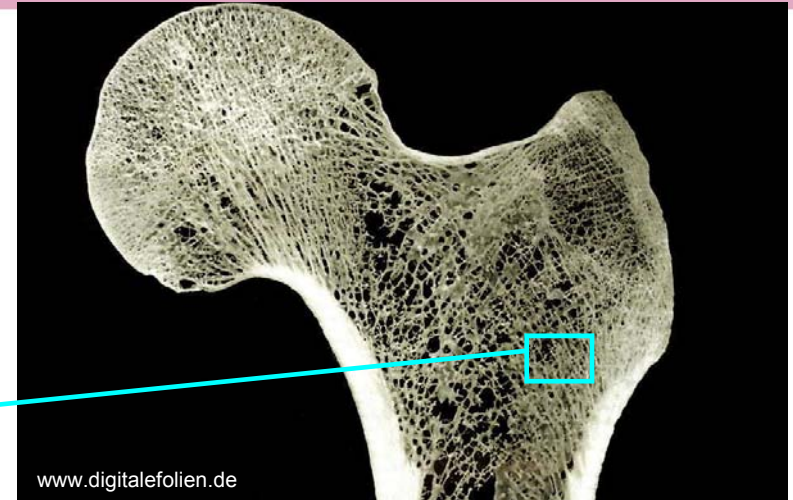


- ▶ **composite-Werkstoff:**  
95 % aragonite  
5 % proteins & chitin
- ▶ **Young's modulus:**  
up to 80 GPa
- ▶ **fracture toughness:**  
1 - 8 MPa m<sup>1/2</sup>





▶ bone

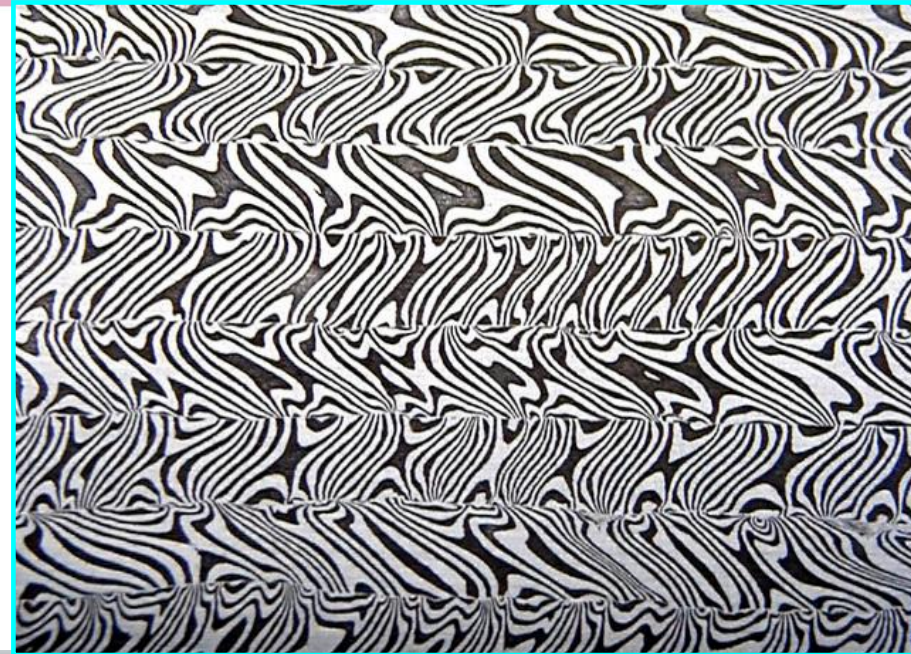


- ▶ **composite-material:**
  - 70 % hydroxyapatite & calciumphosphate
  - 20 % collagen & proteoglycane
  - 10 % water
- ▶ **Young's modulus:**
  - appr. 30 GPa
- ▶ **fracture toughness:**
  - 2 – 12 MPa m<sup>1/2</sup>

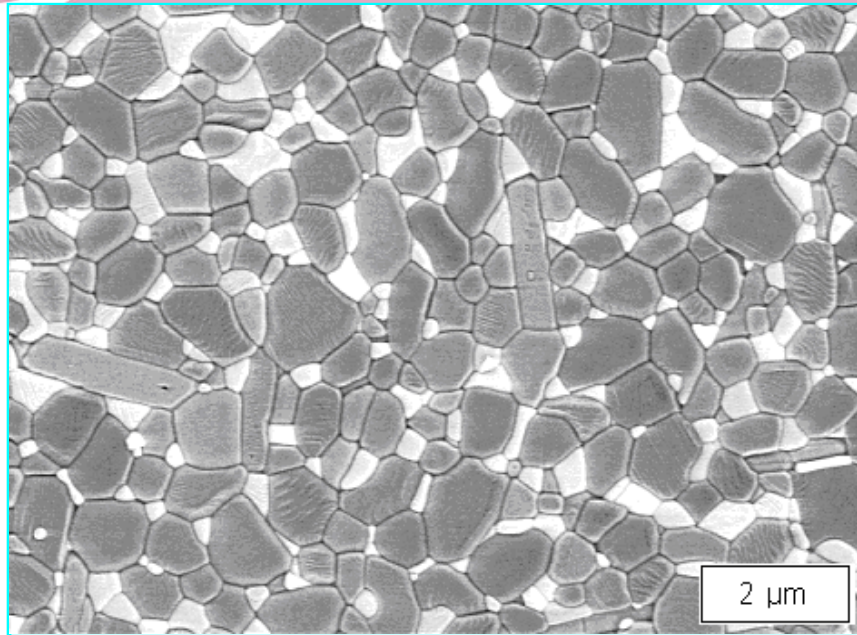
## Damascene-steel



Hochschule Göttingen

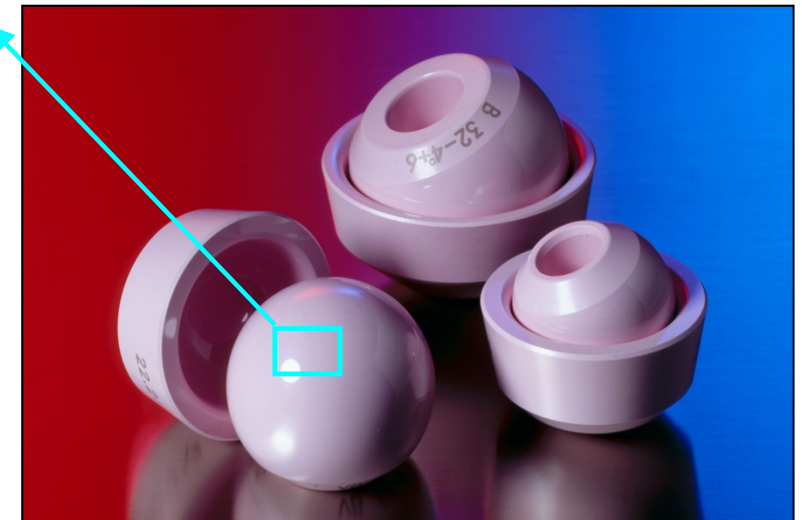


- ▶ **composite-material:**  
50 % low-C steel  
50 % rich-C- or P steel
- ▶ **Young's-modulus:**  
210 GPa
- ▶ **fracture toughness:**  
50 MPa m<sup>1/2</sup>



BIOLOX<sup>®</sup>delta

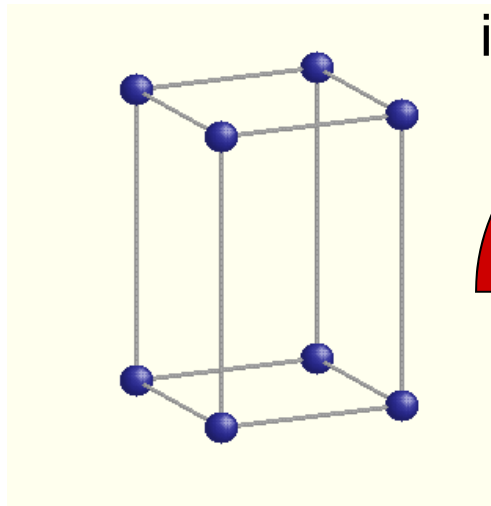
- ▶ **composite-material:**
  - 80 % Al<sub>2</sub>O<sub>3</sub>
  - 17 % ZrO<sub>2</sub>
  - 3 % toughening platelets
- ▶ **Young's modulus:**  
360 GPa
- ▶ **fracture toughness:**  
6.5 MPa m<sup>1/2</sup>





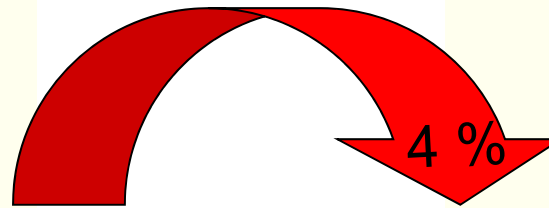


**tetragonal:**  
 $\rho = 6,10 \text{ g/cm}^3$

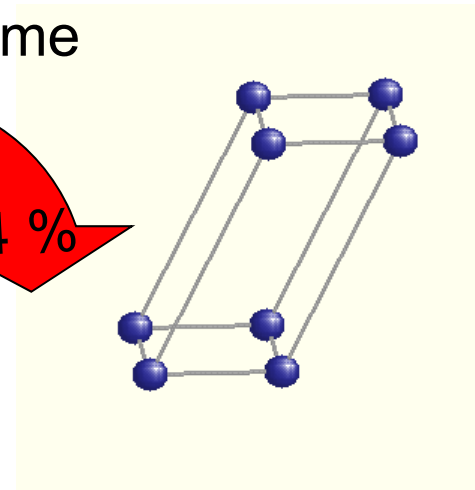


$1170 \text{ }^\circ\text{C} < T$

increase of volume



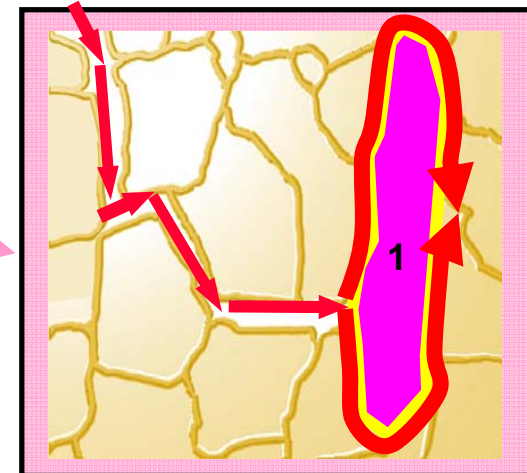
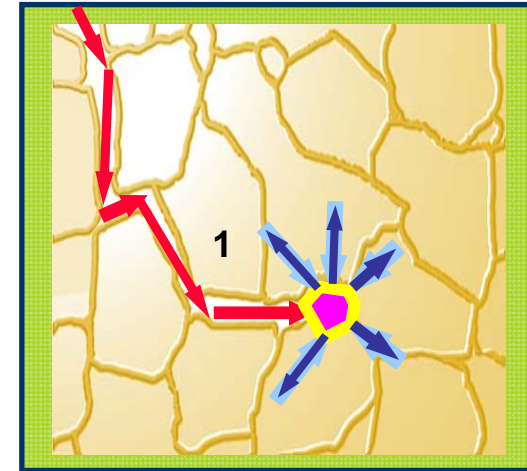
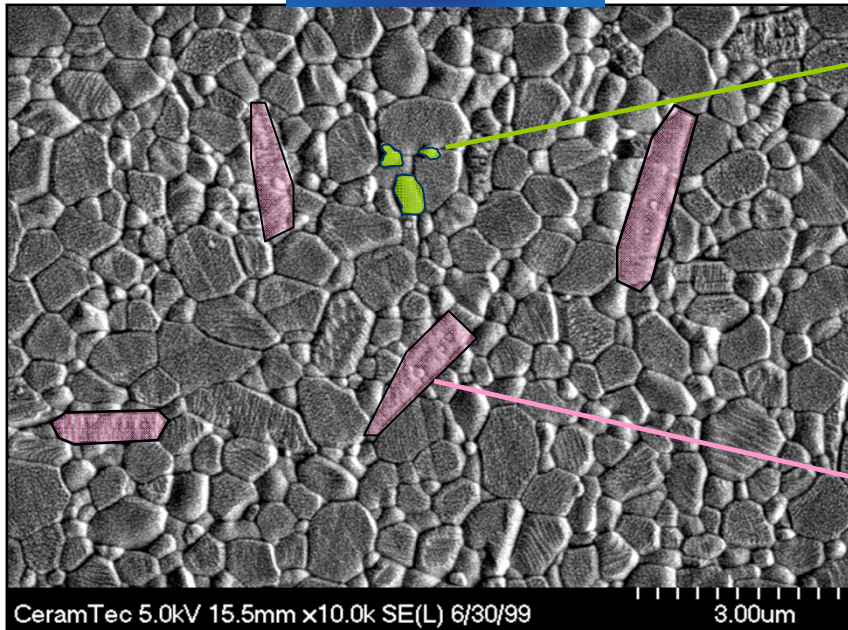
**monoclinic:**  
 $\rho = 5,85 \text{ g/cm}^3$



$T < 1170 \text{ }^\circ\text{C}$

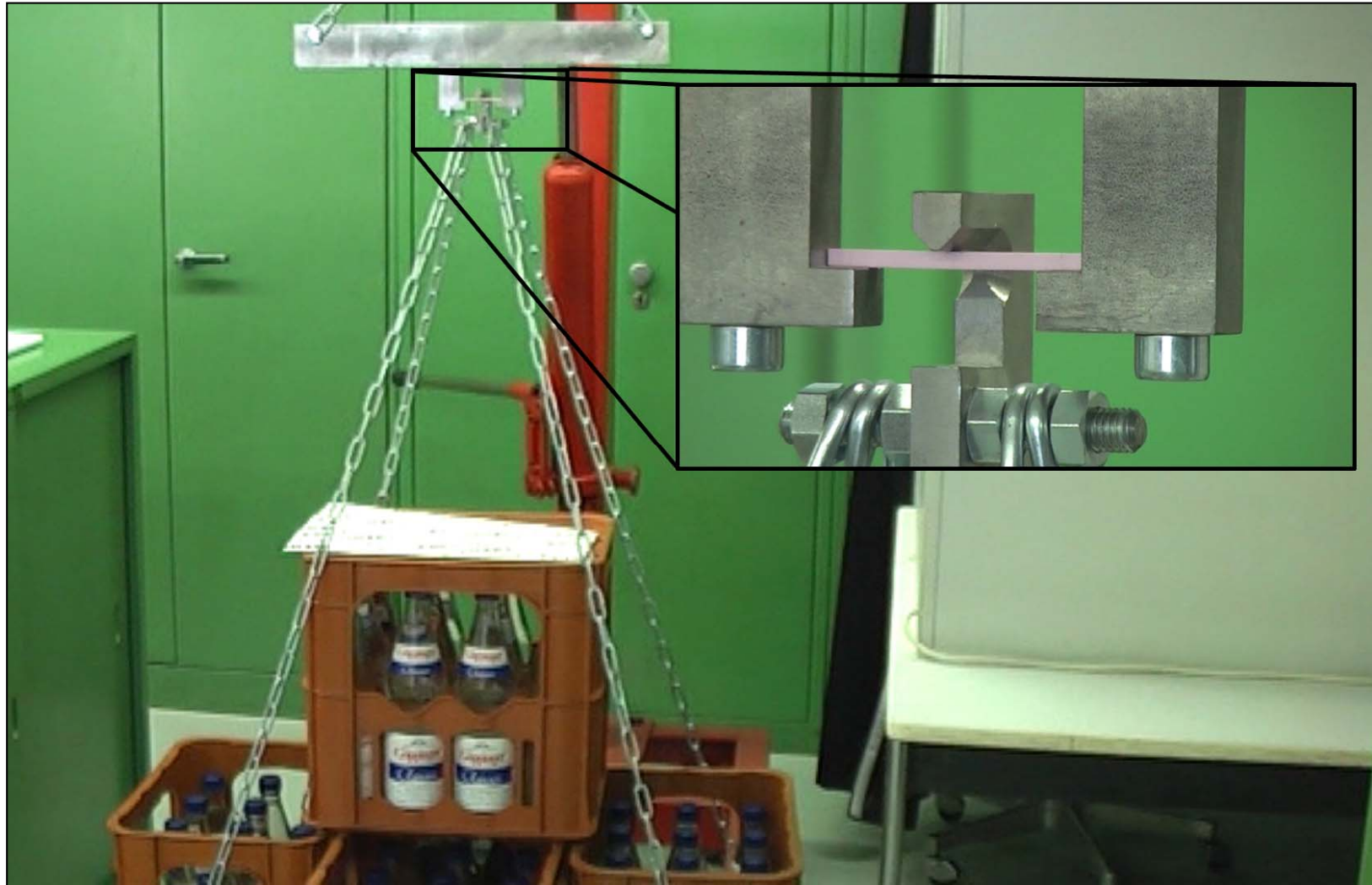


# Toughening mechanisms in BIOLOX<sup>®</sup>delta



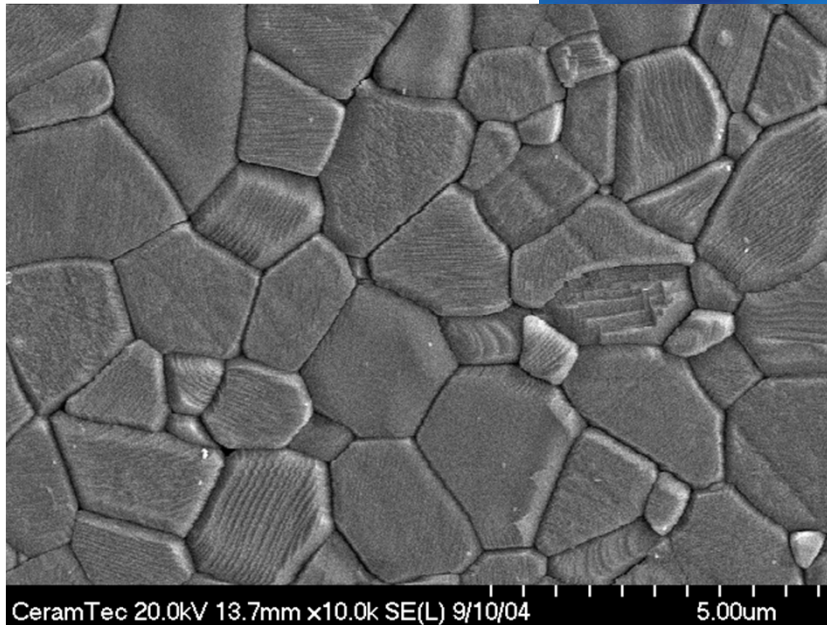


# 3-point-bending strength



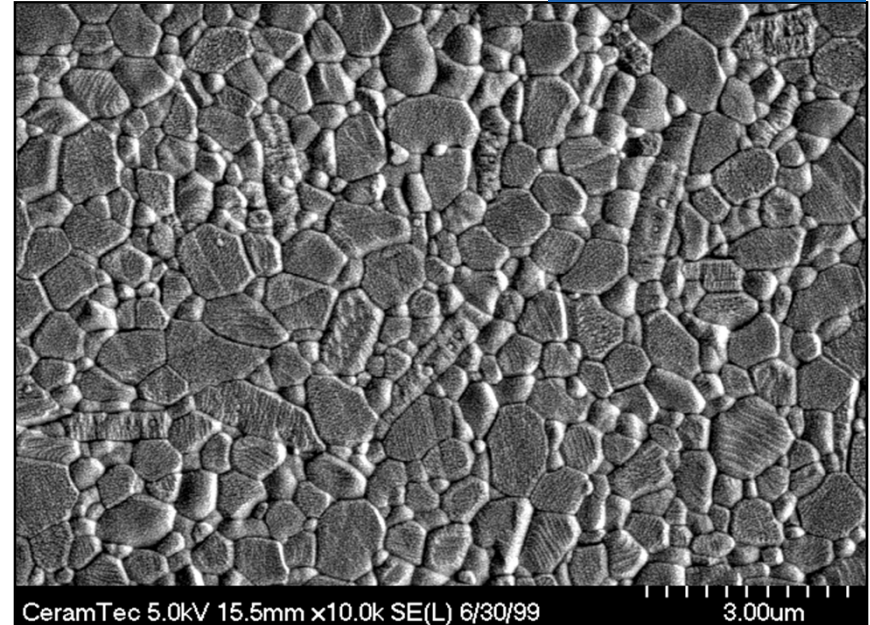


BIOLOX<sup>®</sup> forte



99,8 Vol.% Al<sub>2</sub>O<sub>3</sub> +  
0,2 Vol.% other oxides

BIOLOX<sup>®</sup> delta



80 Vol.% Al<sub>2</sub>O<sub>3</sub> + 17 Vol.% ZrO<sub>2</sub> +  
3 Vol.% other oxides

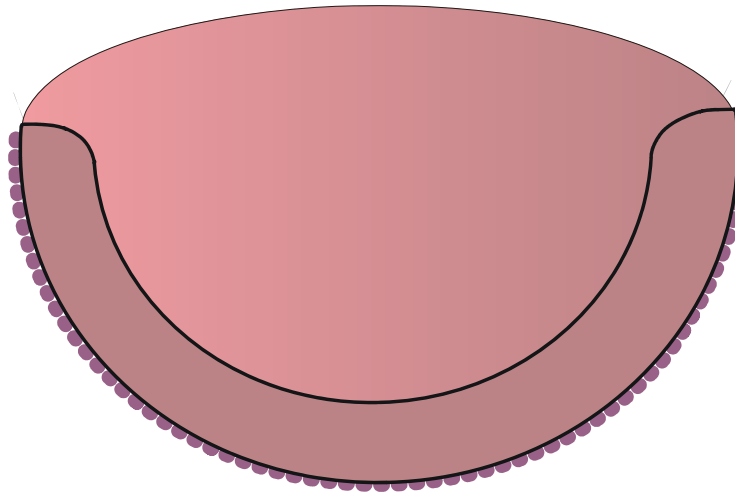


Variable	Unit	BIOLOX <sup>®</sup> forte	BIOLOX <sup>®</sup> delta
		Mean value	Mean value
Al <sub>2</sub> O <sub>3</sub>	Vol. %	99,8	80
ZrO <sub>2</sub>	Vol. %	n.a.	17
mean grain size	µm	1,75	0,56
4-point-bending-strength	MPa	631	1384
Young's modulus	GPa	407	358
frac. toughn. K <sub>IC</sub>	MPa m <sup>1/2</sup>	3,2	6,5



# Aim of the project

- ▶ development of a porous ceramic coating based on BIOLOX® *delta* for all-ceramic joint replacement



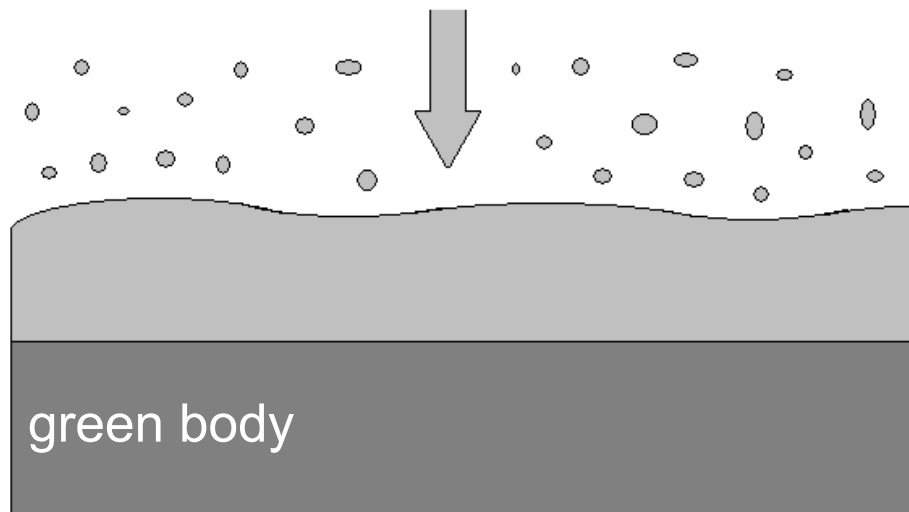
- ▶ reduced wall thickness (3 mm) → lower outer diameter
- ▶ improved functionality → combination of superior tribological properties of ceramics and direct osseointegration
- ▶ monolithical system → simplified implantation, avoiding surgical errors



- ▶ Background
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## spraying of ceramic slurry

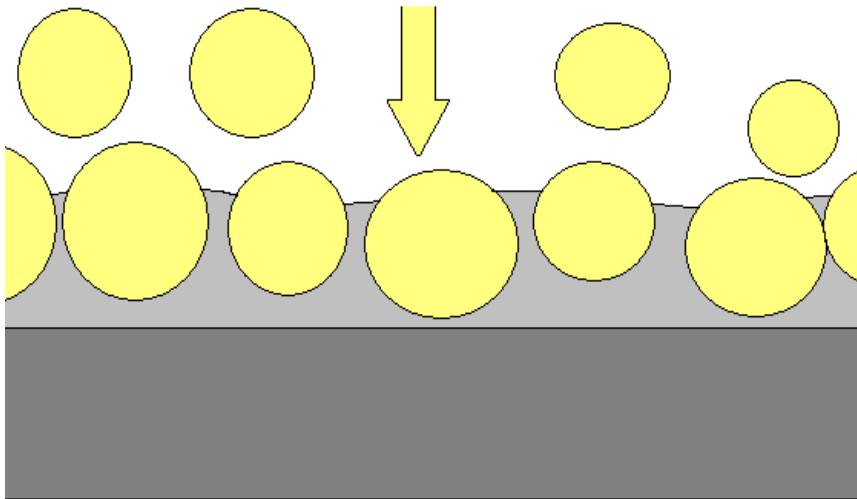


▶ semi - automated process





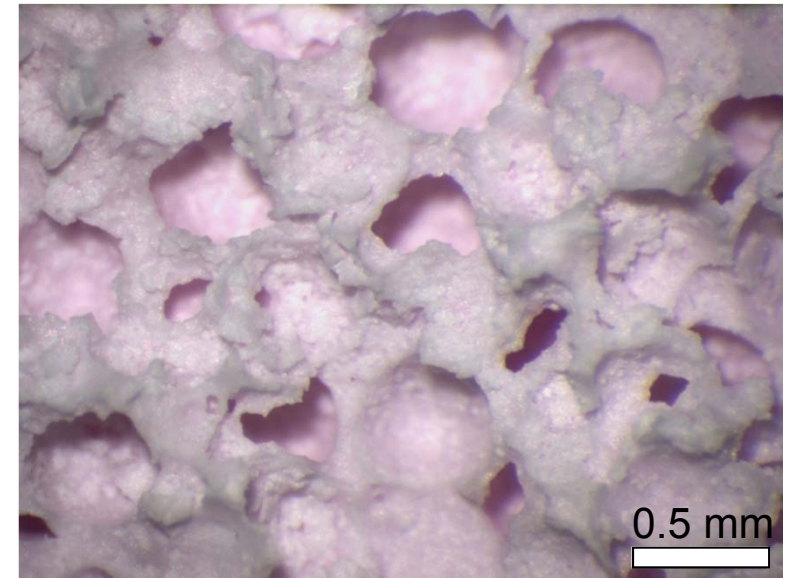
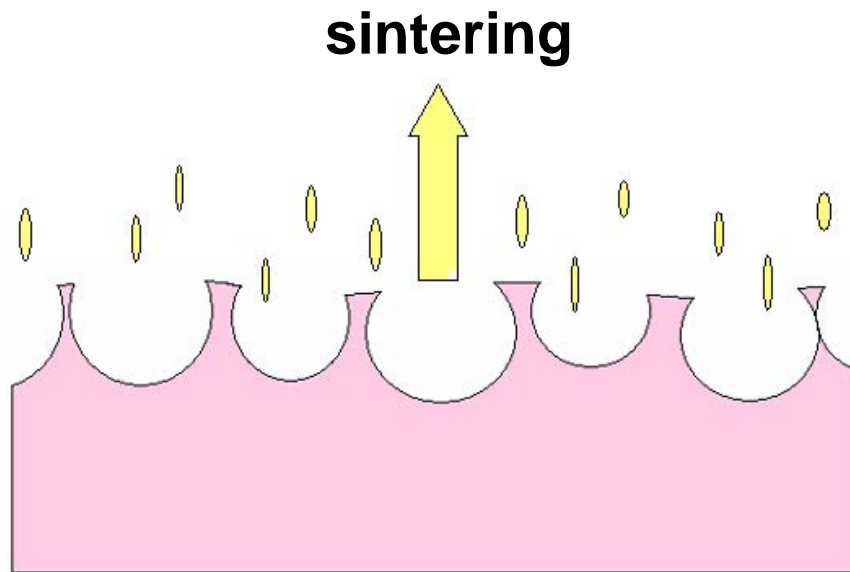
## spraying of pore forming agent



- ▶ pore forming agent: organic material
- ▶ pore forming agent is completely removed during sintering process



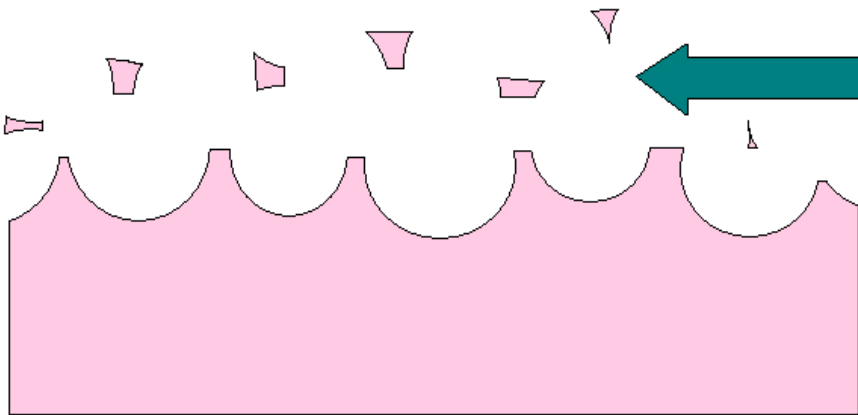
## sintered coating



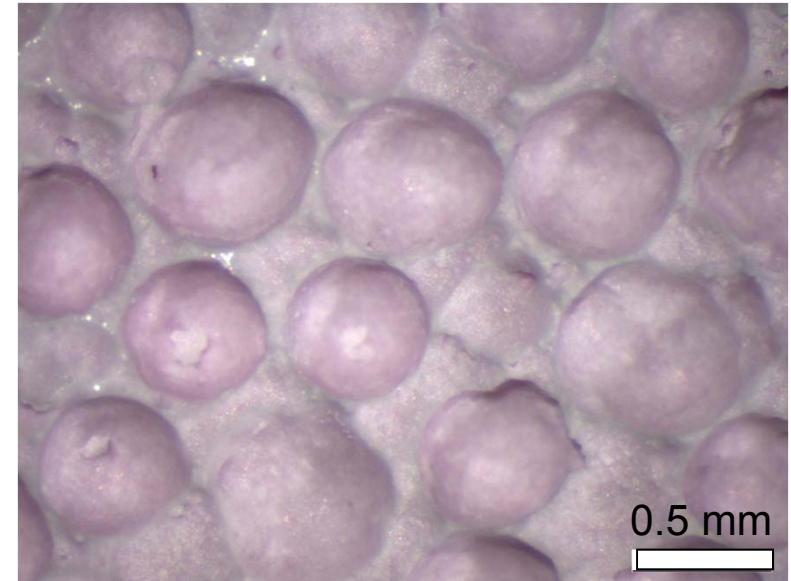
- ▶ thermal removing of pore forming agent
- ▶ properties of coating depend on sintering temperature, pressure and sintering time



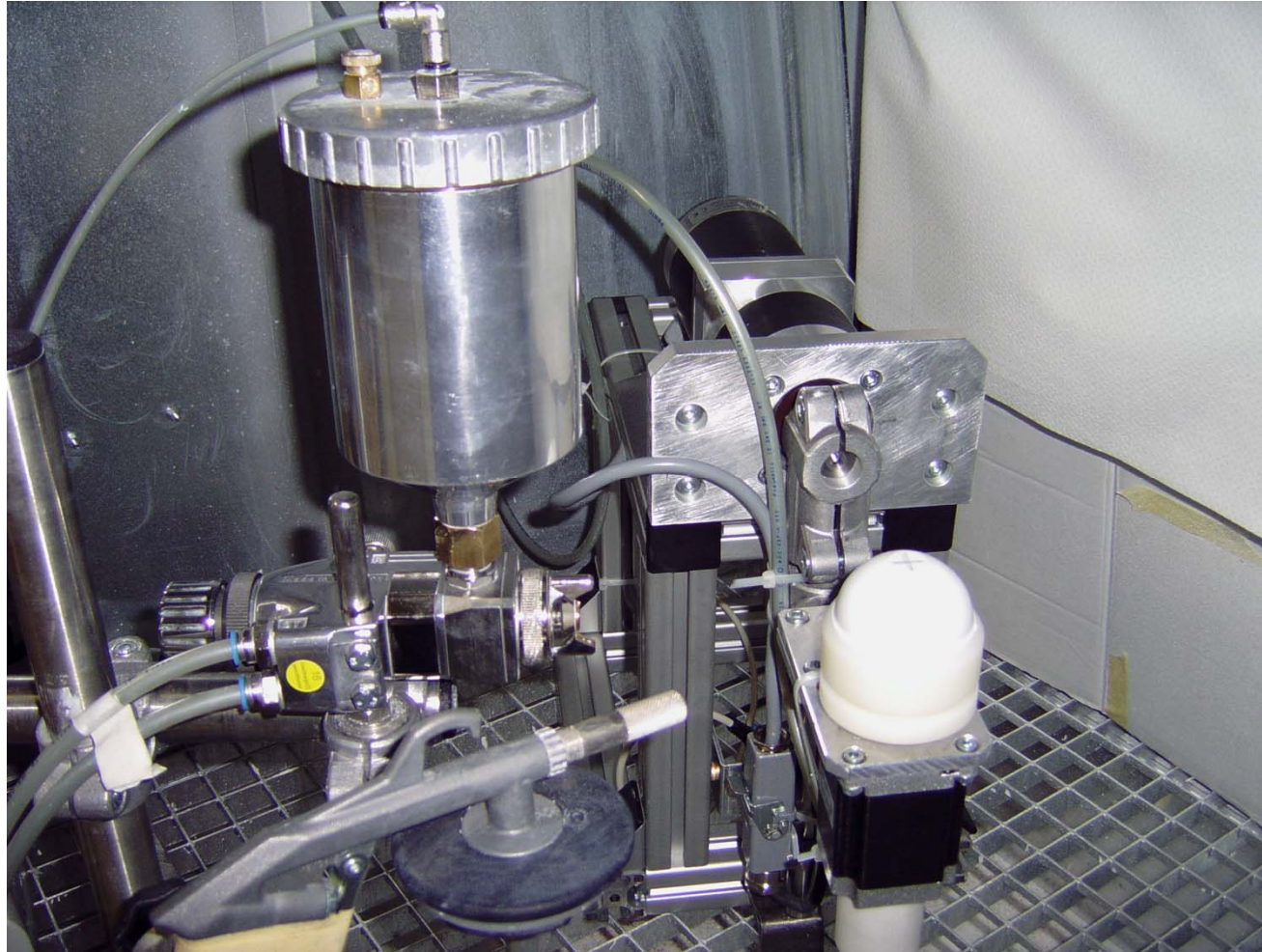
## blasting process



## finished coating surface



- ▶ removing mechanically instable parts of the coating
- ▶ pore opening



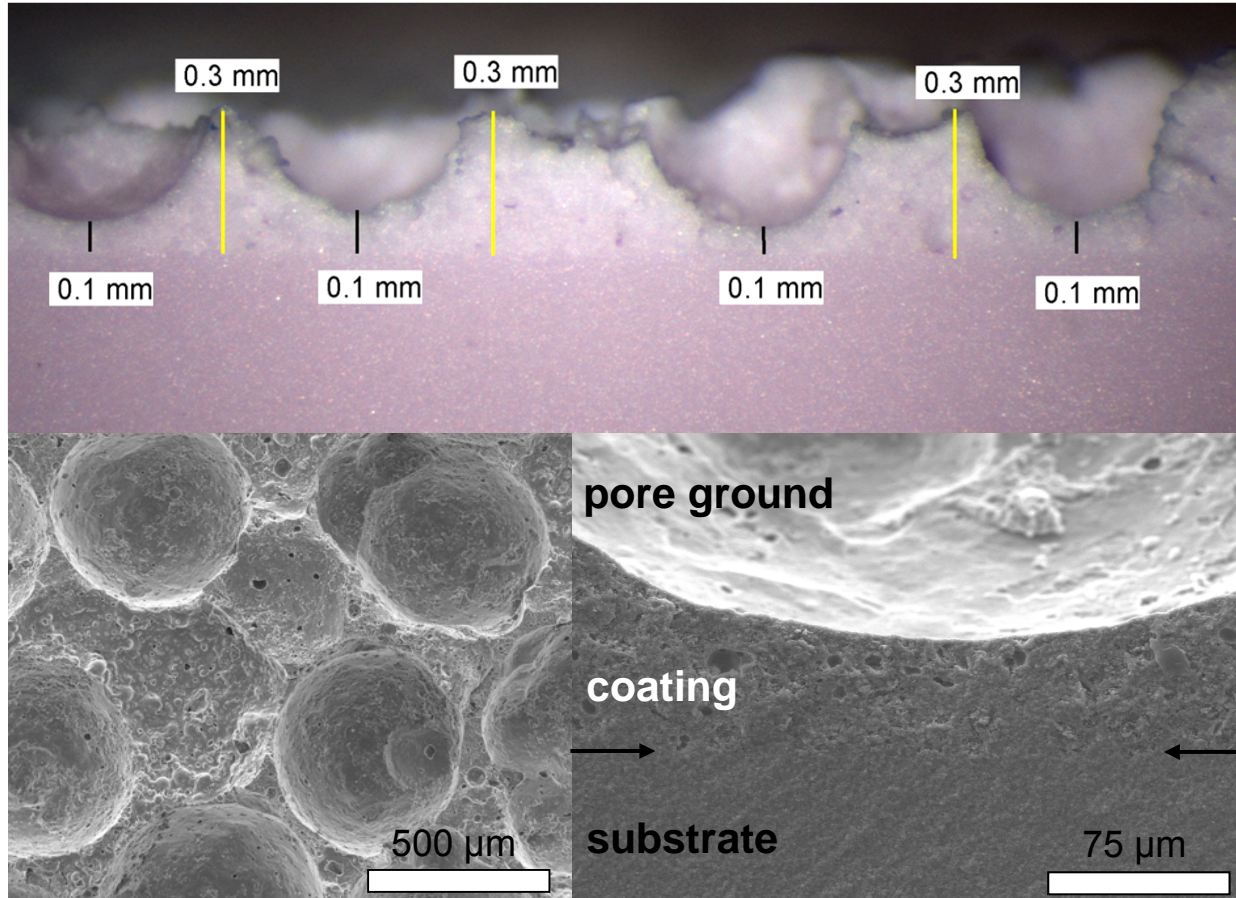
Coating process is bench-scale unit



- ▶ Background
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# Characterization: optical microscope / SEM



→ surface porosity  
app. 47 %

→ pore size (diameter)  
200 – 500 μm

→ hemispherical pores

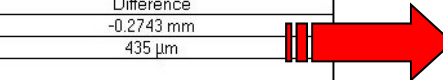
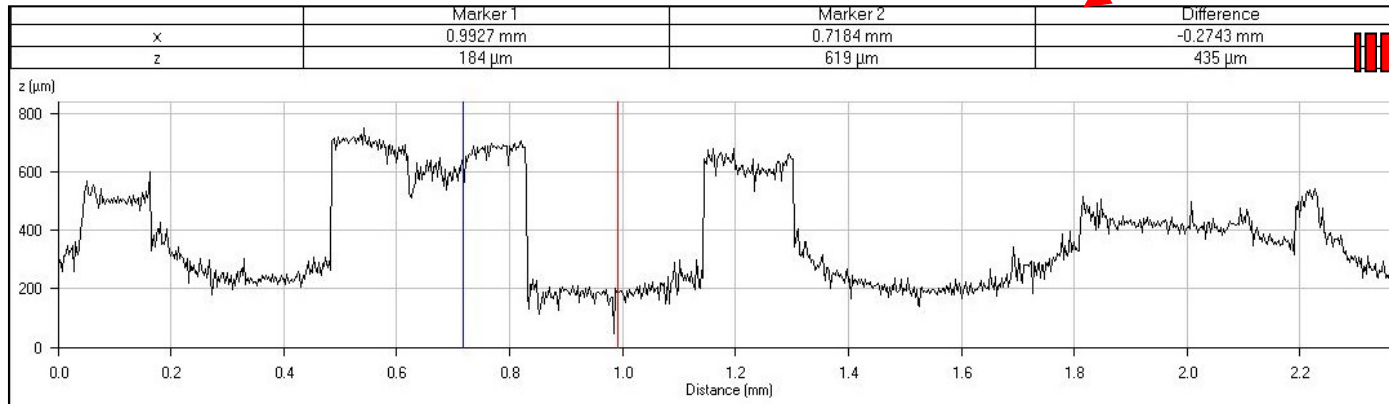
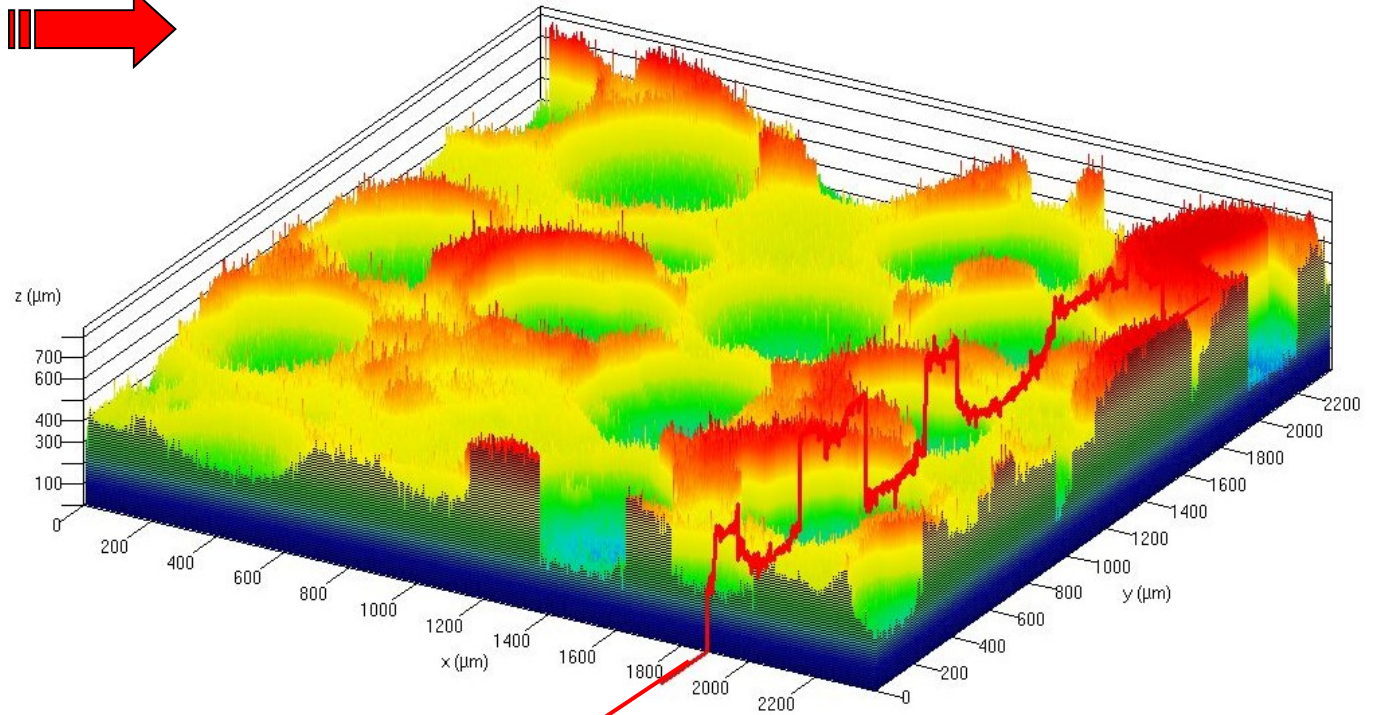
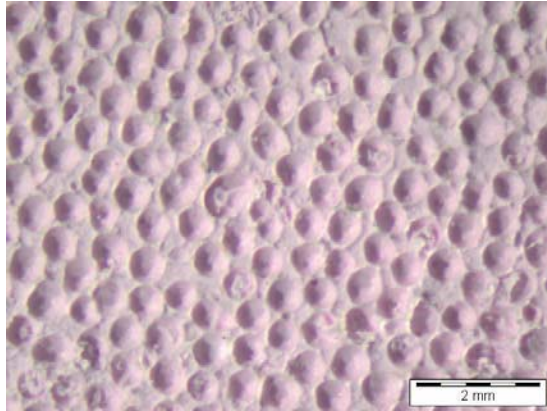
→ surface enlargement by  
factor 2 to 3



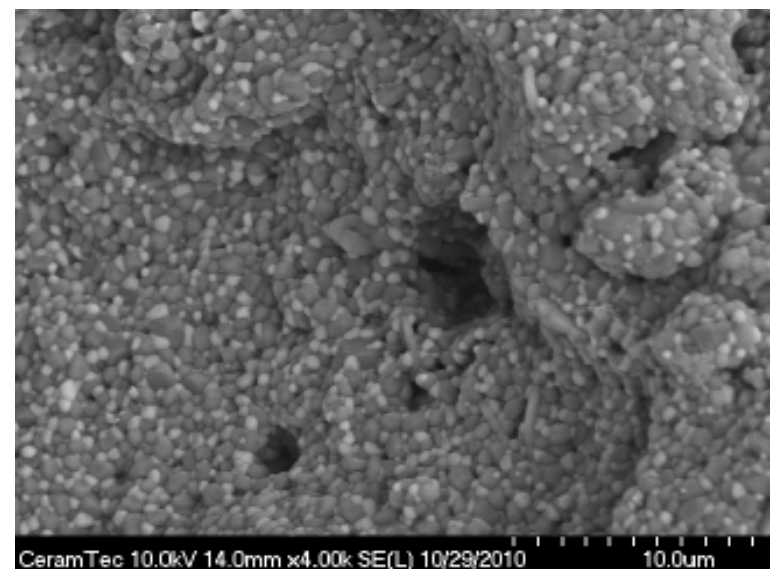
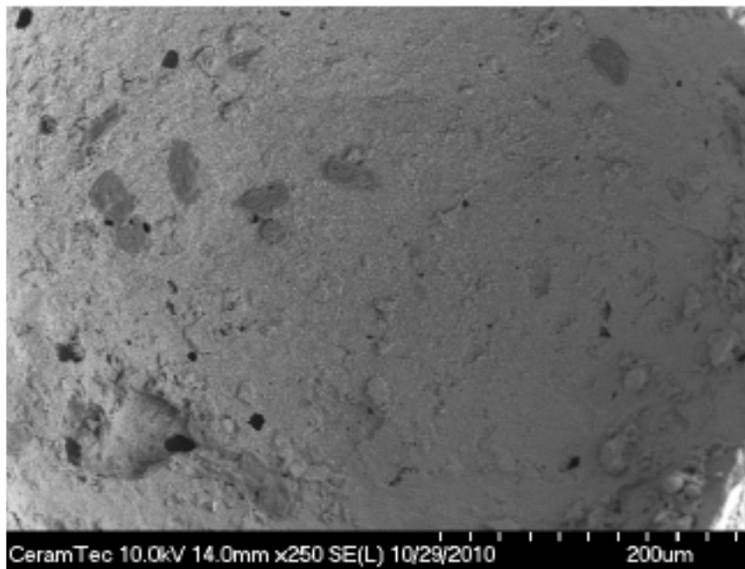
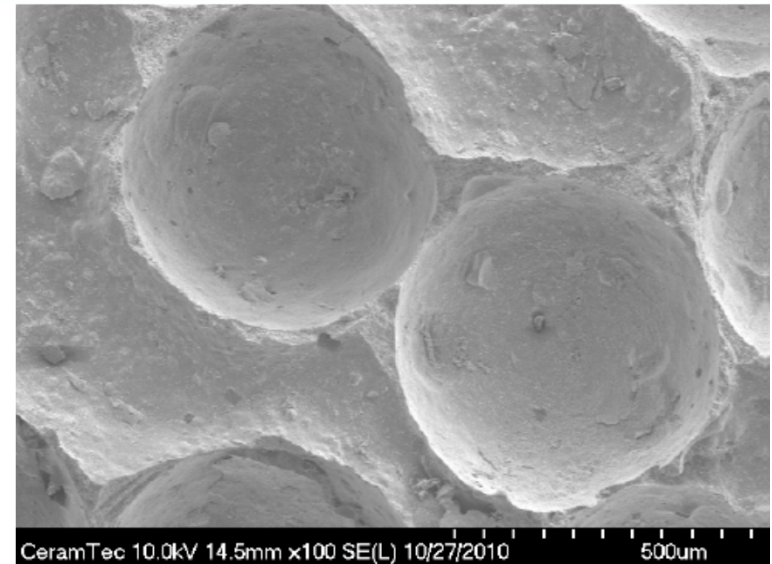
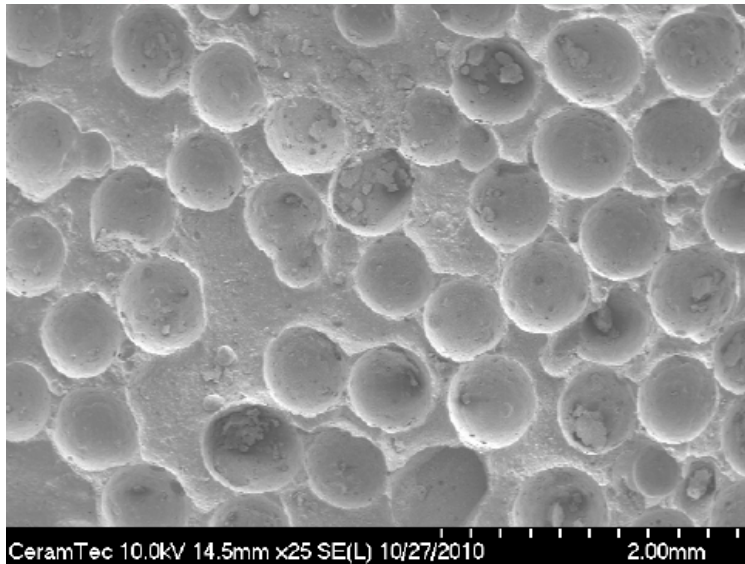
**highly reproducible surface structure**



# Characterization: Laser-scanning-microscope



roughness:  
 $R_z = 435 \mu\text{m}$



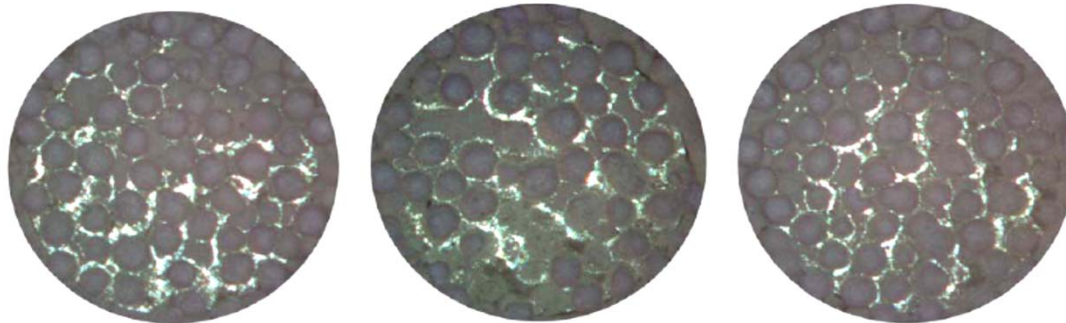
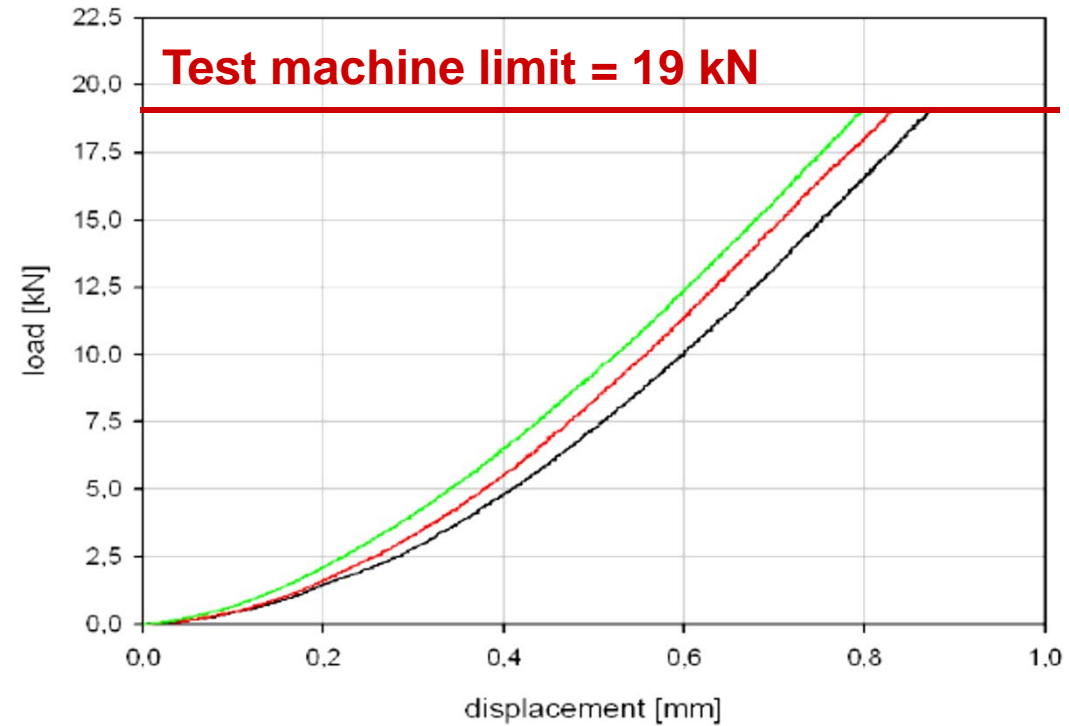
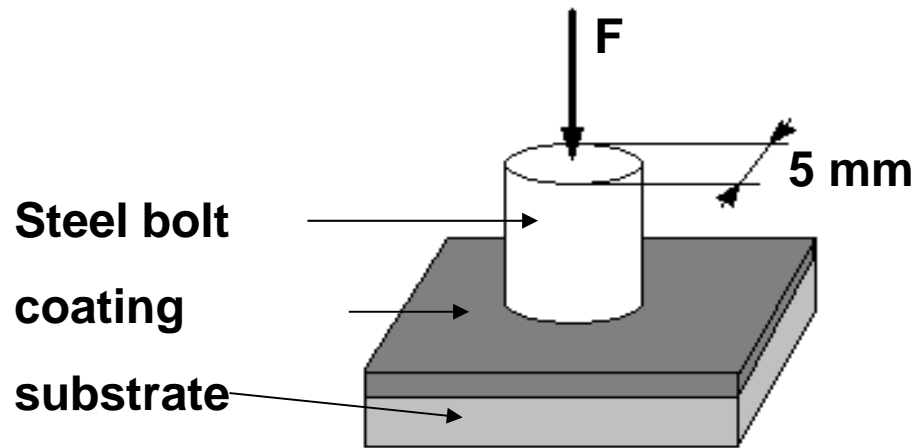




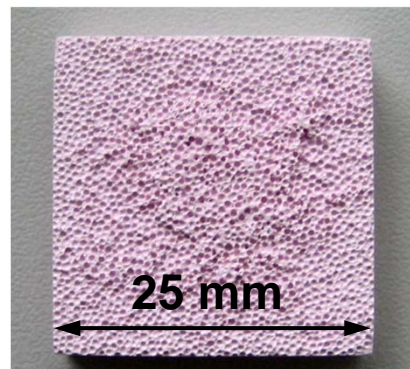
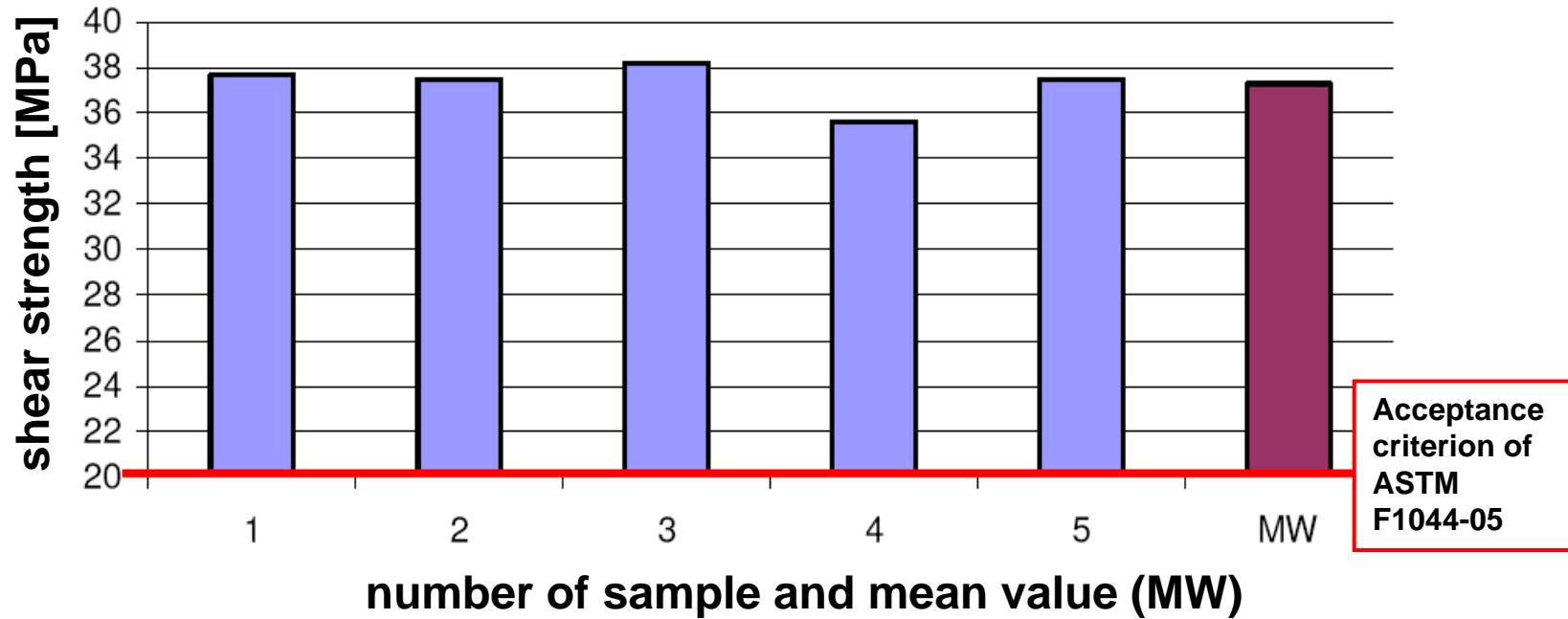
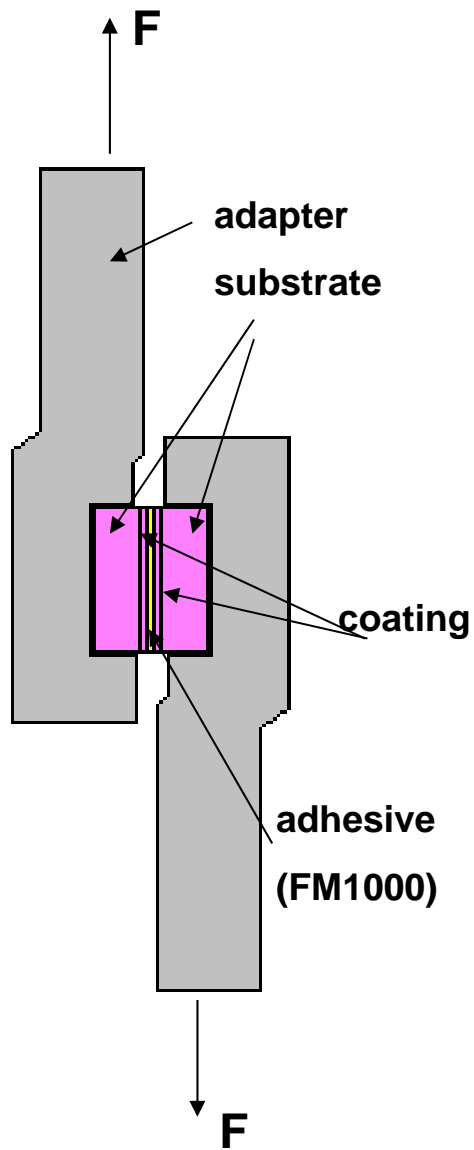
- ▶ Background
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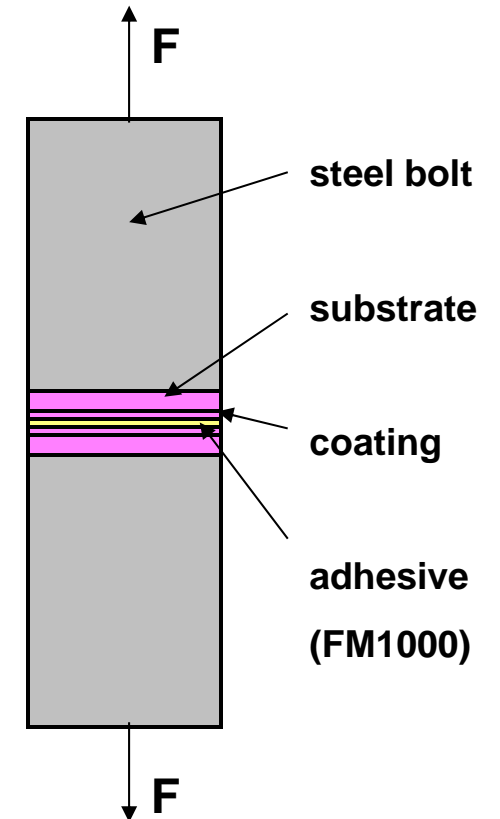
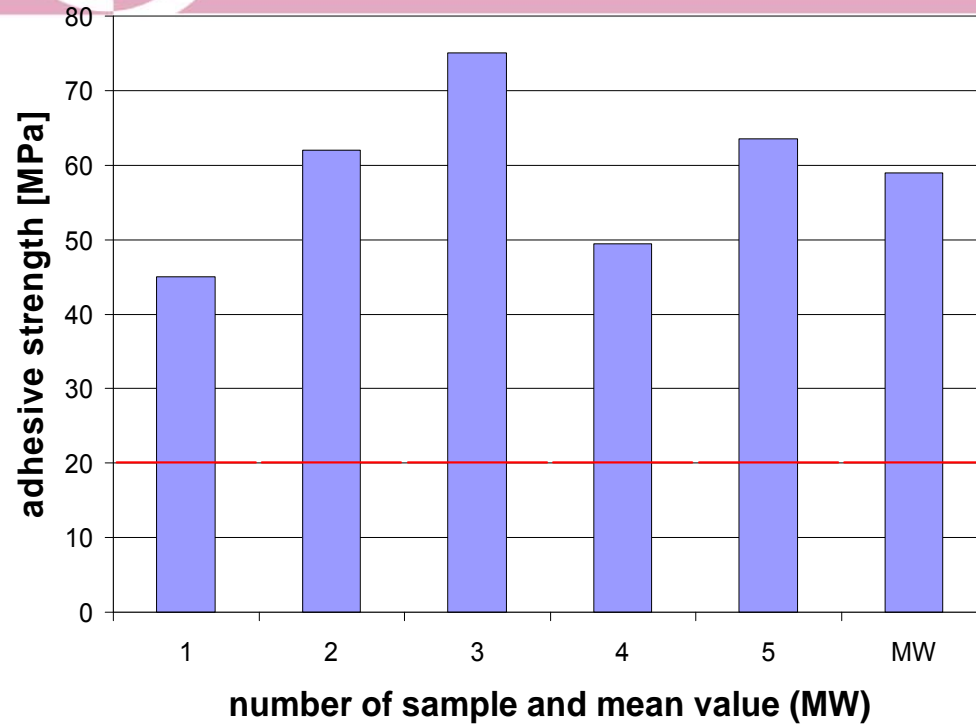
# Characterization: compression strength



- weight equivalent 1,9 t
- steel bolts were deformed
- no damage occurred at the coating

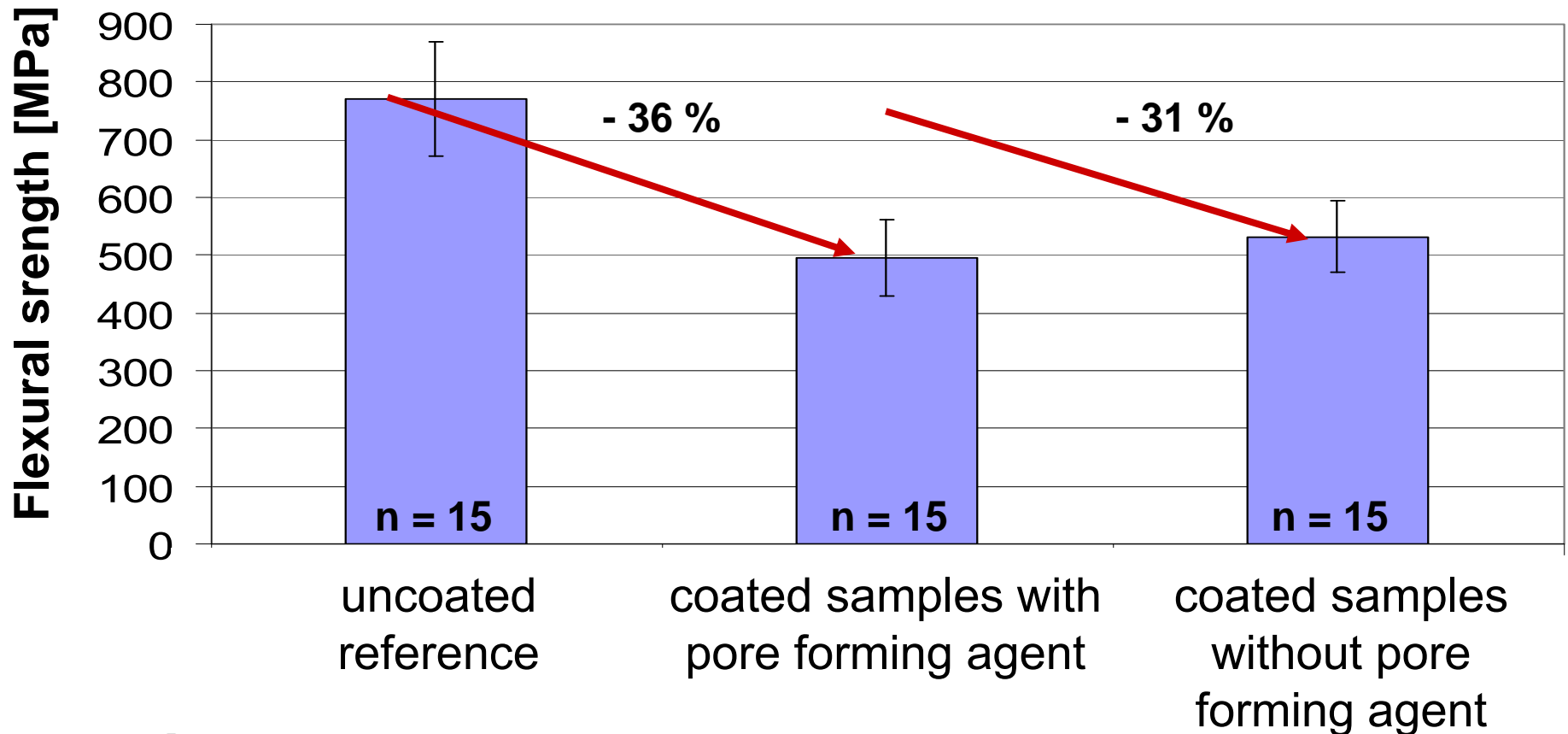
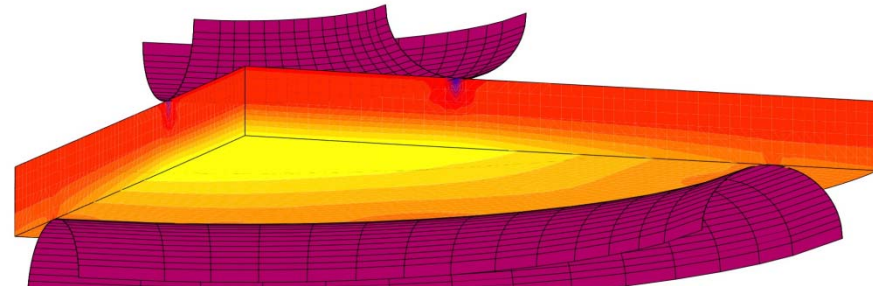


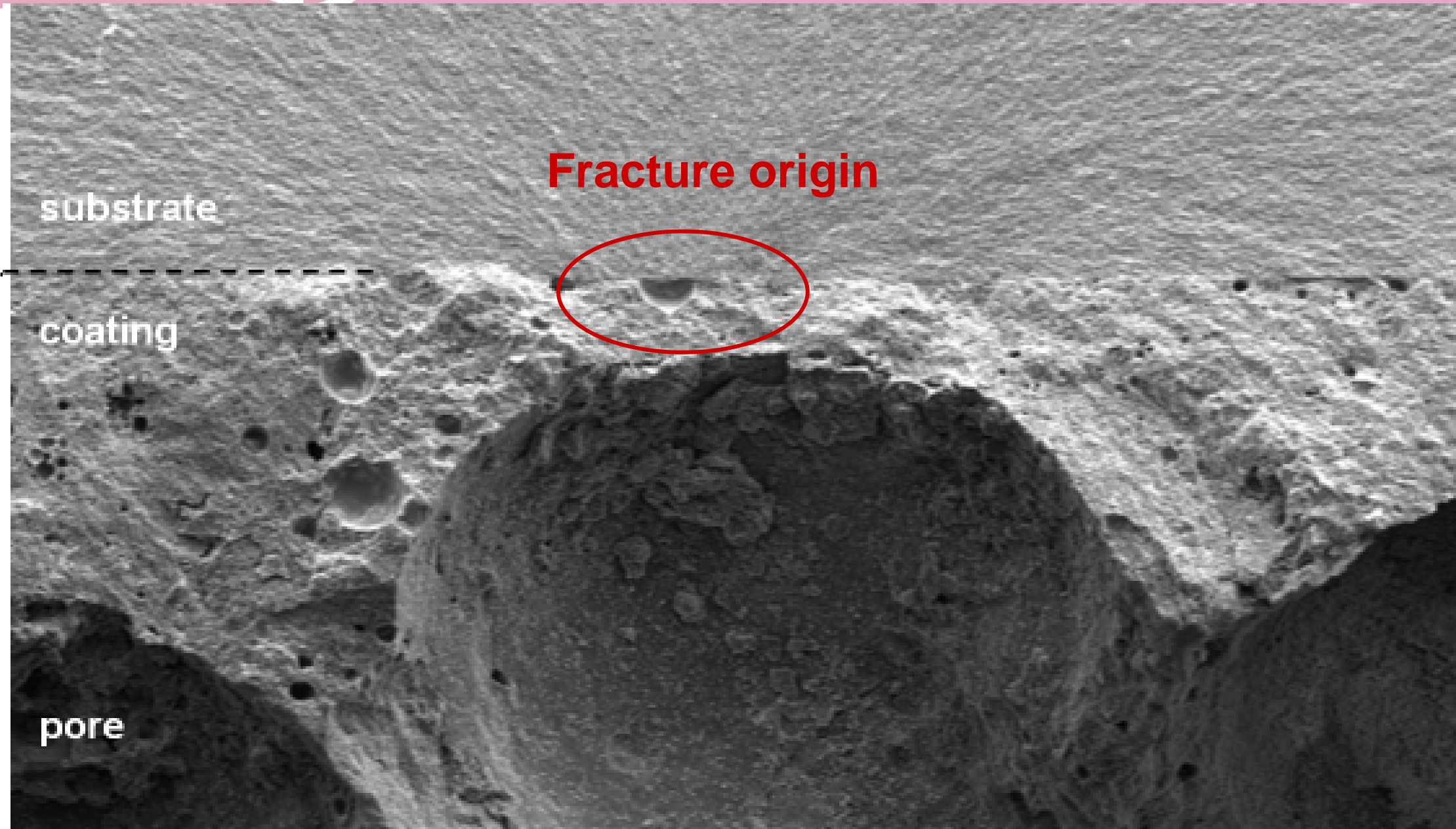
► no delamination of the coating





# Characterization: biaxial bending strength





substrate

**Fracture origin**

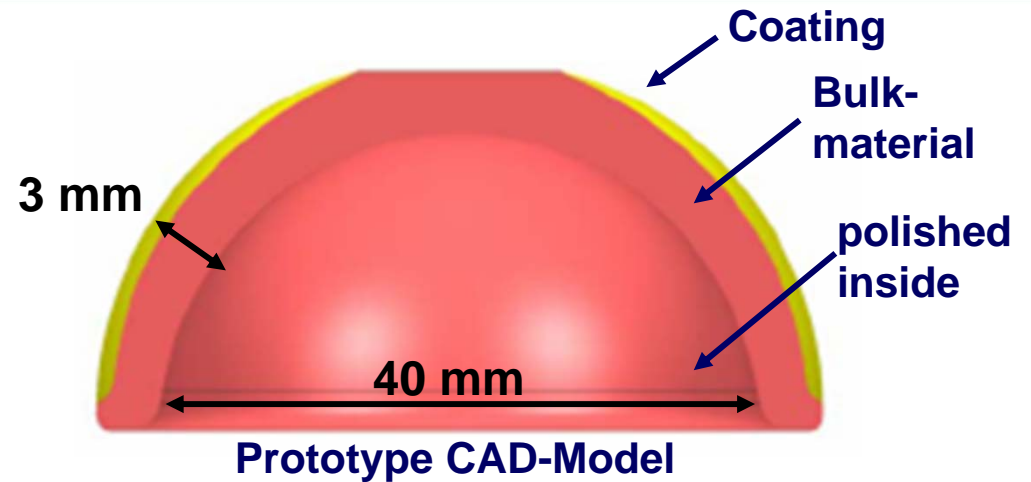
coating

pore



## Requirements:

- Testing geometry hip joint cup
- bearing couple 40 mm diameter
- wall thickness as small as possible  
(minimized space requirement)



## Cup-Design relates to:

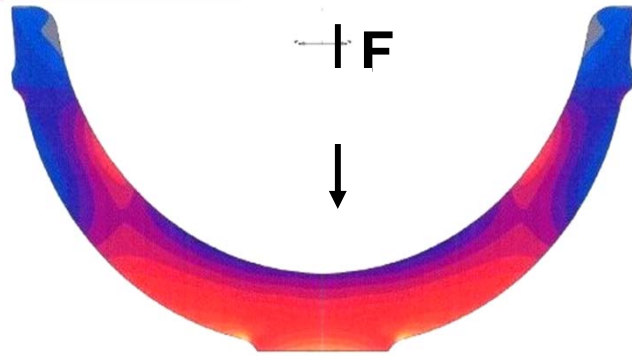
- range of motion
- luxation stability
- mechanical stability
- production process



Prototype



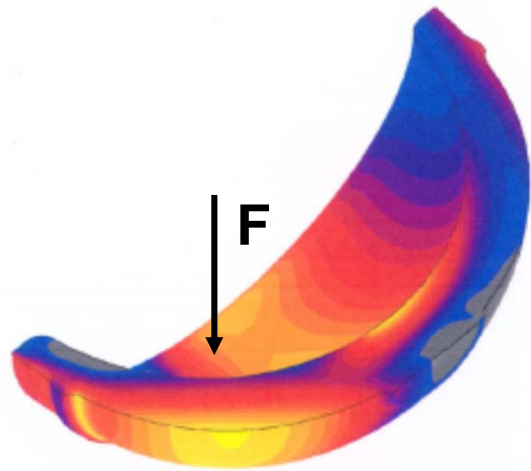
# In-vivo like burst-test without backside support



**Burst-Test axial**



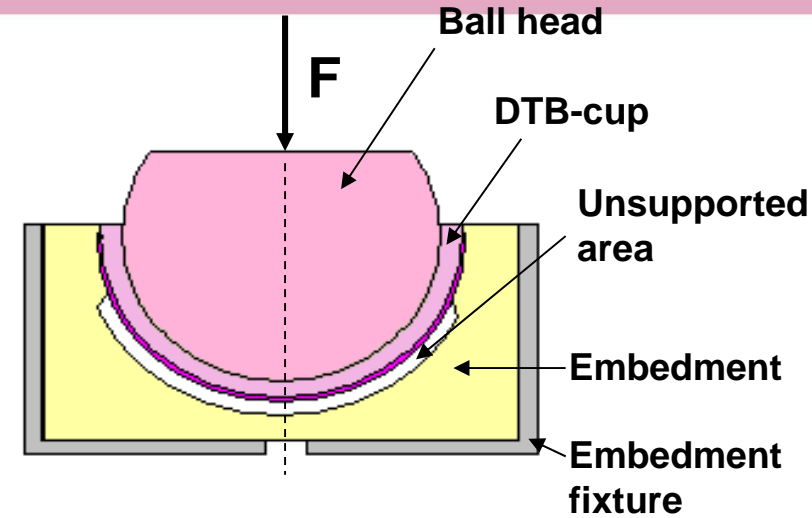
**Stress-analysis  
(Finite Element Methode)**



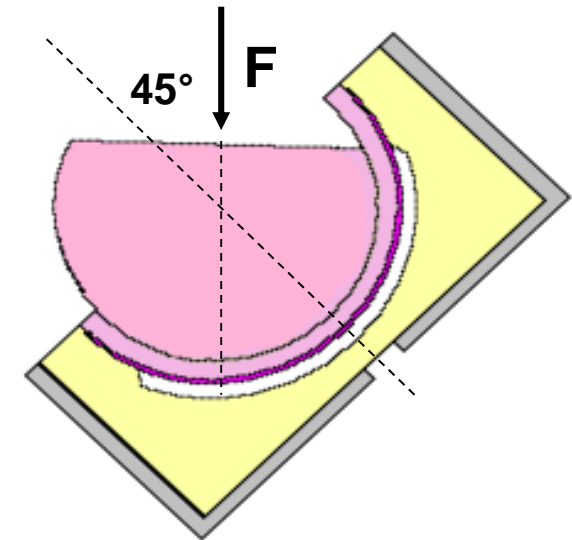
**Burst-Test 45°**



**according  
„upright standing“**



**Test Setup**





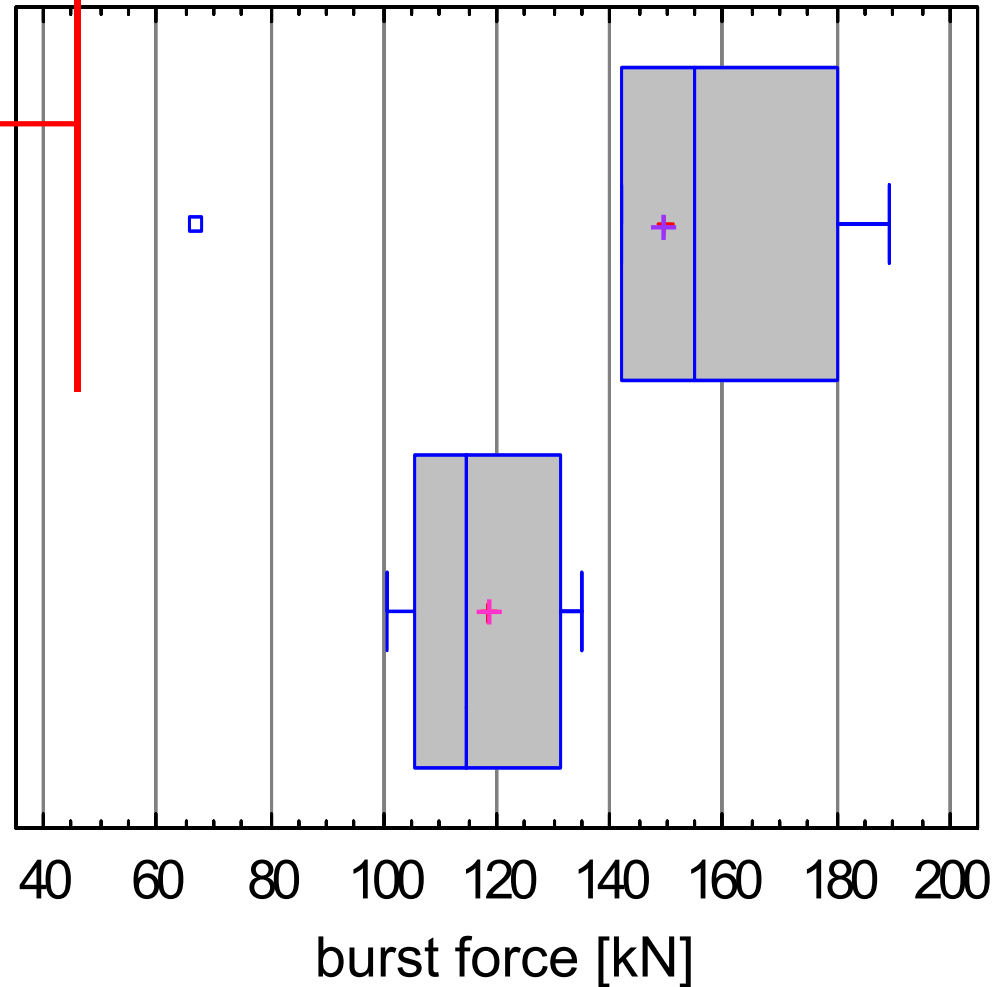


# Results of burst-test

Acceptance criteria for  
regular ceramic inserts  
in metal shells  
 $F \geq 46$  kN

burst-test axial

Burst-test 45°

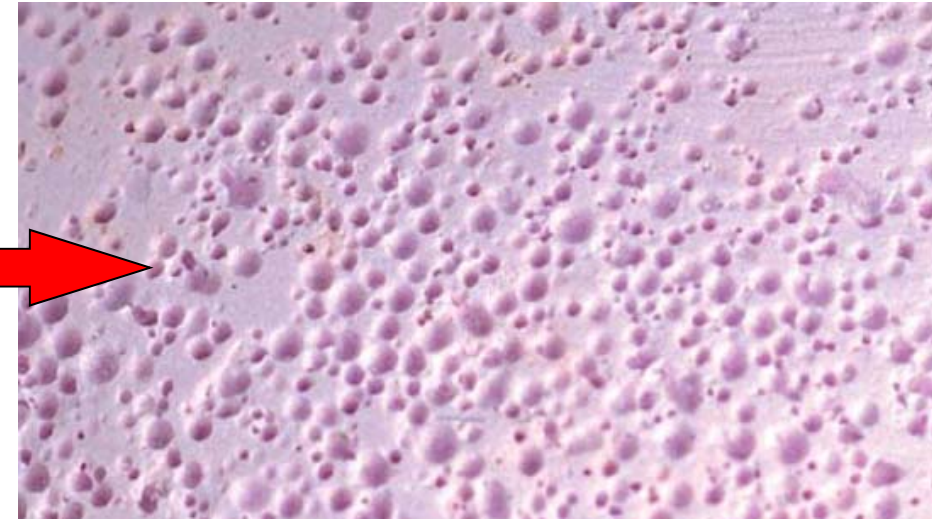
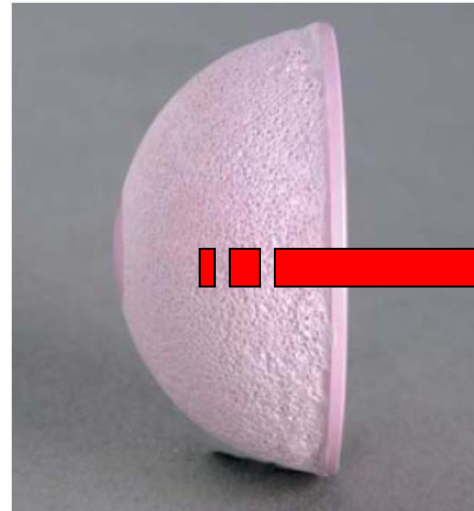
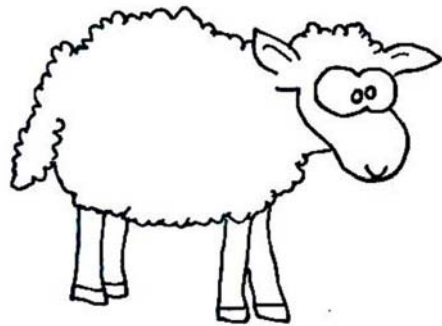


+ mean value  
150 kN  
std. dev. 40 kN  
n = 7

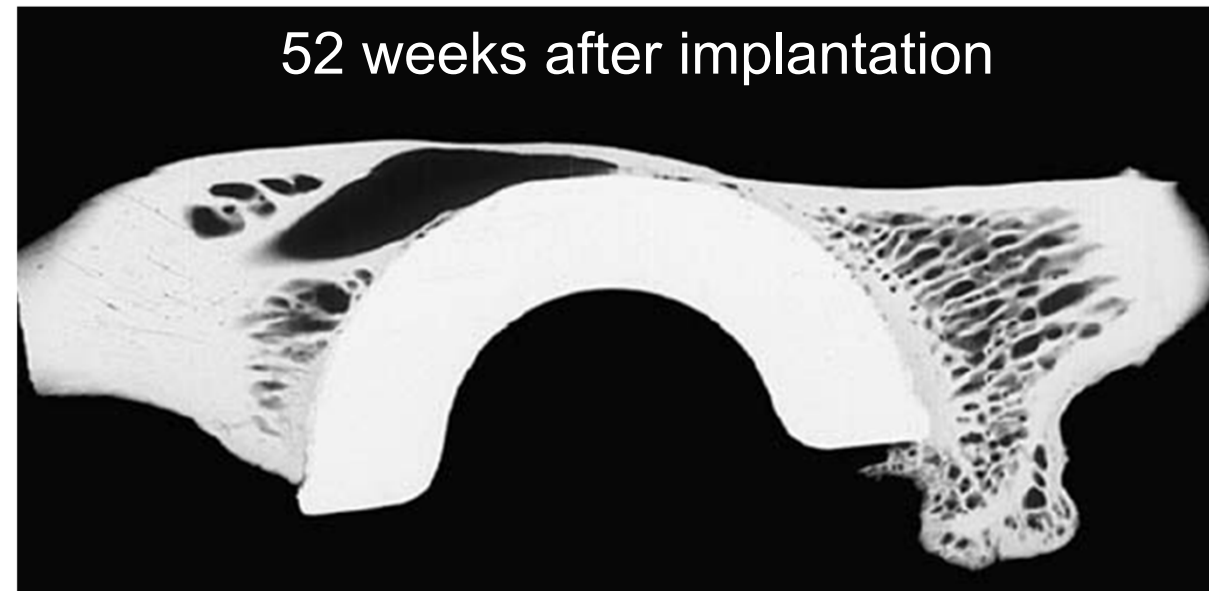
+ mean value  
118 kN  
std. dev. 14 kN  
n = 7



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Schreiner,  
Schulze,  
Schwarz et  
al.,  
ZOrthopUnf  
all 2011

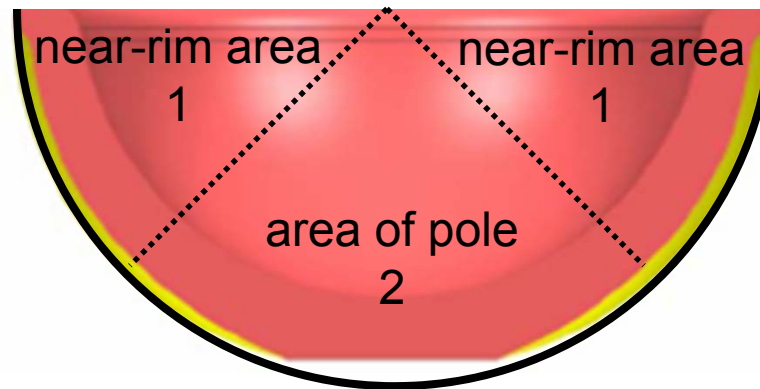


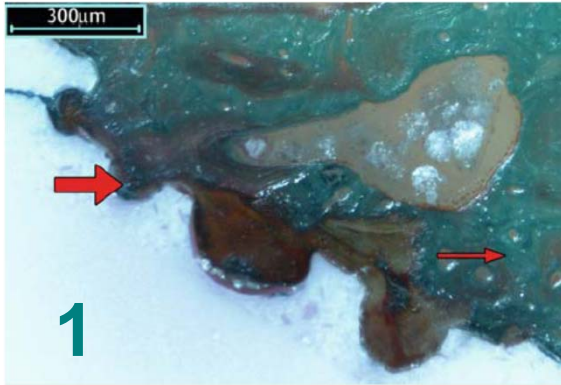


## Masson-Goldner stain

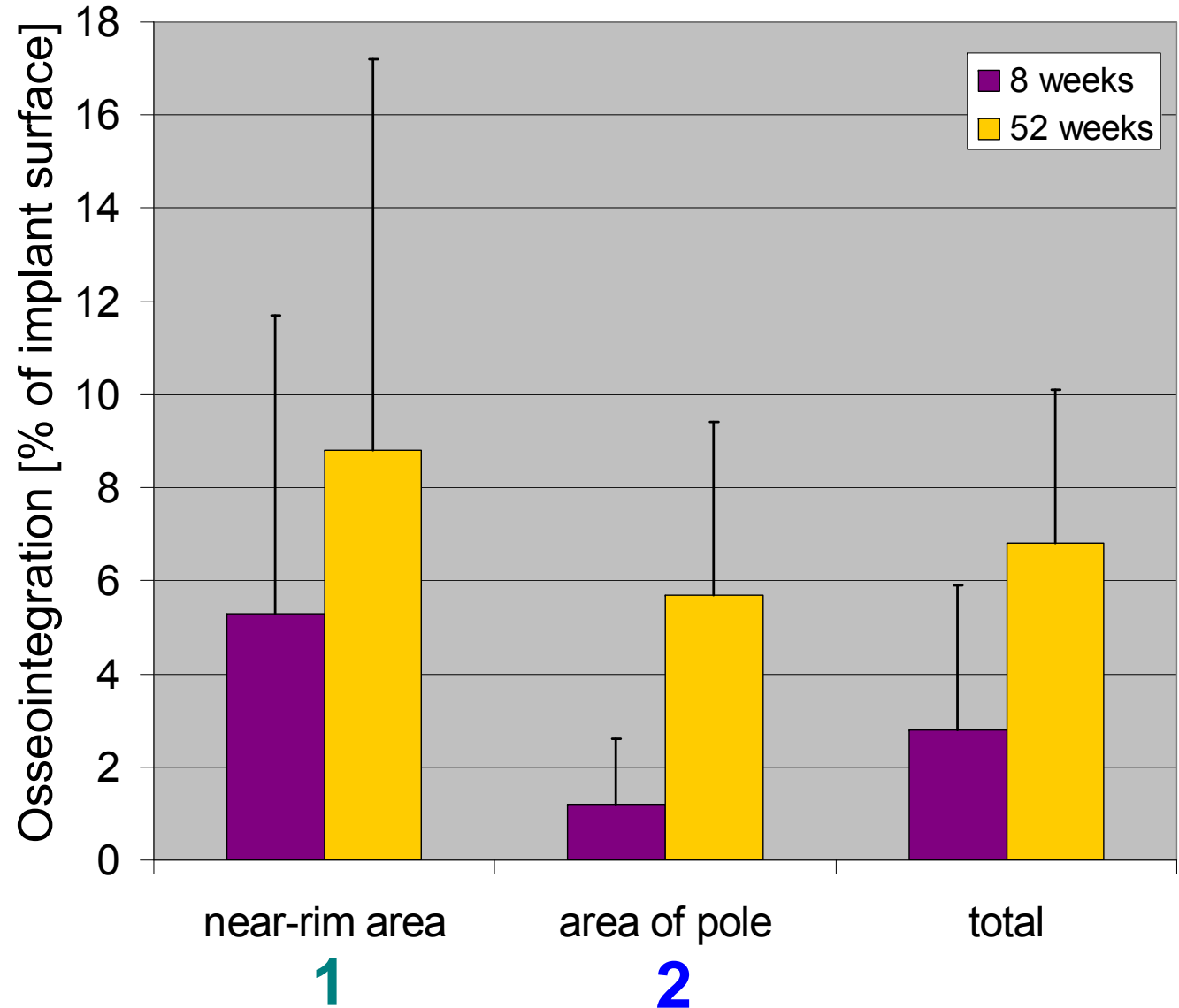


Schreiner,  
Schulze,  
Schwarz et  
al.,  
ZOrthopUnf  
all 2011



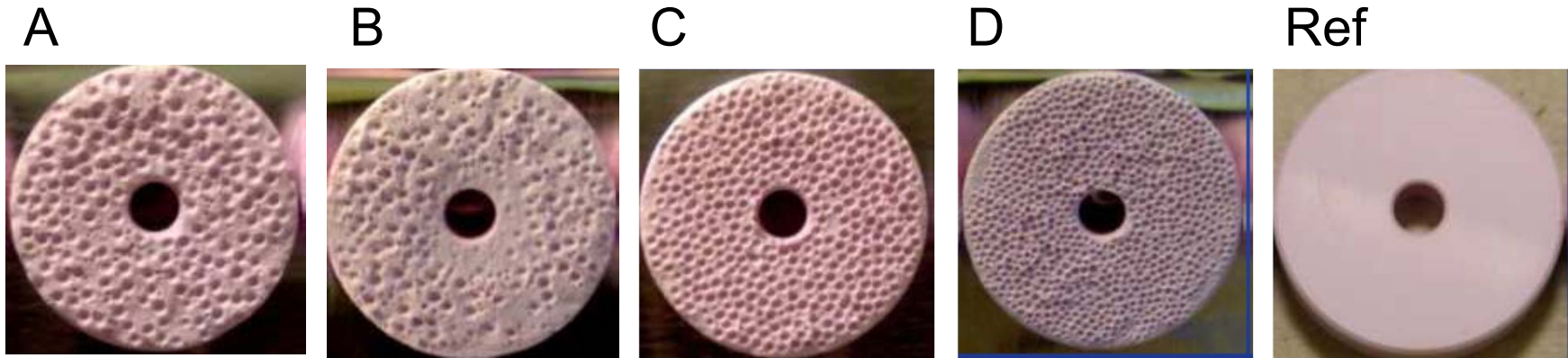


Schreiner,  
Schulze,  
Schwarz et  
al.,  
ZOrthopUnf  
all 2011



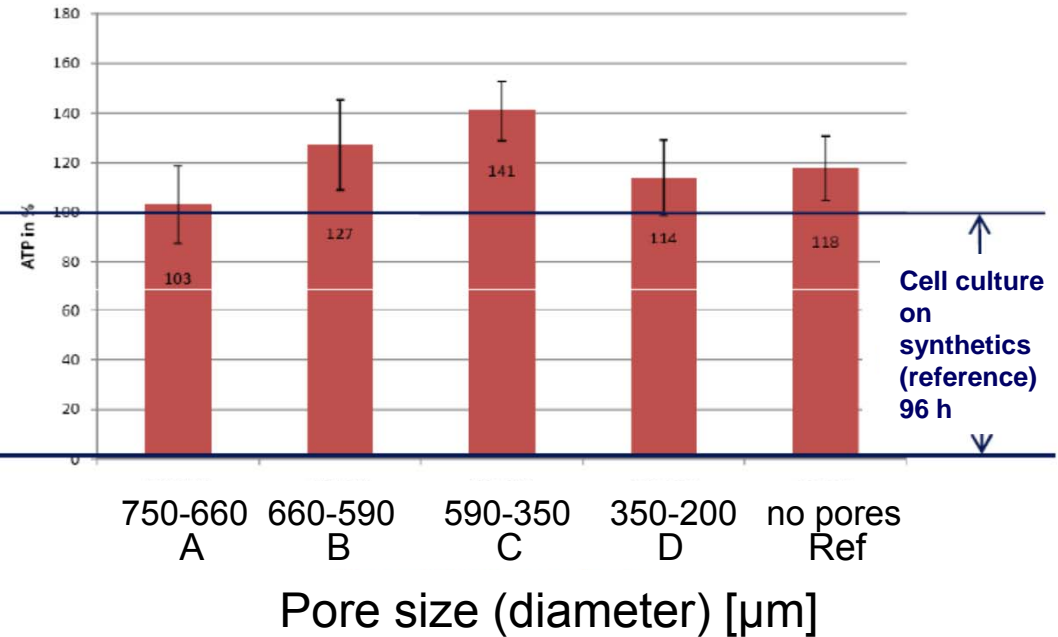
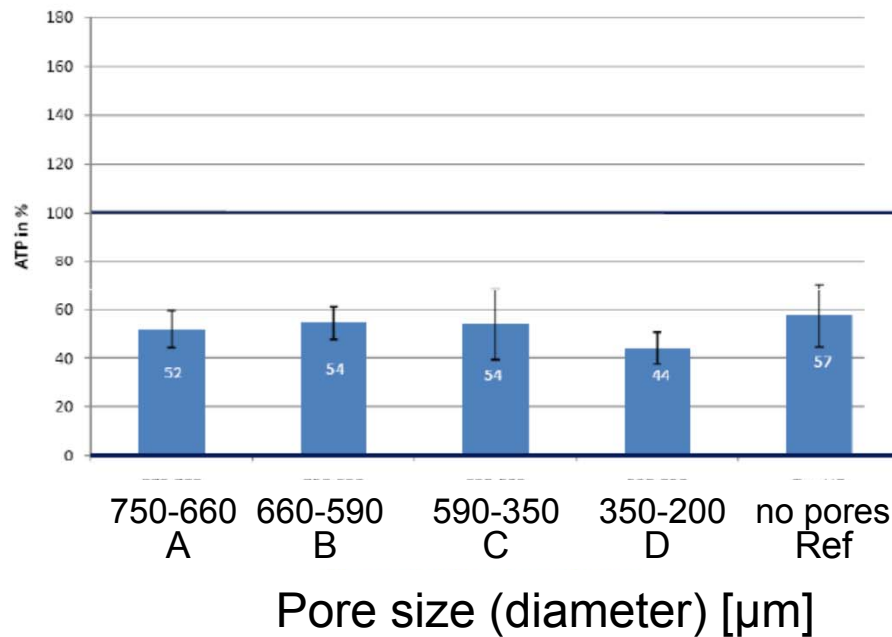


# Cell-tests (humane osteoblasts) of different pore size distributions



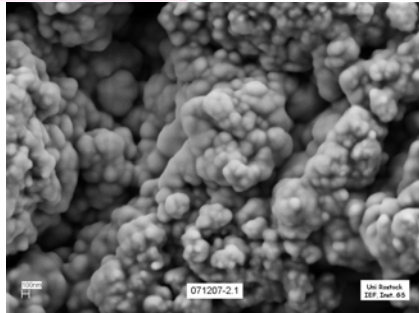
Proliferation after 24 h (n=14)

Proliferation after 96 h (n=14)



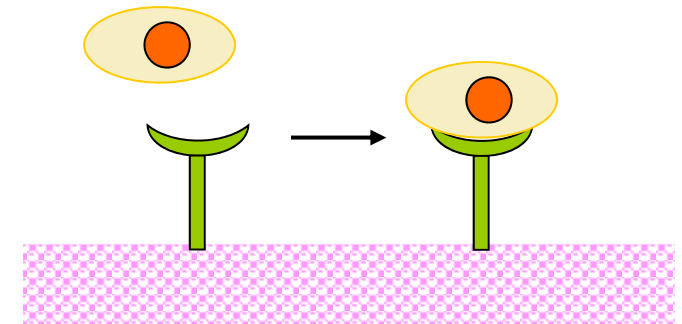
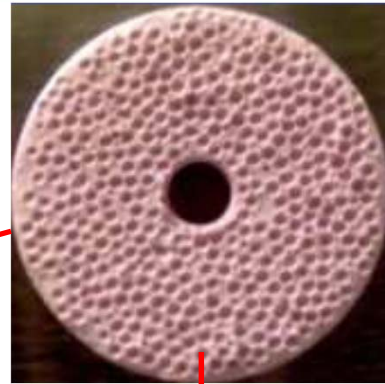


# Test of osseointegration



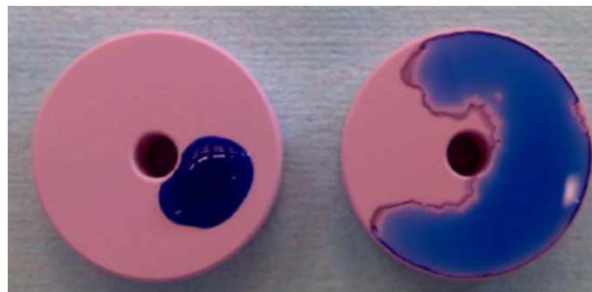
+ Hydroxyapatite,  
 $\text{Ca}_5[\text{OH}(\text{PO}_4)_3]$

- ▶ inorganic part of bone
- ▶ no development of connective tissue



+ RGD-Peptides

- ▶ protein of extracellular matrix
- ▶ adhesion of cells using Integrin-coupling
- ▶ mechanically stable cell network



not activated

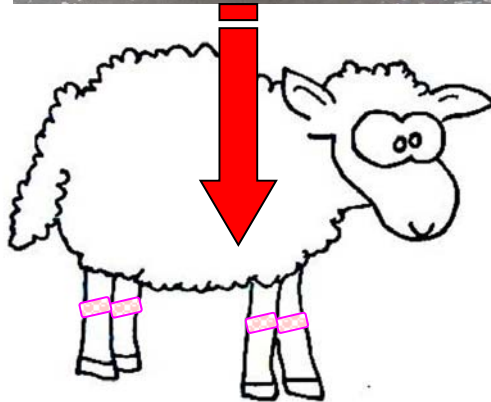
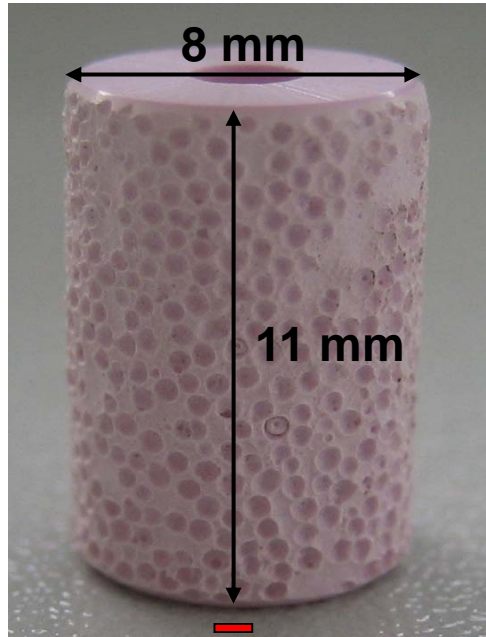
with O<sub>2</sub>-Plasma  
activated

+ Plasma-activation

- ▶ decrease of contact angle (↓)
- ▶ increase of surface energy (↑), leads to higher adhesion of bone cells
- ▶ reaction gas: oxygen
- ▶ durability: 4 days (reversible reaction)



# Osseointegration in biological study (sheep)



4 implants per leg



Bulk material (pink)

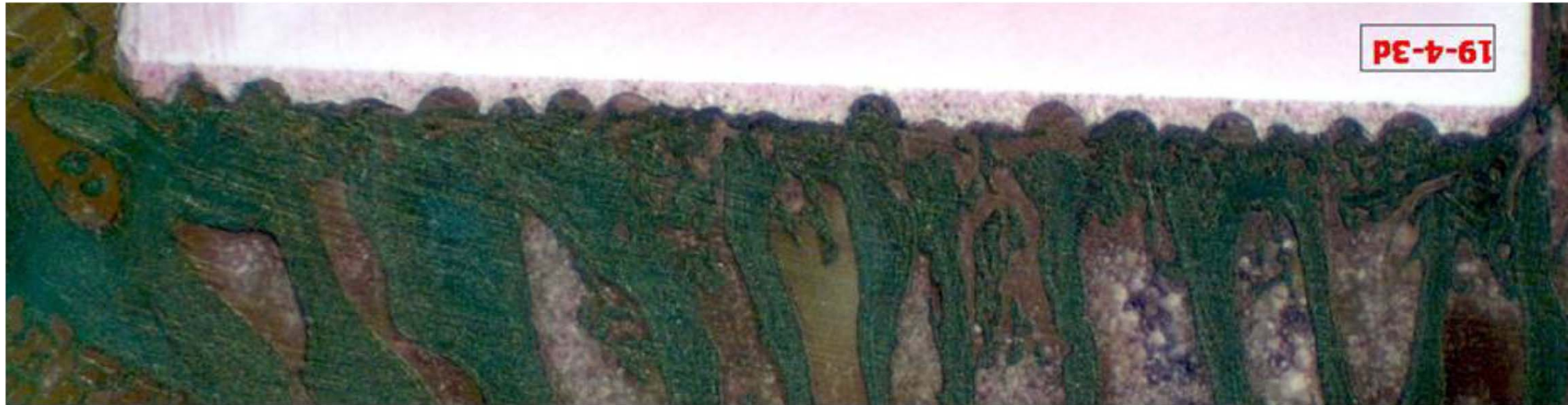
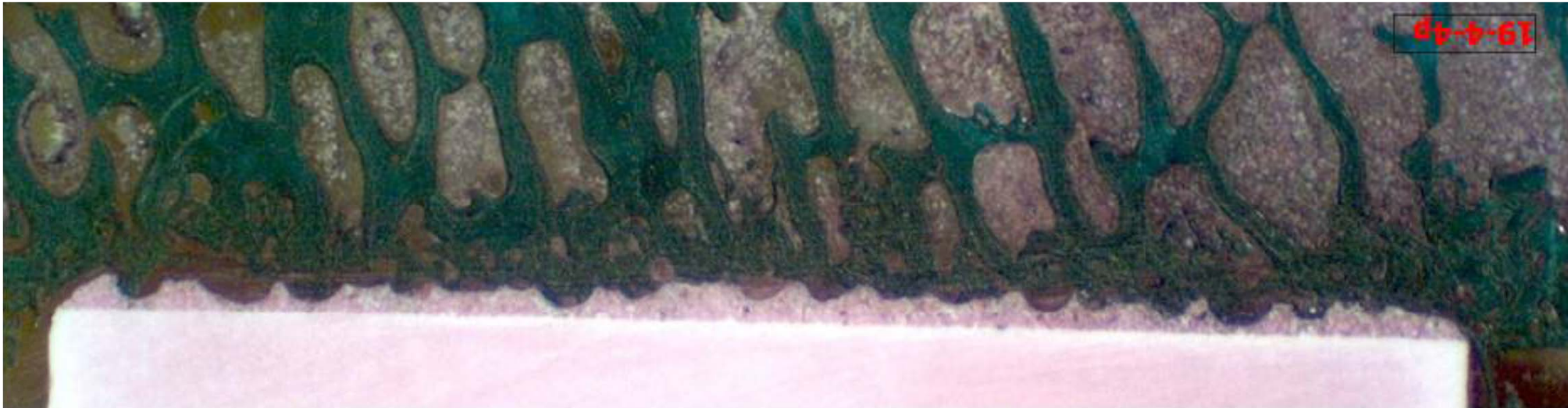
Coating (pink)

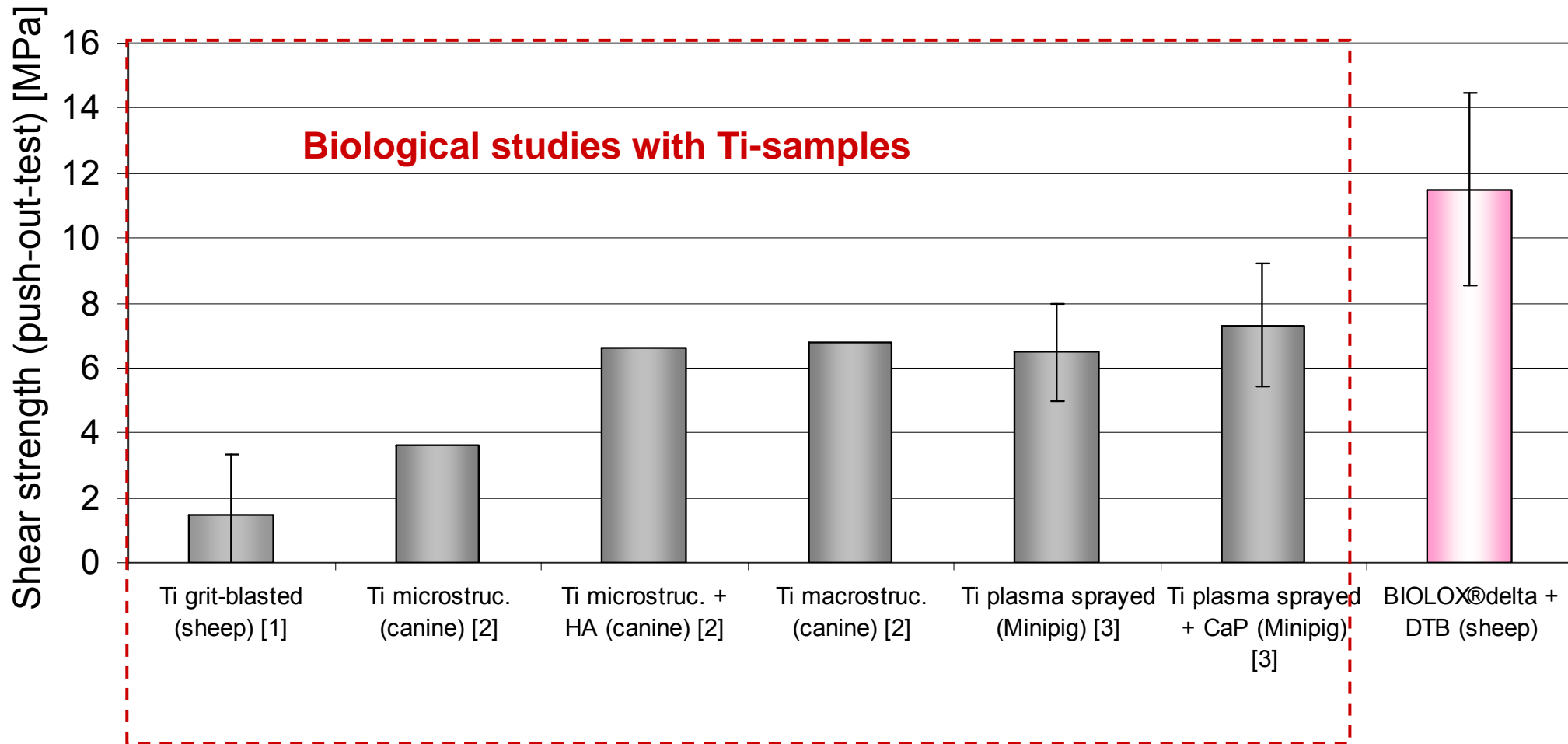
Bone (green)





# Osseointegration in biological study (sheep)

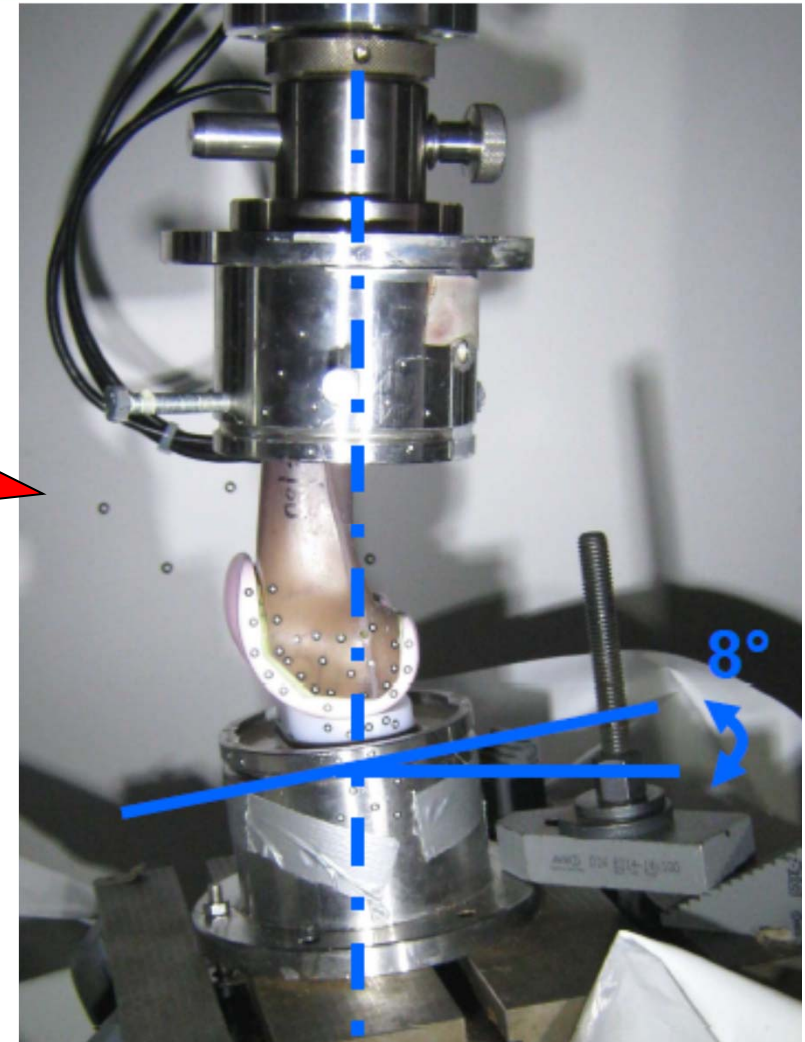
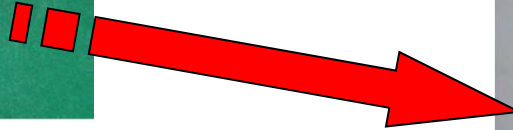
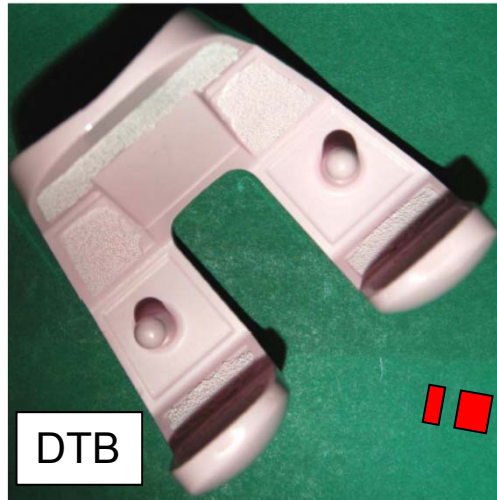




[1] H. Hartwig, L. Rehak, et al., Biomed. Tech. 1995 40, S. 99-105

[2] R. Rack et al., Bioceramics in Joint Arthroplasty Stuttgart, New York: Thieme 2001, S. 103-108

[3] E. Steinhauser, R. Bader, et al., Materialprüfung 2005 47 S. 197-202



## fatigue-test:

cementing on Sawbone<sup>®</sup> using Palacos<sup>®</sup>R,

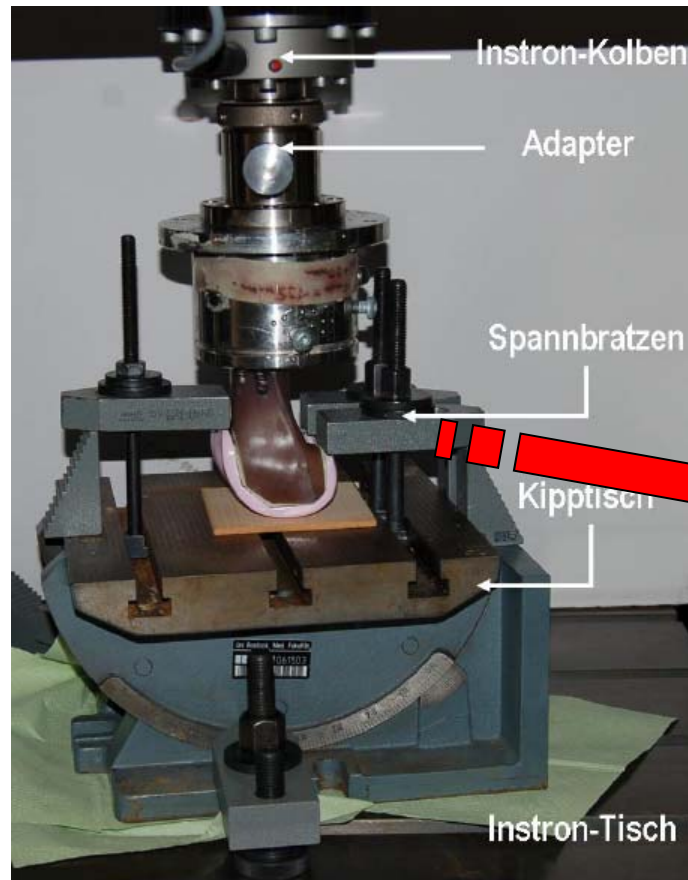
**1.5 million cycles, 5 Hz**

with flexion angles of 8°, 15° and 110°

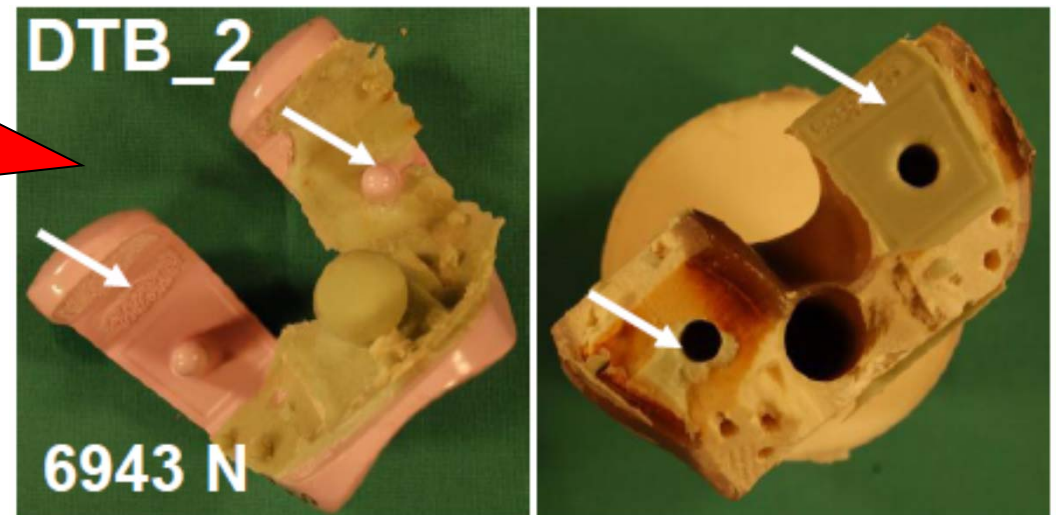
**highest load 2.6 kN**

**lowest load 168 N**

outer/inner rotation between -1.9° and +5.7°



**Post-fatigue pull-off test:**  
way-controlled, 5 mm/min





- ▶ Coating process is reproducible
- ▶ Alumina-Zirconia-ceramics are biocompatible materials
- ▶ porous coating leads to bone ingrowth ⇒ shear strength of bone and implant is comparable with Titanium implants
- ▶ Coating is fully bonded to substrate during sintering ⇒ very good mechanical testing results ⇒ acceptance criteria of FDA passed!



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